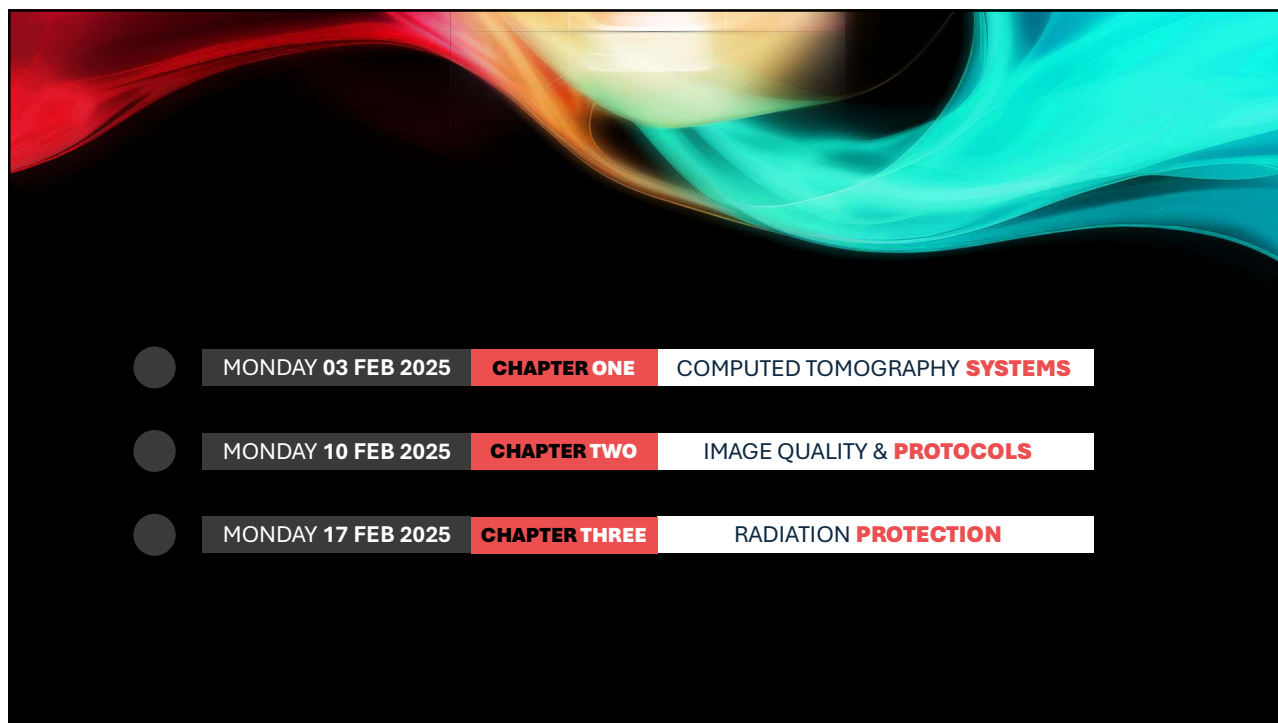
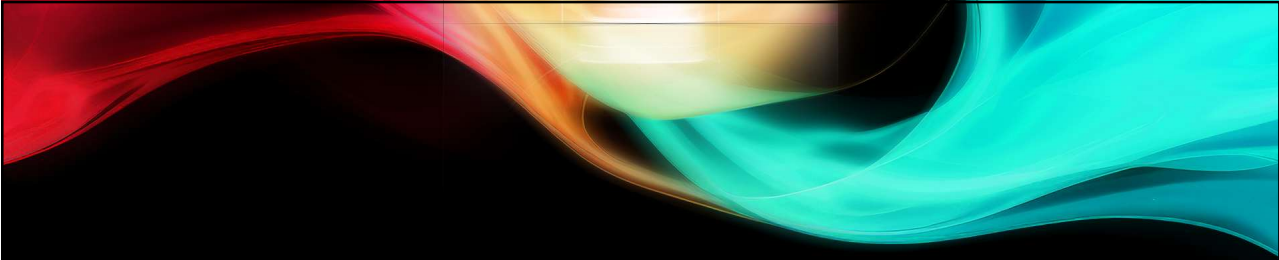





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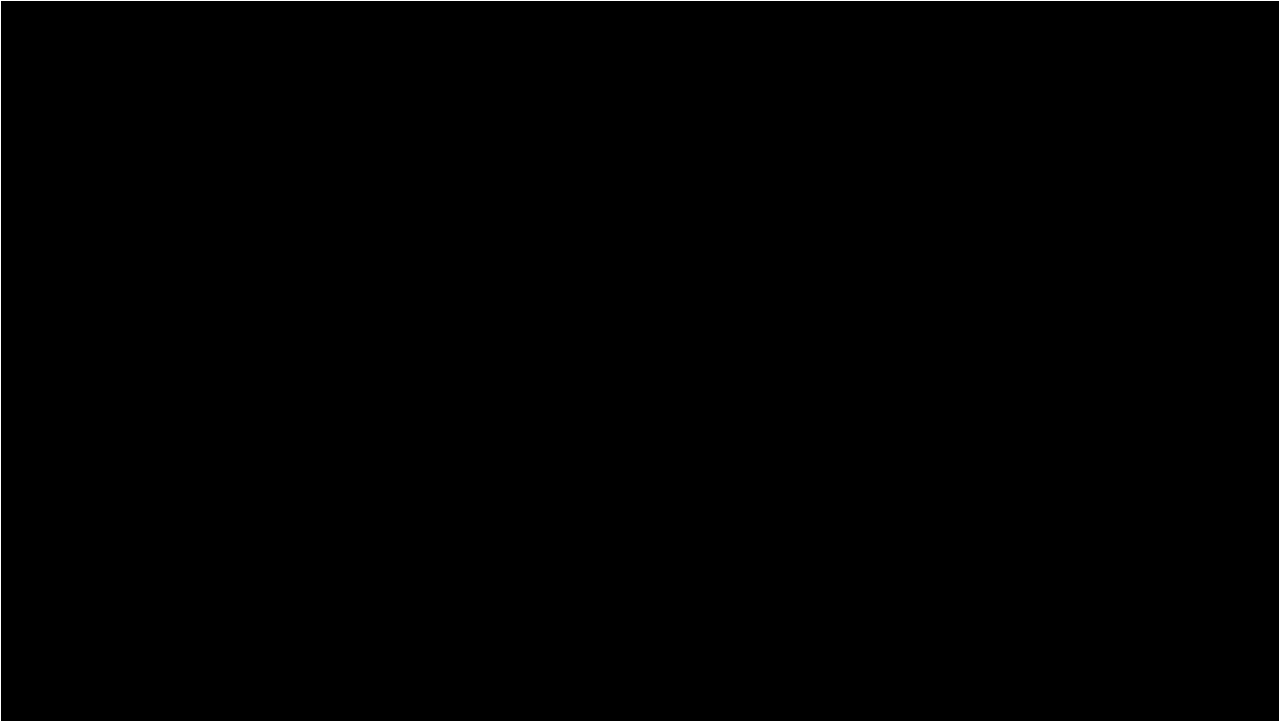


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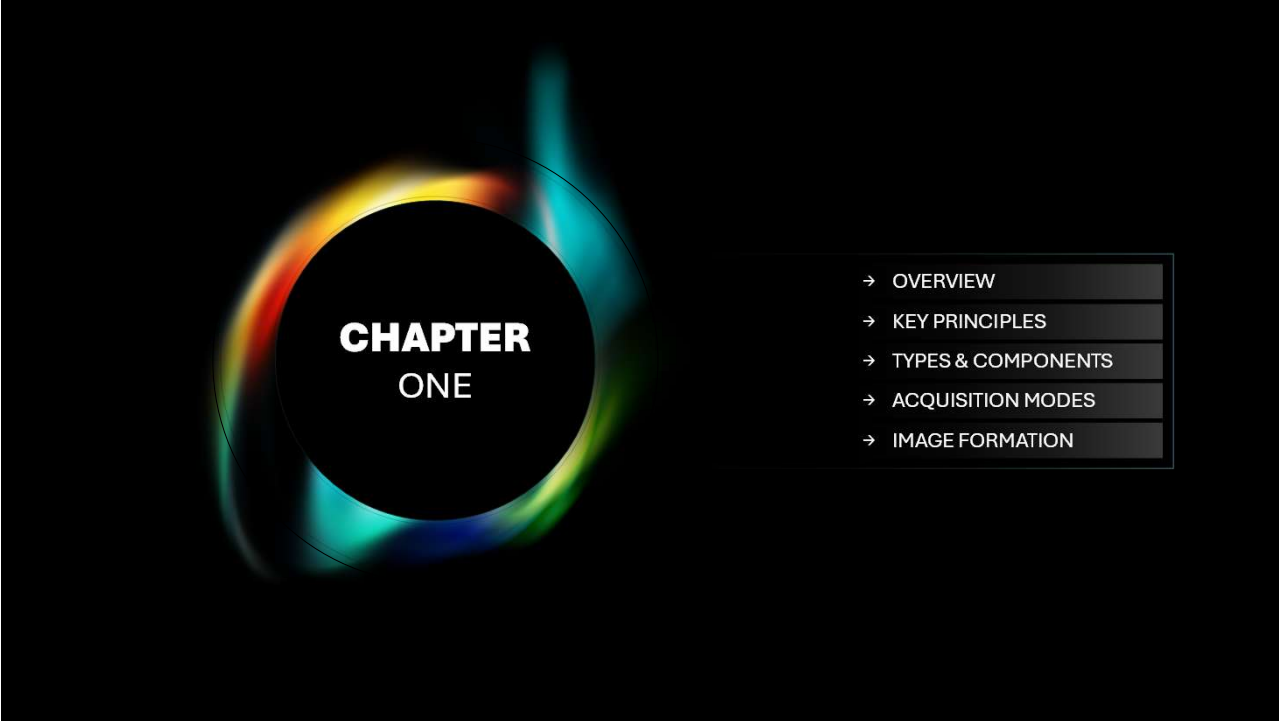


-  **MONDAY 03 FEB 2025** **CHAPTER ONE** COMPUTED TOMOGRAPHY **SYSTEMS**
-  **MONDAY 10 FEB 2025** **CHAPTER TWO** IMAGE QUALITY & **PROTOCOLS**
-  **MONDAY 17 FEB 2025** **CHAPTER THREE** RADIATION **PROTECTION**

4



5



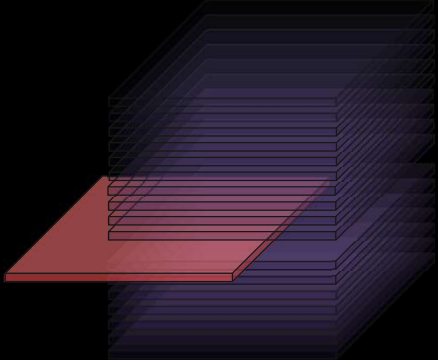
6



7

**COMPUTED TOMOGRAPHY**

Computed Tomography (CT) is a imaging technique that **uses x-rays** to create detailed **cross-sectional images** of the body. It provides significantly more information than traditional 2D radiography.




The diagram shows a stack of numerous thin, horizontal, semi-transparent slices. The top slice is highlighted in a reddish-pink color, while the others are in shades of purple and blue, receding into the distance to represent depth. This visualizes the process of building a 3D volume from multiple 2D cross-sections.

CH.1

8

**COMPUTED TOMOGRAPHY**

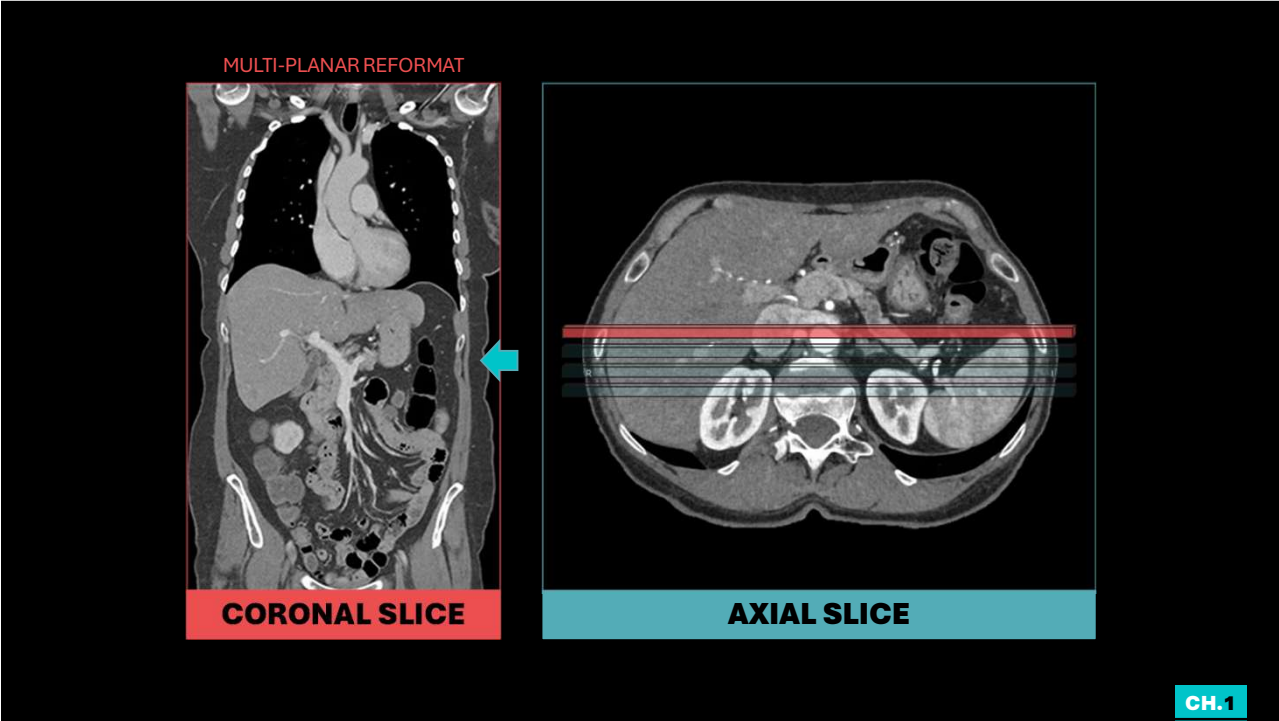
Computed Tomography (CT) is a imaging technique that **uses x-rays** to create detailed **cross-sectional images** of the body. It provides significantly more information than traditional 2D radiography.



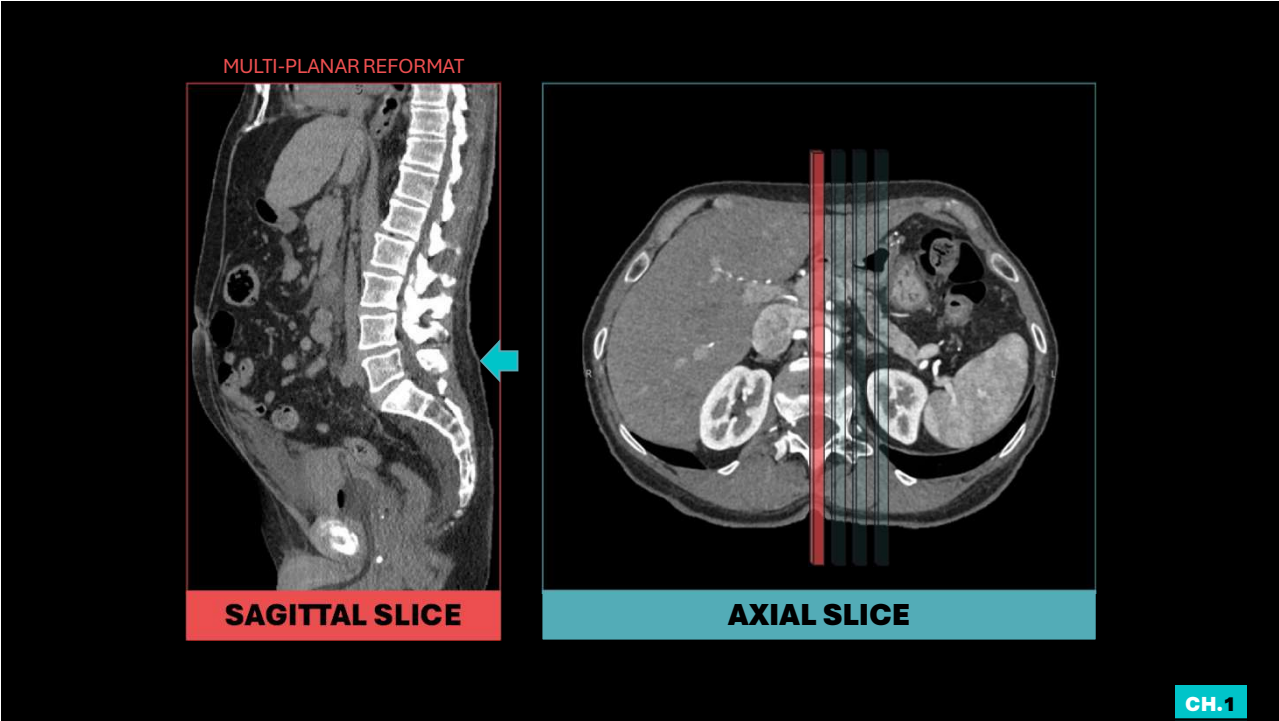
This is a grayscale axial CT scan of the abdomen. It shows a cross-section of the body at the level of the kidneys and the spine. The kidneys are visible as bright, bean-shaped structures on either side of the spine. The liver is on the left side of the image, and the spleen is on the right. The vertebral body is in the center, and the surrounding soft tissue and organs are clearly delineated.

CH.1

9



10




11

## THE IMPACT OF CT

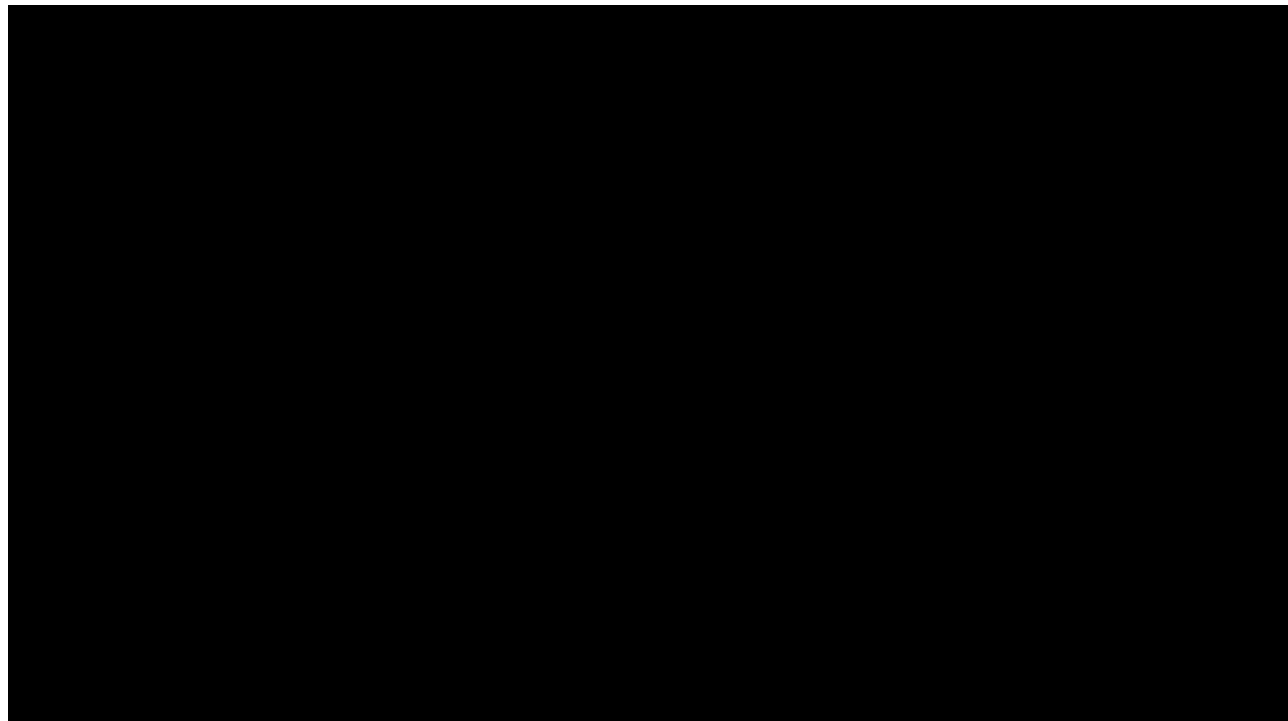
In summary, CT has revolutionized medical imaging by providing a powerful tool for visualizing internal anatomy with exceptional detail and clarity. Its versatility, speed, and ability to differentiate between subtle tissue differences have made it indispensable in modern healthcare, leading to improved diagnosis, treatment, and patient care across numerous medical specialties.

- Improved accuracy of diagnosis
- Minimally invasive
- Enhanced treatment planning
- Better patient outcomes

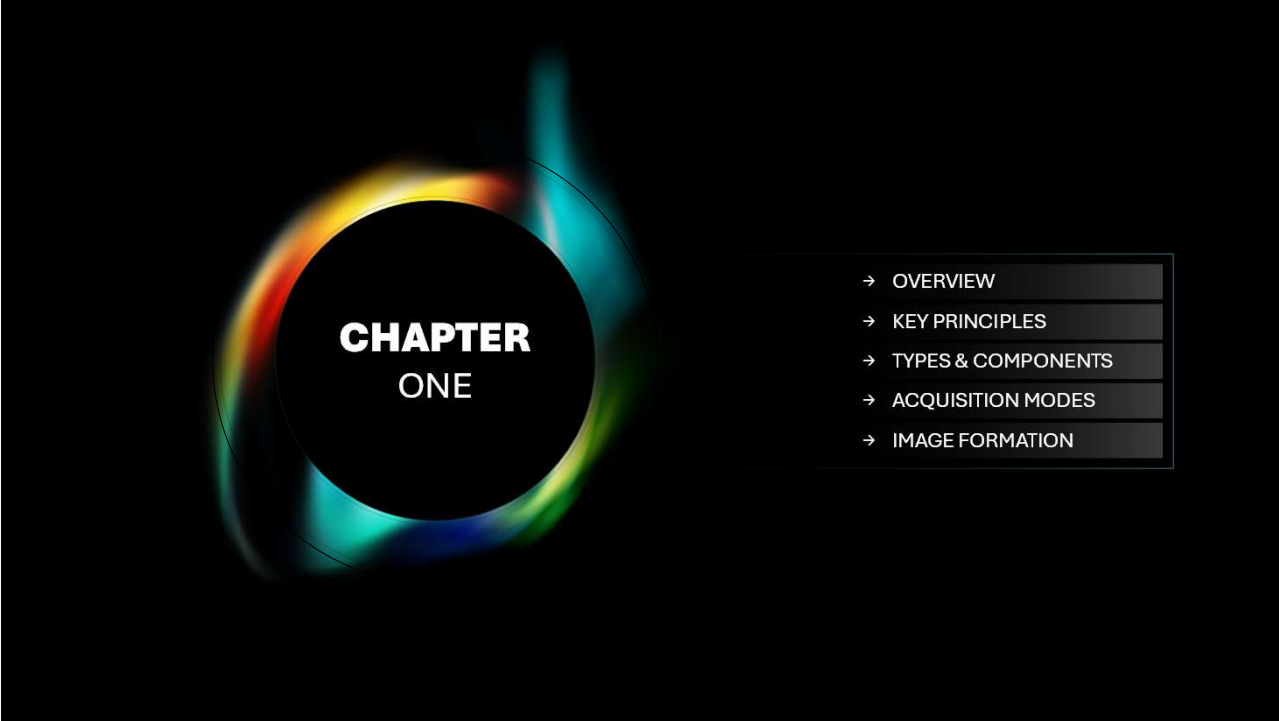


CH.1

12



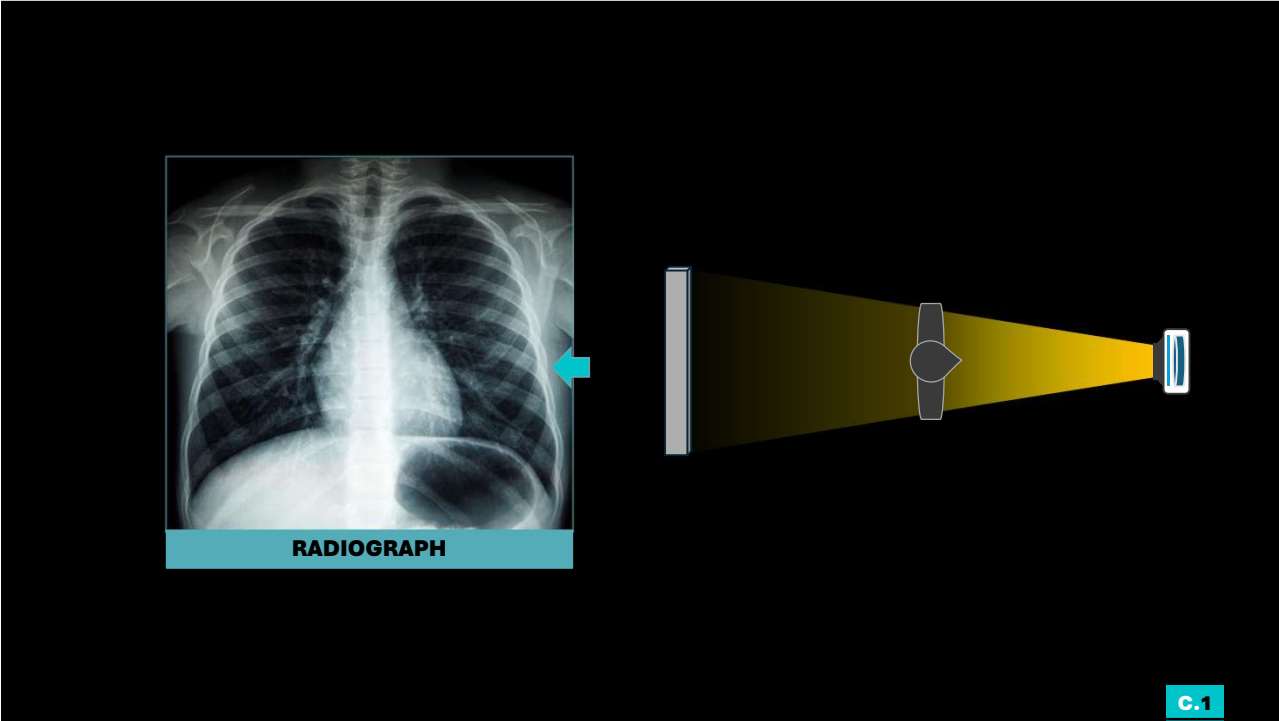
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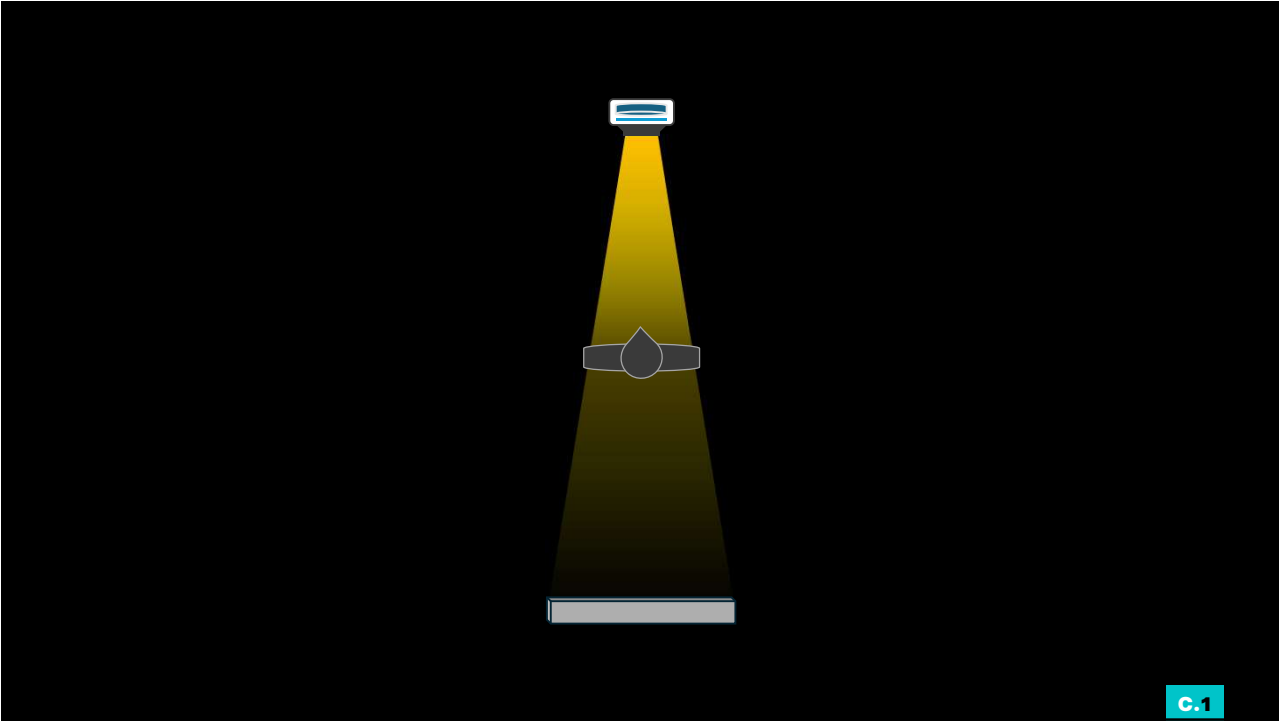
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16



17





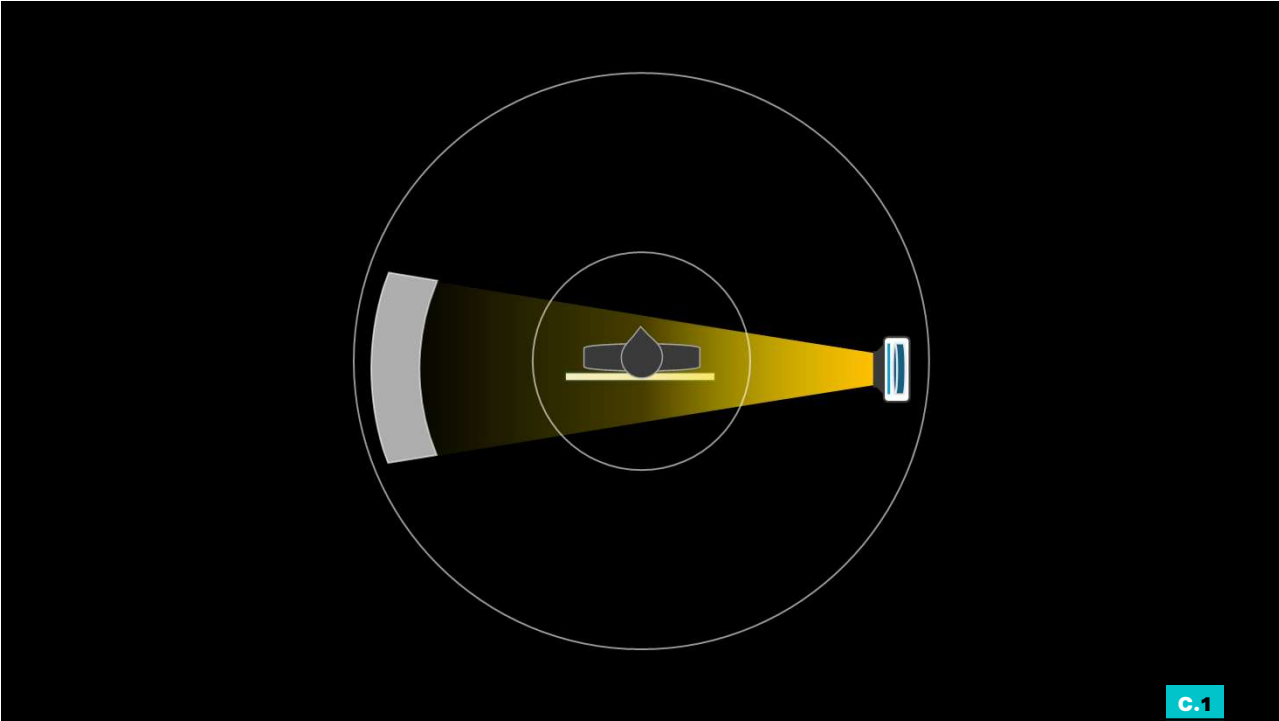
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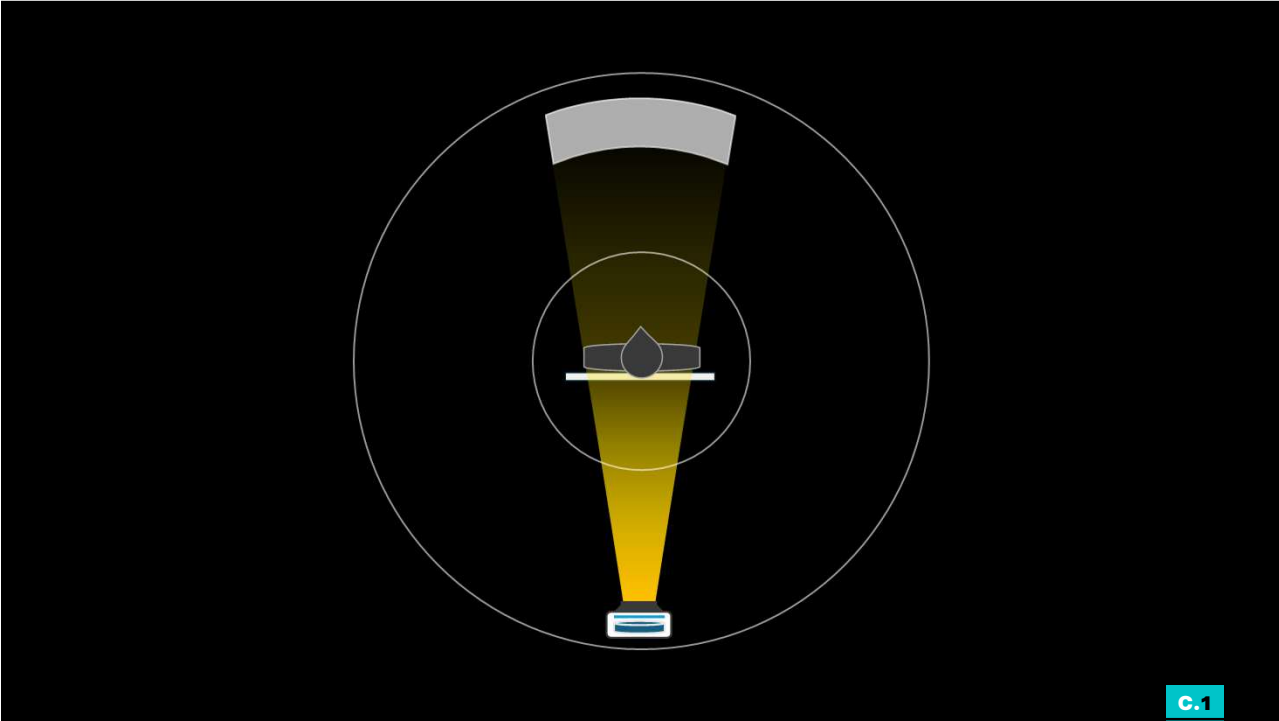
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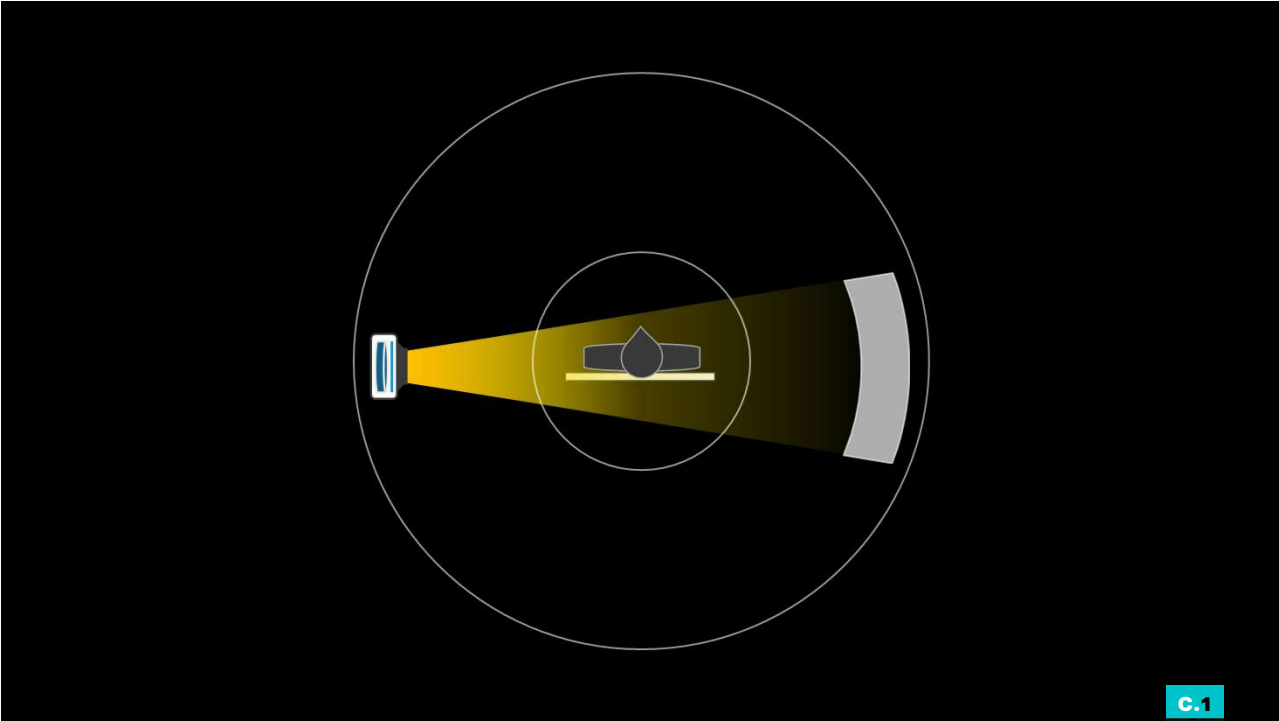
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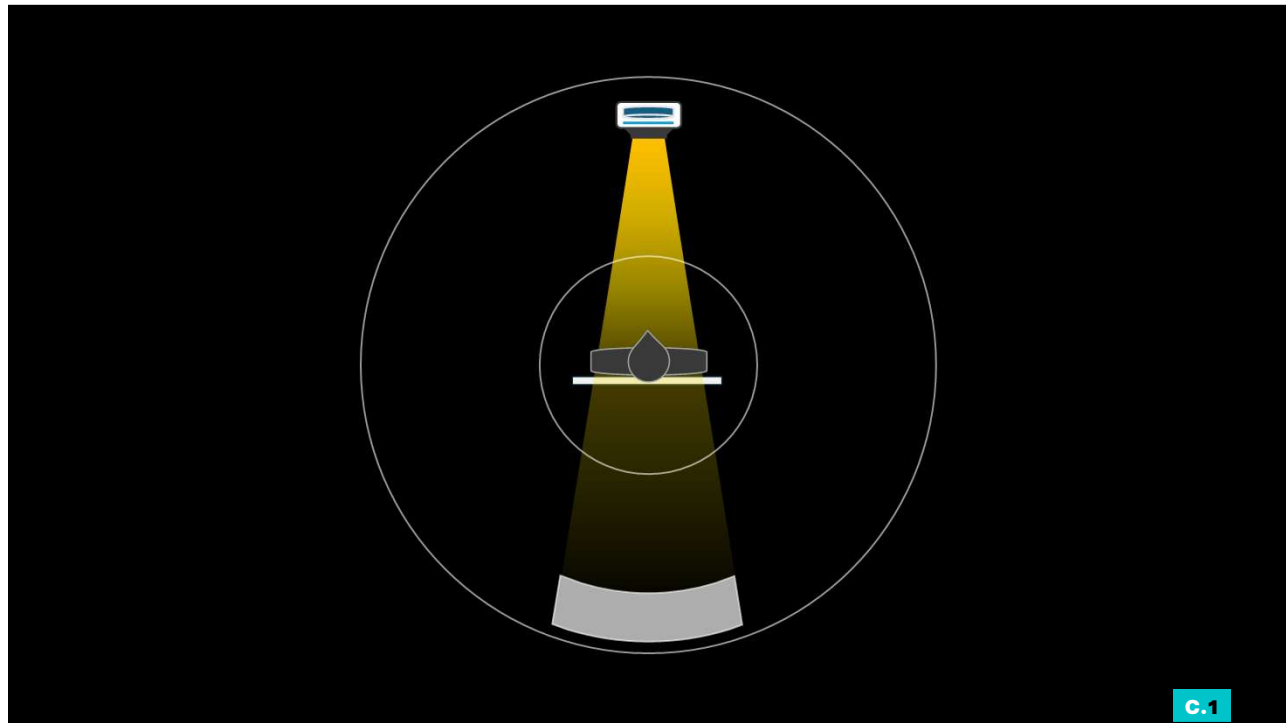
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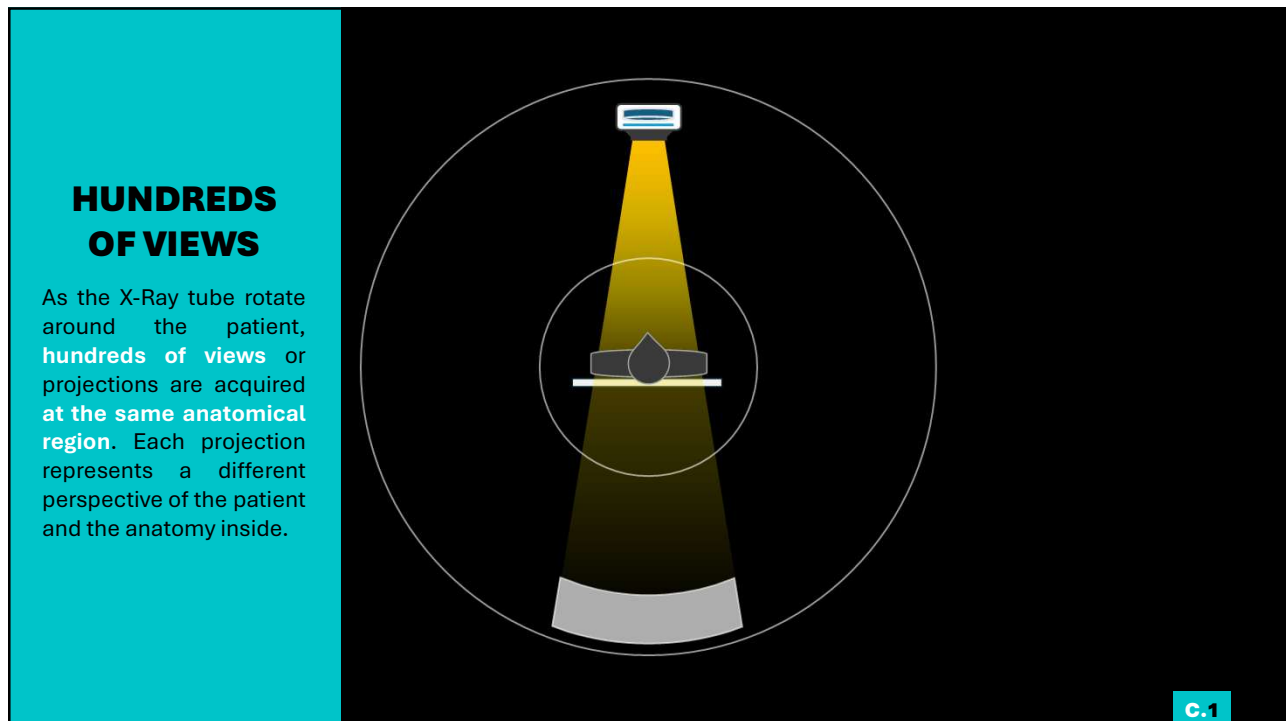
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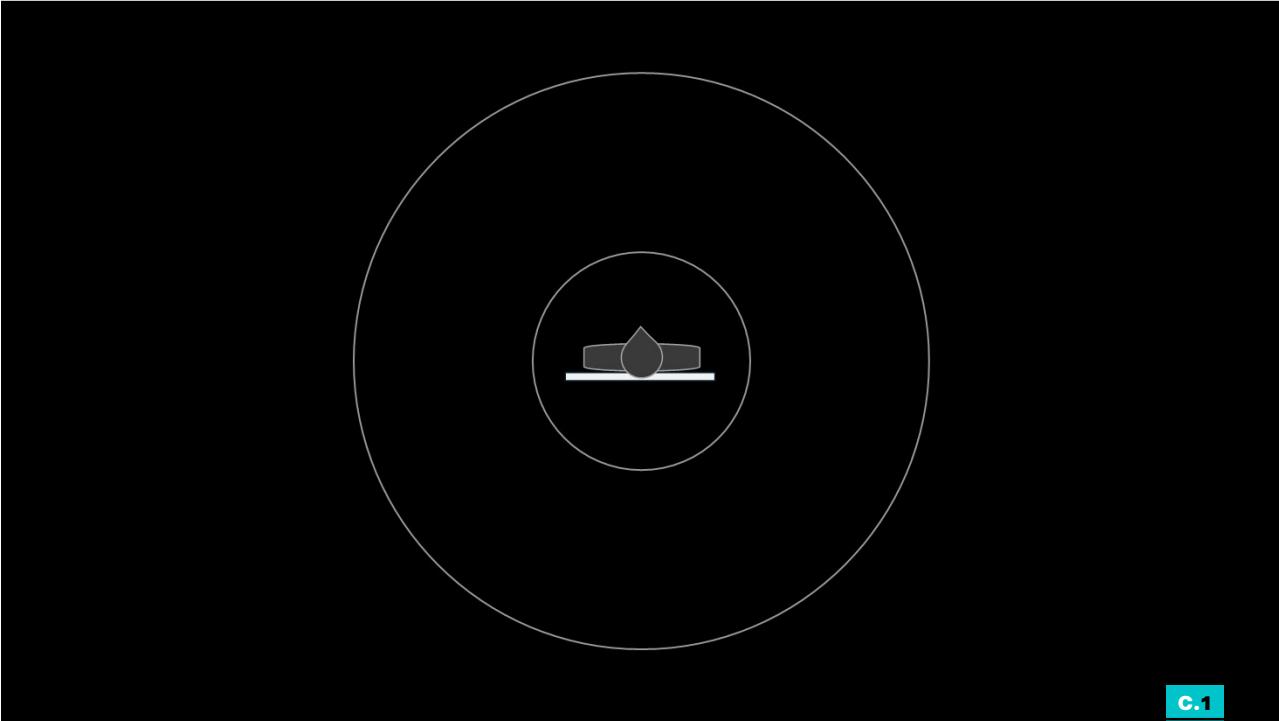
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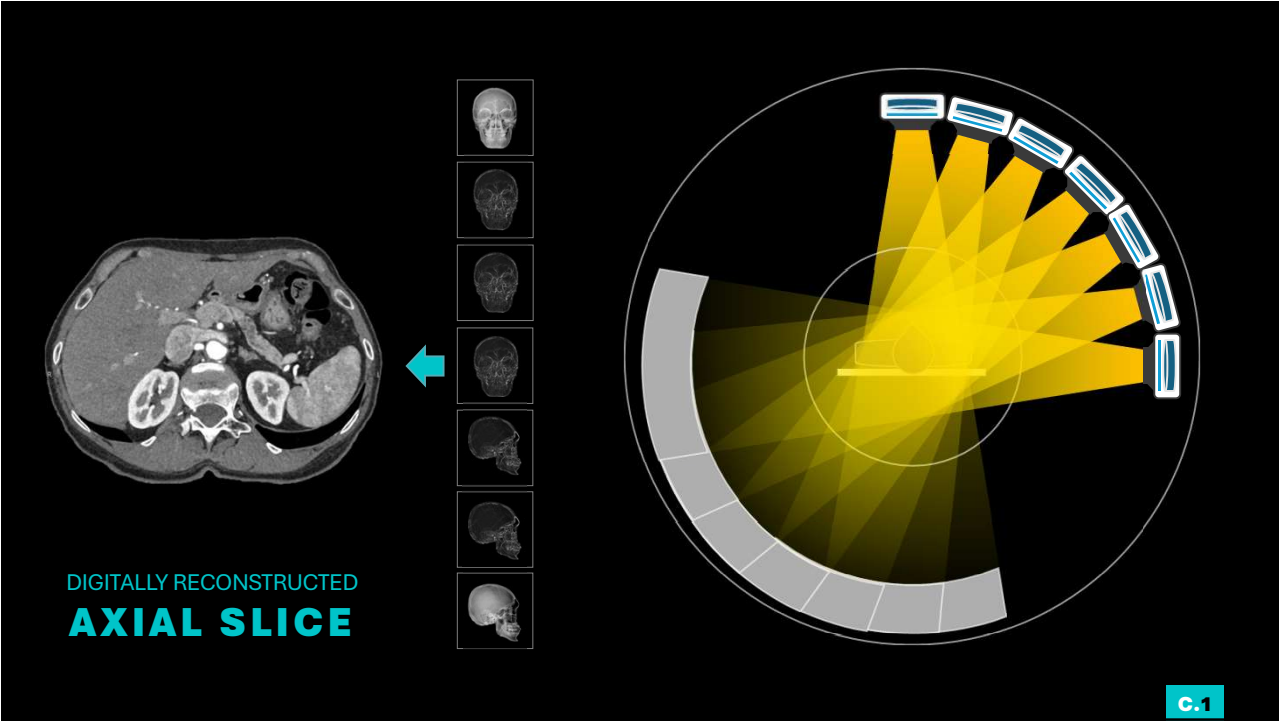


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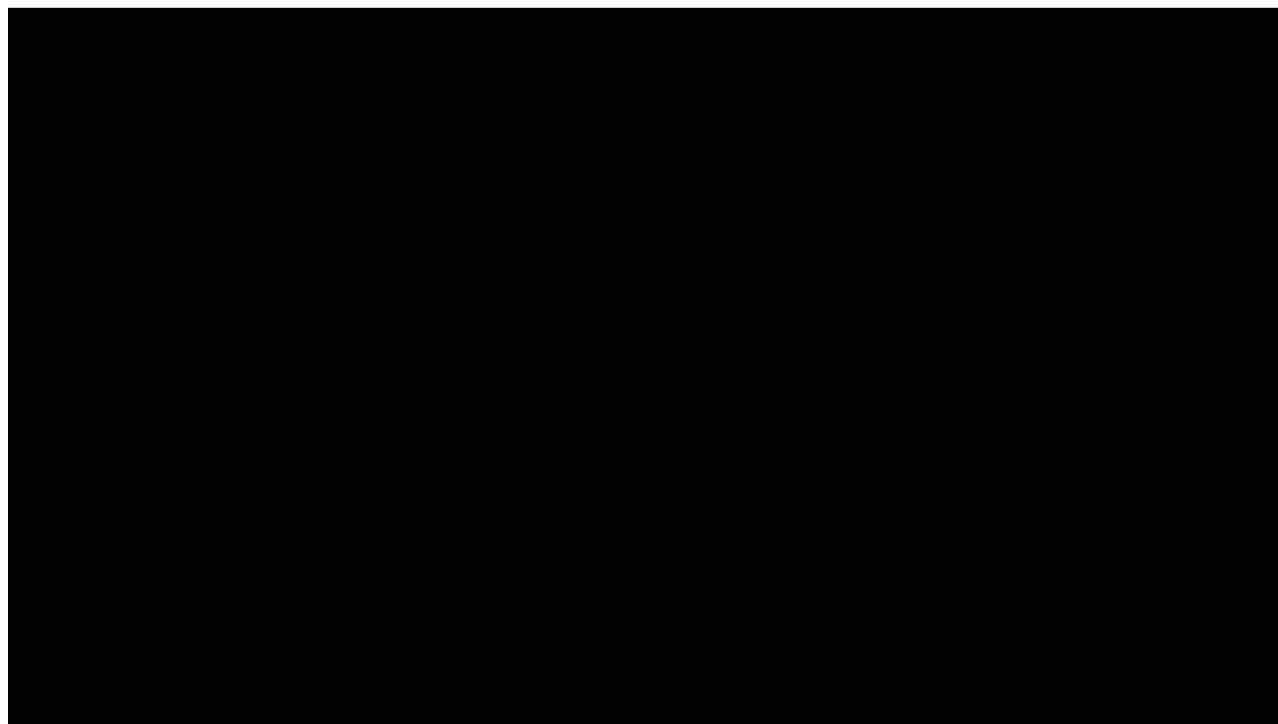
C.1

26

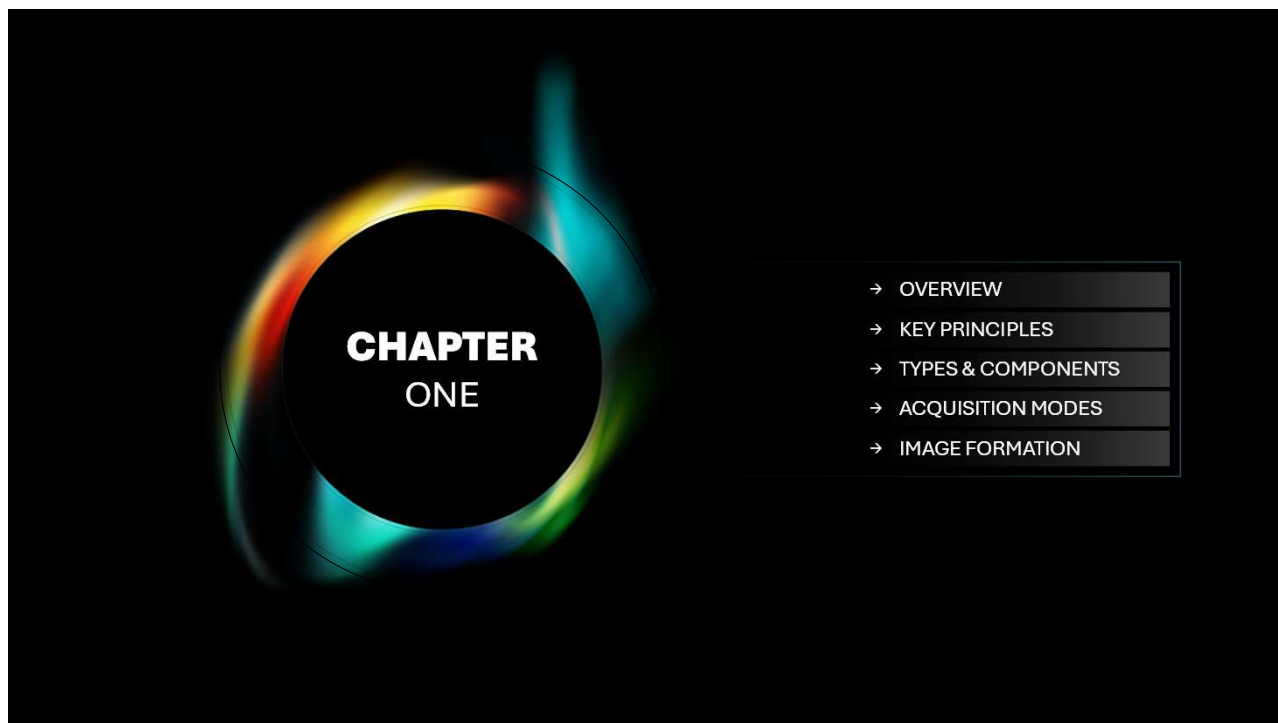


C.1

27



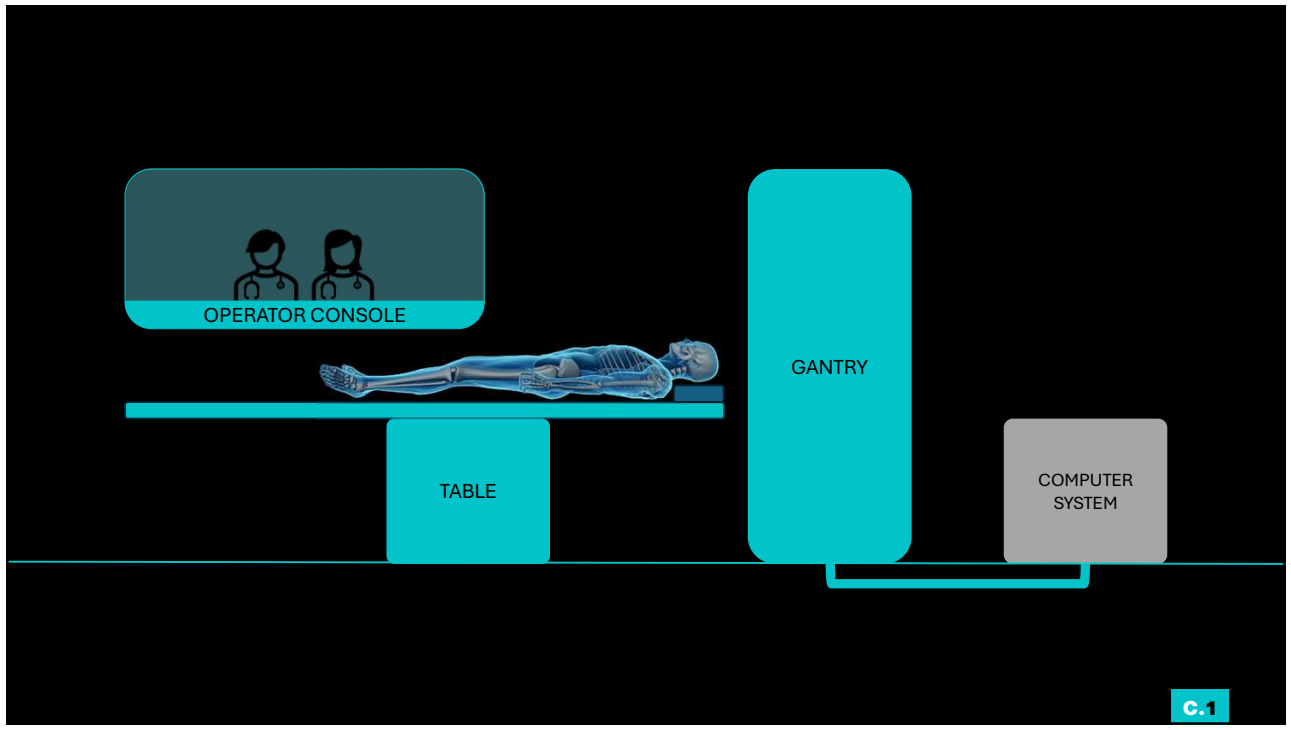
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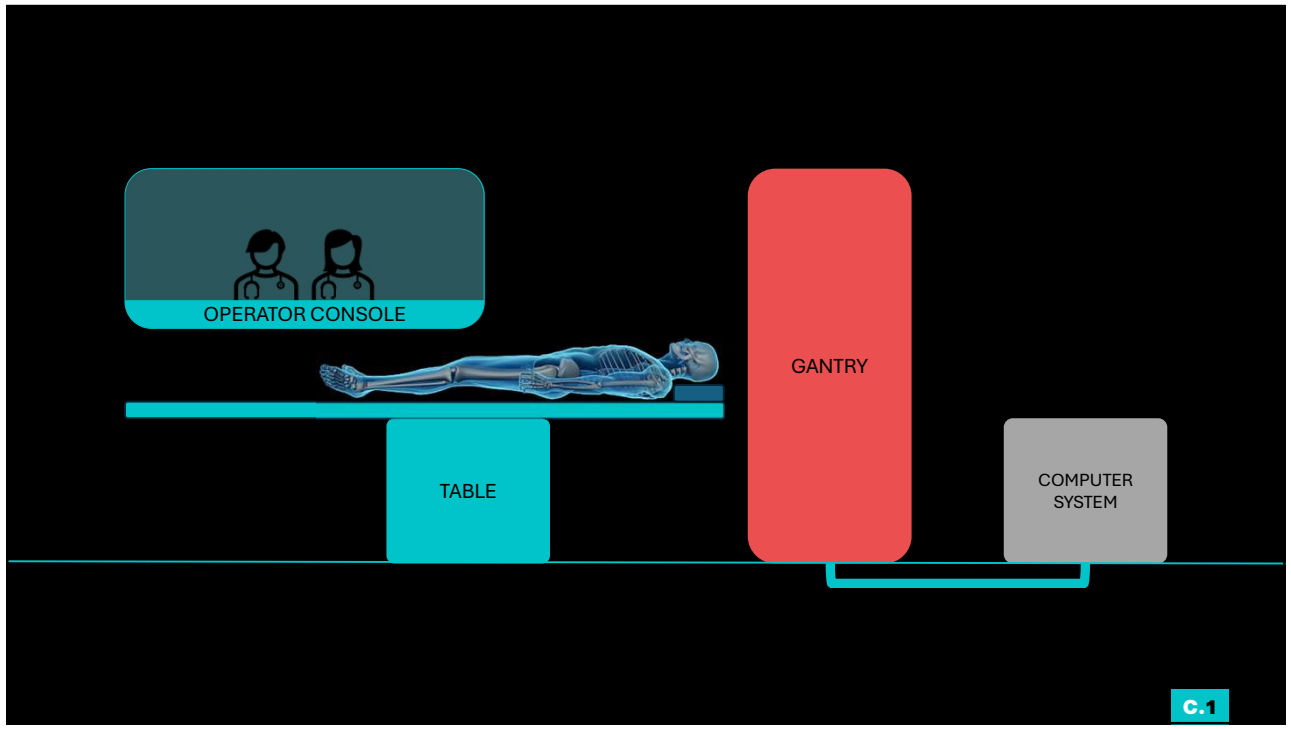
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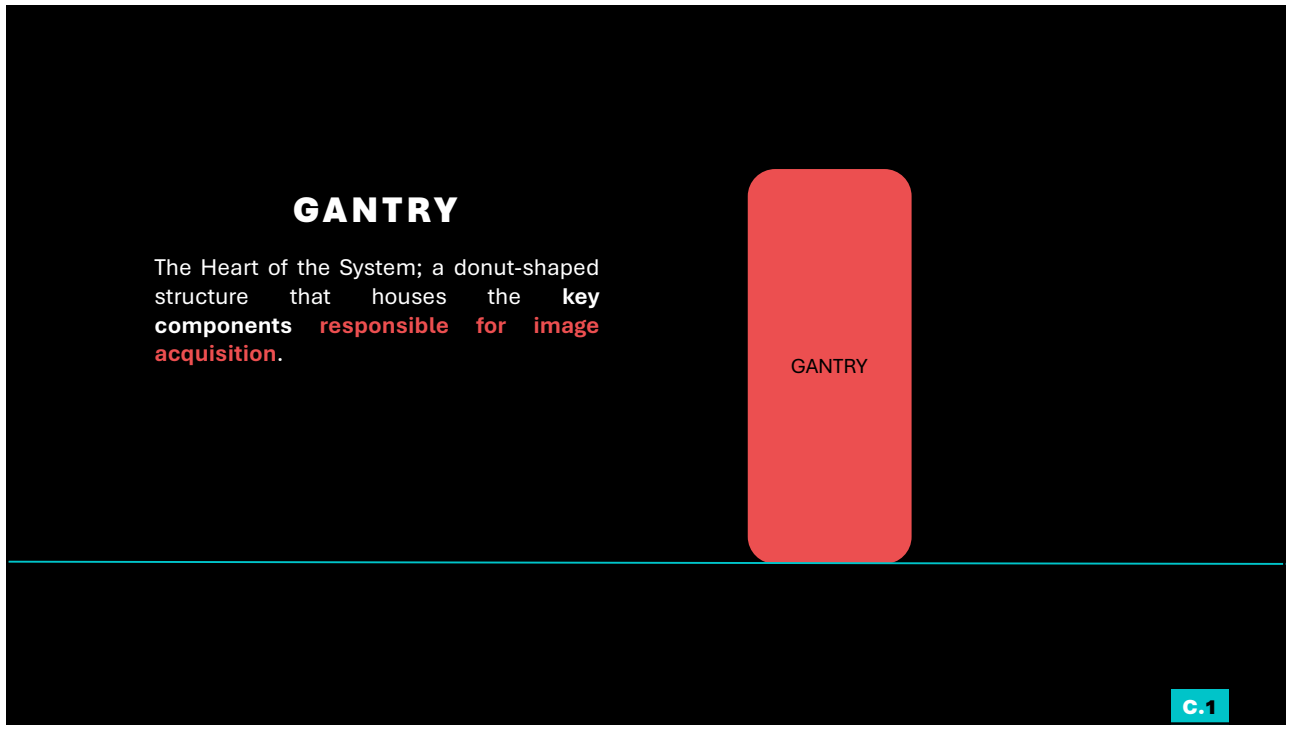
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31

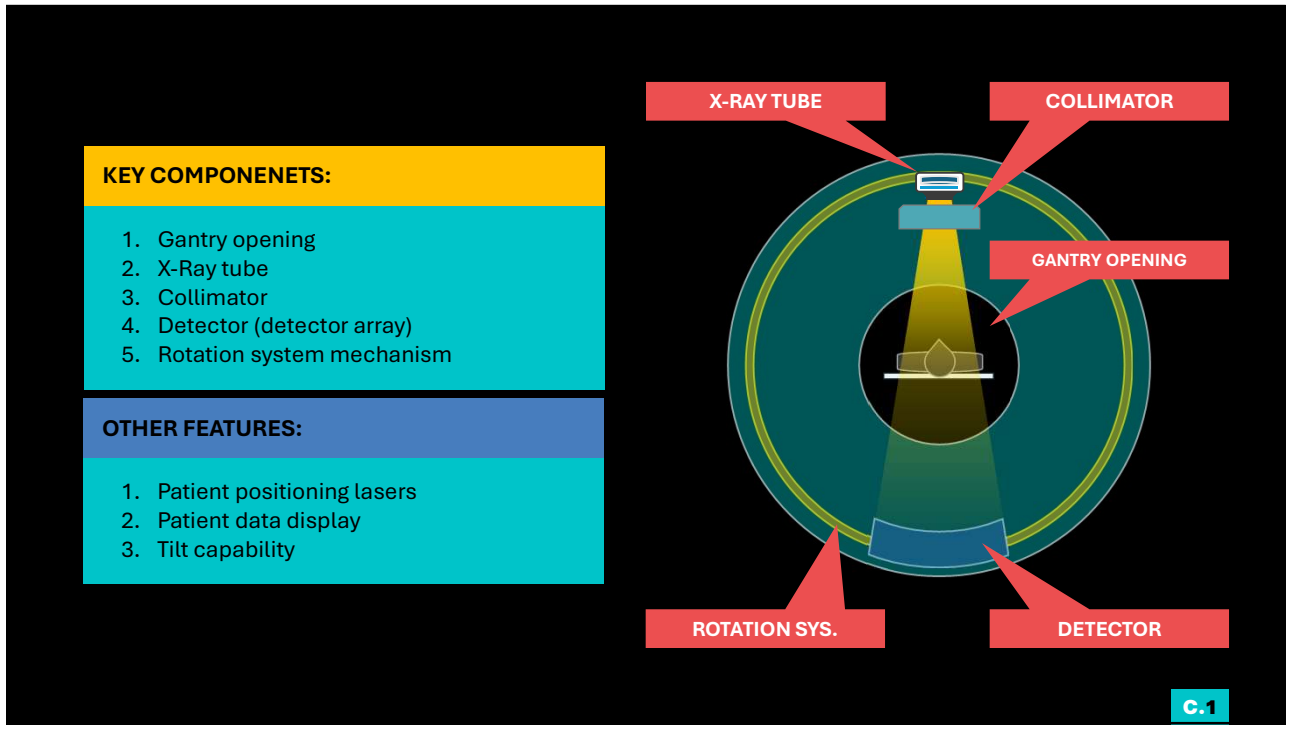


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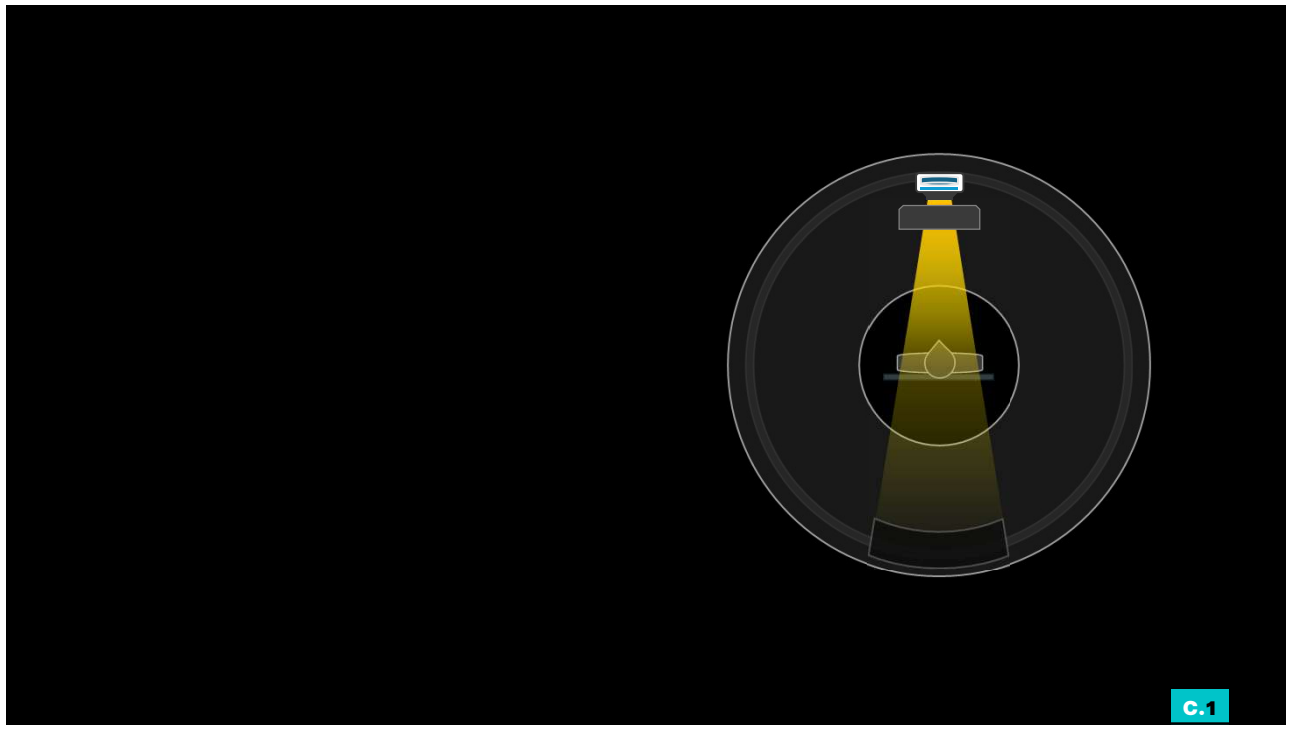


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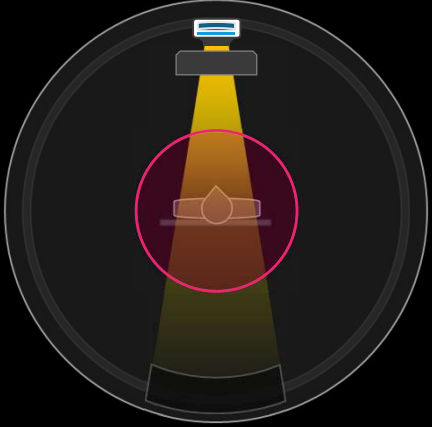
34



35

**GANTRY OPENING**


the size of the gantry opening is crucial. It determines the **maximum allowed patient size** and the maximum possible **scan field of view (SFOV)**



The diagram shows a top-down view of a CT gantry. A yellow cone representing the X-ray beam originates from the top and passes through a patient (represented by a brown shape) positioned on a table. A pink circle highlights the patient's position, and a larger, semi-transparent circle represents the maximum possible scan field of view (SFOV). The gantry opening is the circular area through which the beam and patient pass.

C.1

36




This diagram is similar to the one on slide 36, showing a top-down view of a CT gantry. A yellow cone representing the X-ray beam originates from the top and passes through a patient (represented by a brown shape) positioned on a table. A white circle highlights the patient's position, and a larger, semi-transparent circle represents the maximum possible scan field of view (SFOV). The gantry opening is the circular area through which the beam and patient pass.

C.1

37


### X-RAY TUBE

the CT X-Ray tube is similar to the one used in general radiography in principle. However, it differs in performance greatly. CT X-Ray tubes have **substantially higher heat capacity** to allow them to tolerate the higher mA values and longer exposure times necessary for CT procedures.



C.1

38



C.1

39

### COLLIMATORS

Beam limiting device responsible for adjusting the width of the beam. Adjusting the width in:

- **X-Y-Axis:** affects the scan field of view (SFOV)
- **Z-axis:** affects the patient coverage per rotation

40

**SFOV SIZES**

SMALL

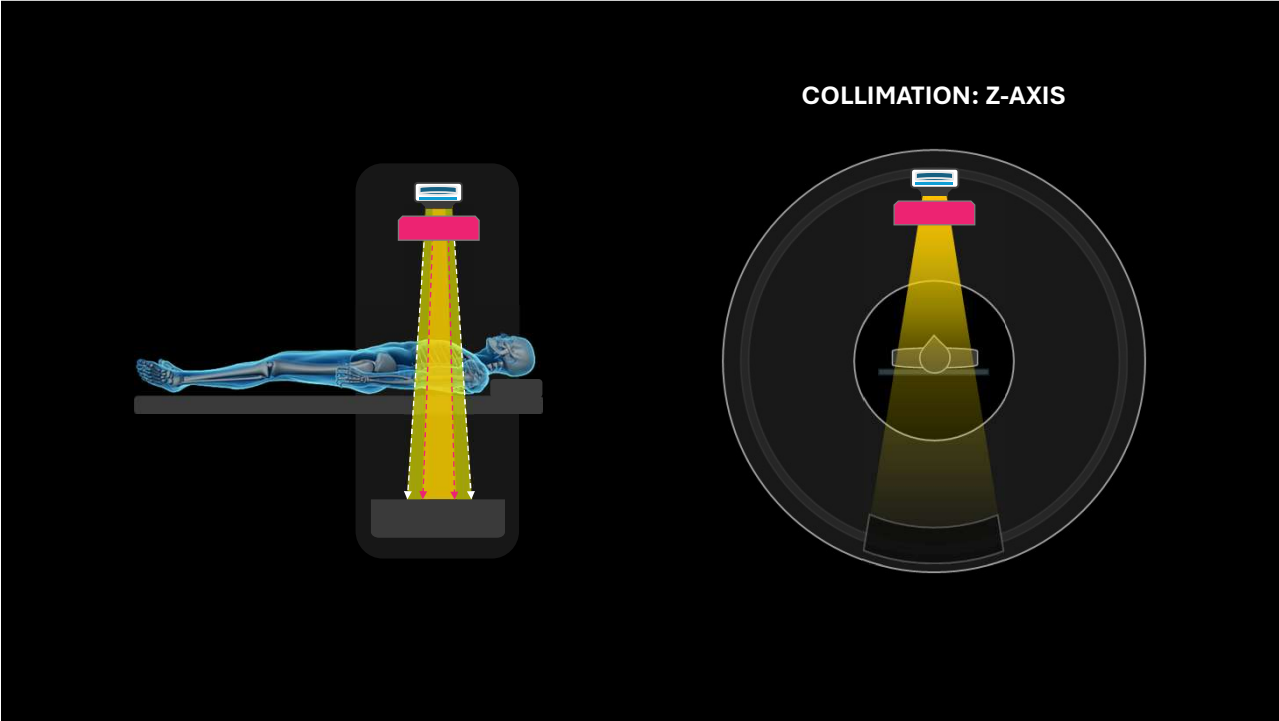
MEDIUM

LARGE

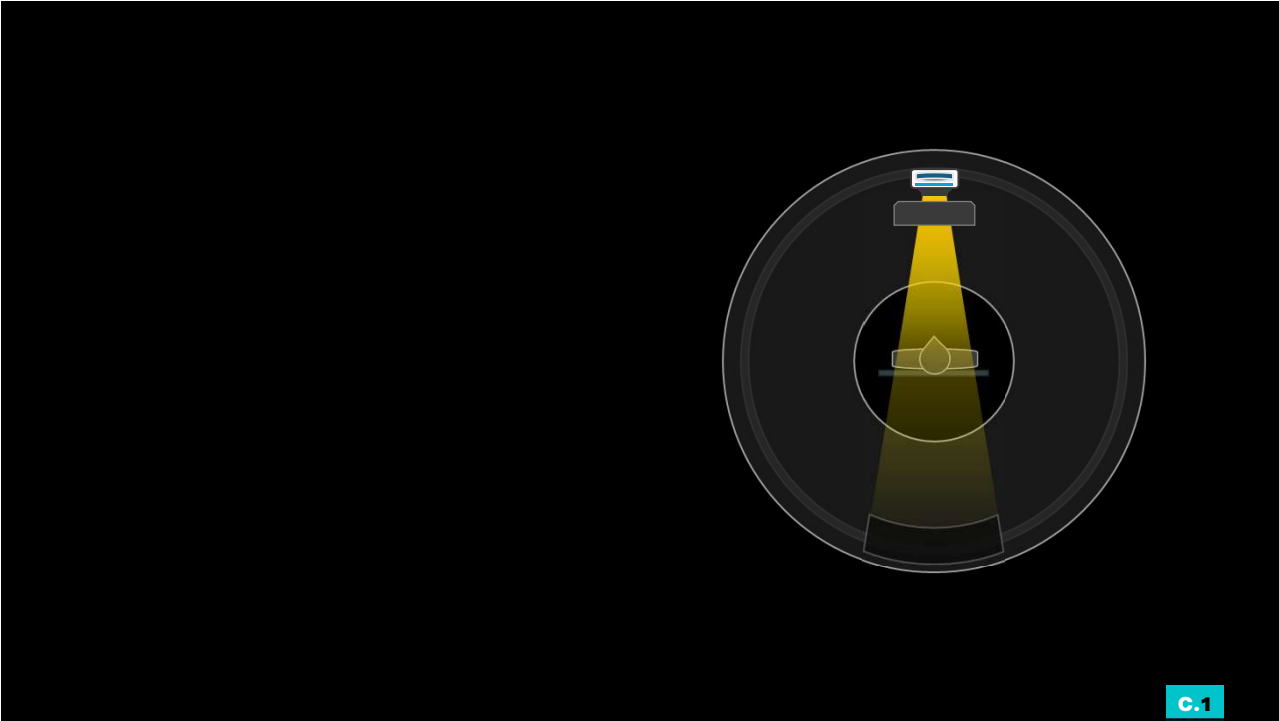
#### COLLIMATION: X-Y-AXIS

The largest possible SFOV is limited by the gantry opening size and length of the detector

41



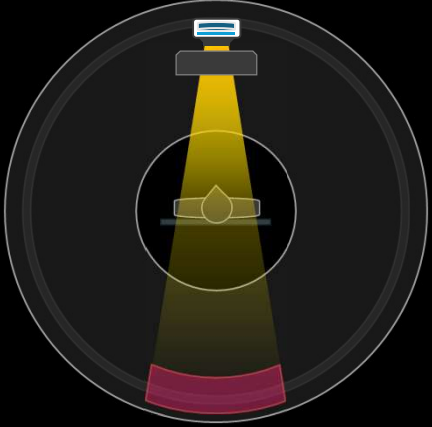
42



43

**DETECTOR**

One of most important parts of the CT scanner (if not the most important!). The detector is responsible for many of the performance characteristics of the scanner.




C.1

44

**DETECTOR**

One of most important parts of the CT scanner (if not the most important!). The detector is responsible for many of the performance characteristics of the scanner.

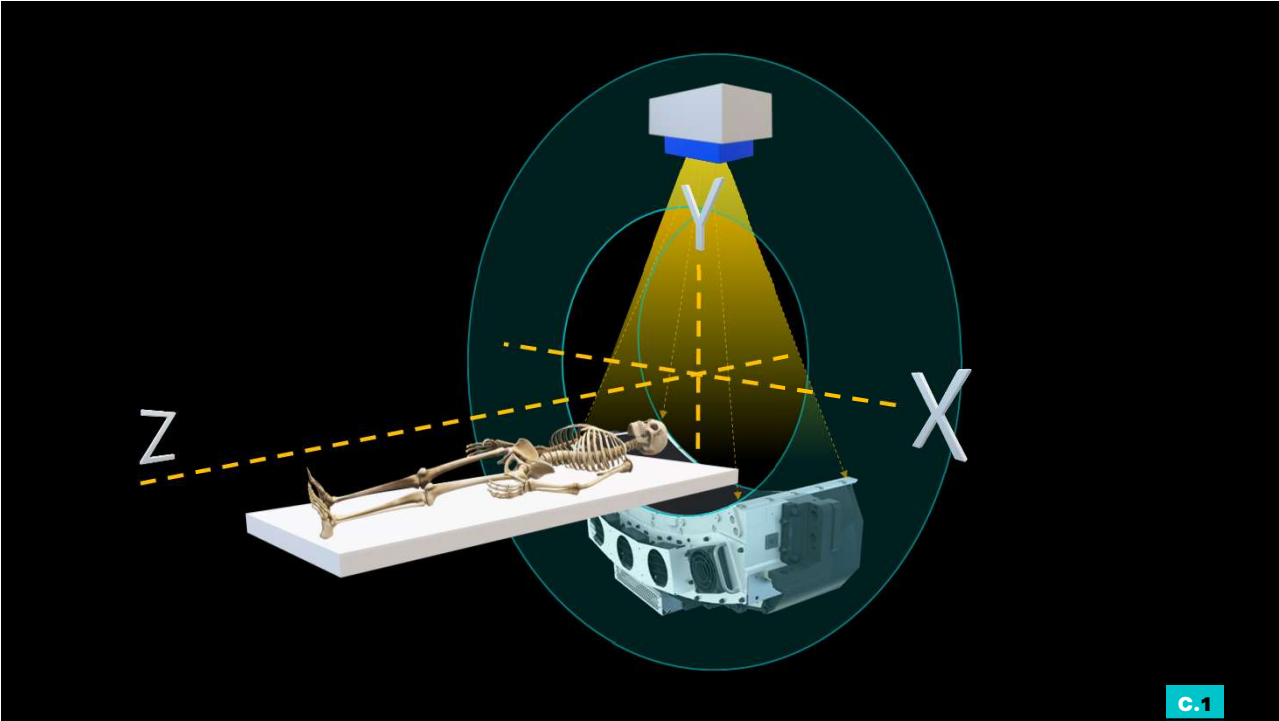


C.1

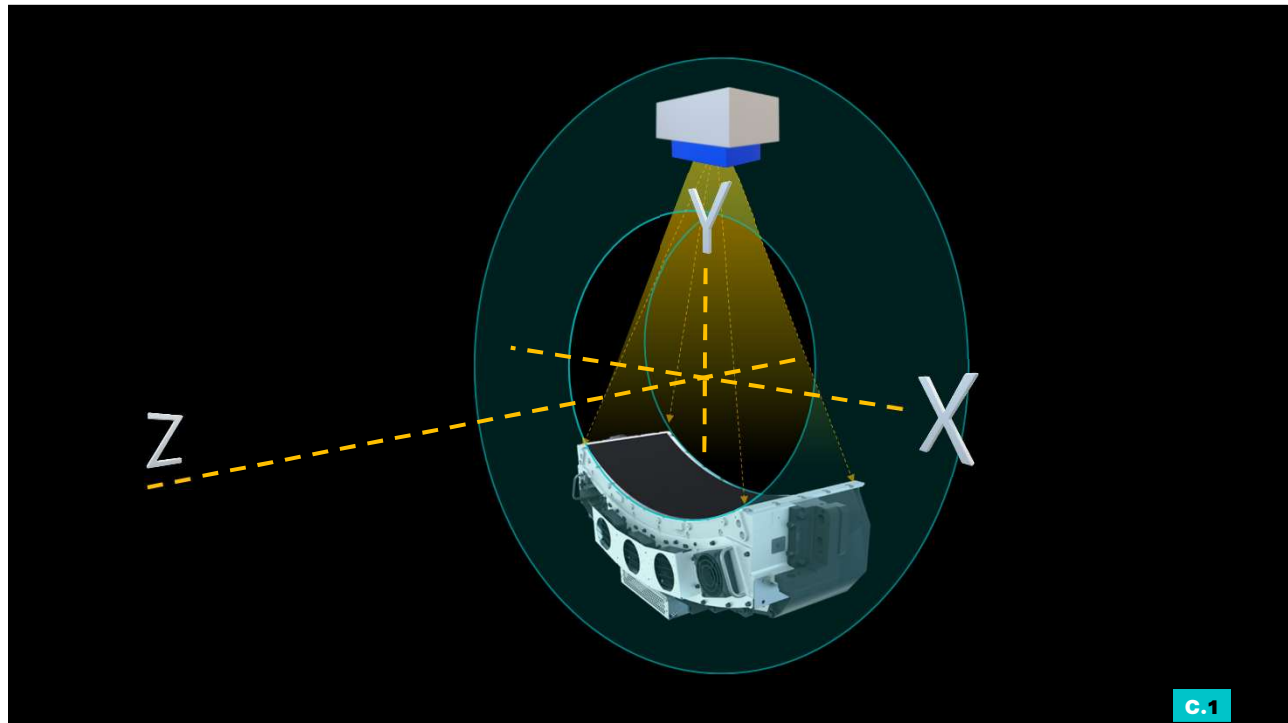
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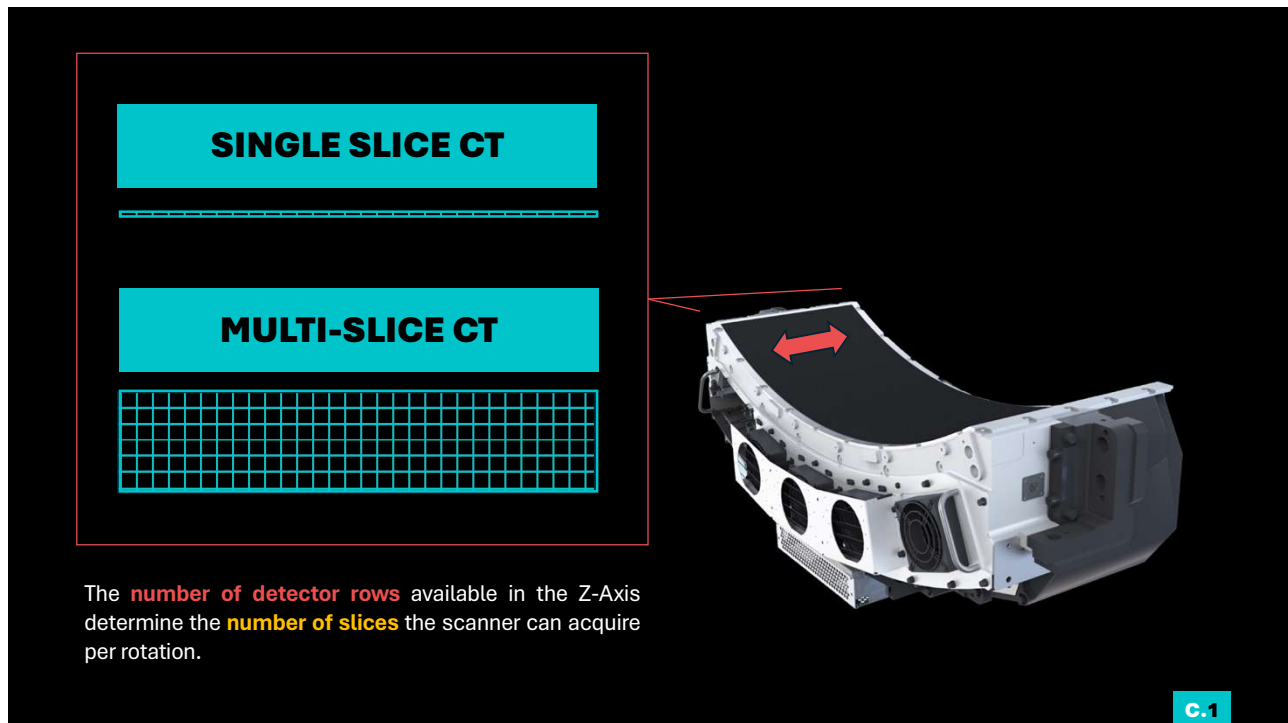
46



47



48



The **number of detector rows** available in the Z-Axis determine the **number of slices** the scanner can acquire per rotation.

49



CELL (DETECTOR ELEMENT) SIZE

NUMBER OF DETECTOR ELEMENTS

The **cell size** in the detector array determines the **minimum slice thickness possible** during an acquisition. While the **number of elements** within a slice determines **X-Y-Axis spatial resolution**.

C.1

50

The **number of detector rows and their size** (Detector width along the Z-Axis) also determines the amount of patient coverage possible for every rotation.

C.1

51

The number of detector rows and their size (Detector width along the Z-Axis) also determines the amount of patient coverage possible for every rotation.

**64 Row (slice) detector with 0.625mm cell size has Z-Axis coverage of  $(64 \times 0.625\text{mm}) = 40\text{mm}$**

**320 Row (slice) detector with 0.5mm cell size has Z-Axis coverage of  $(320 \times 0.5\text{mm}) = 160\text{mm}$**

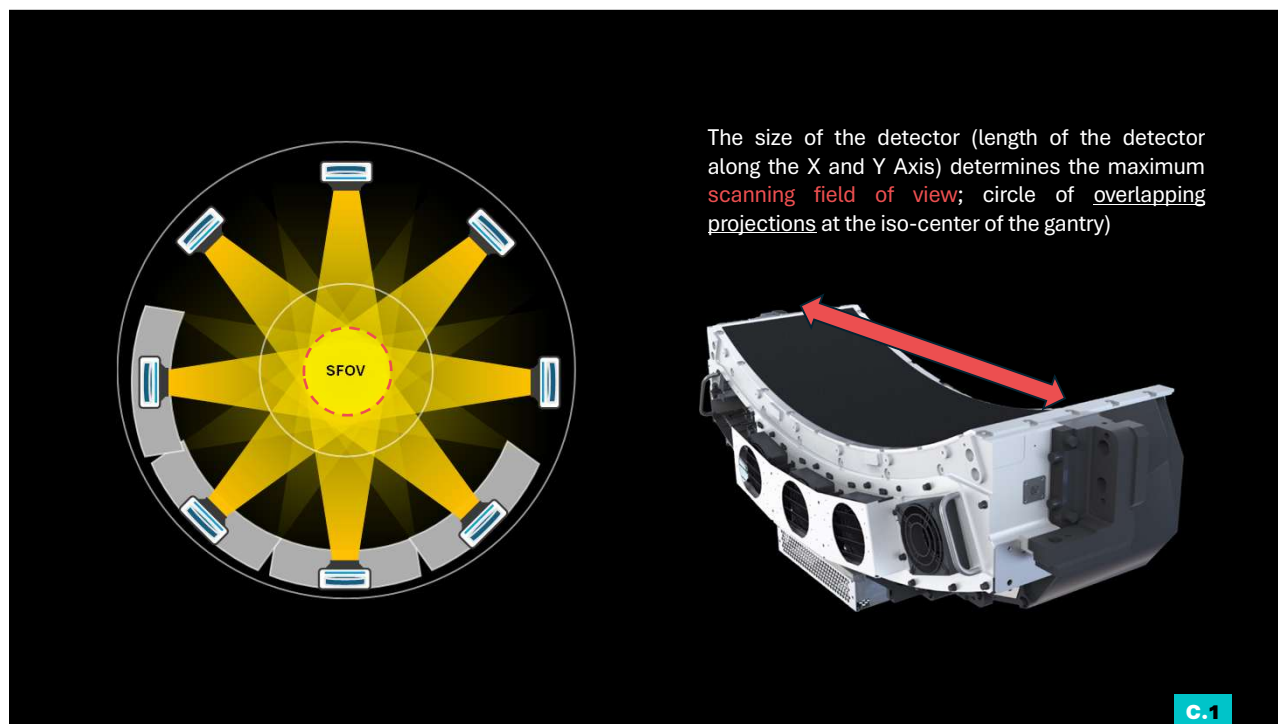
**C.1**

52

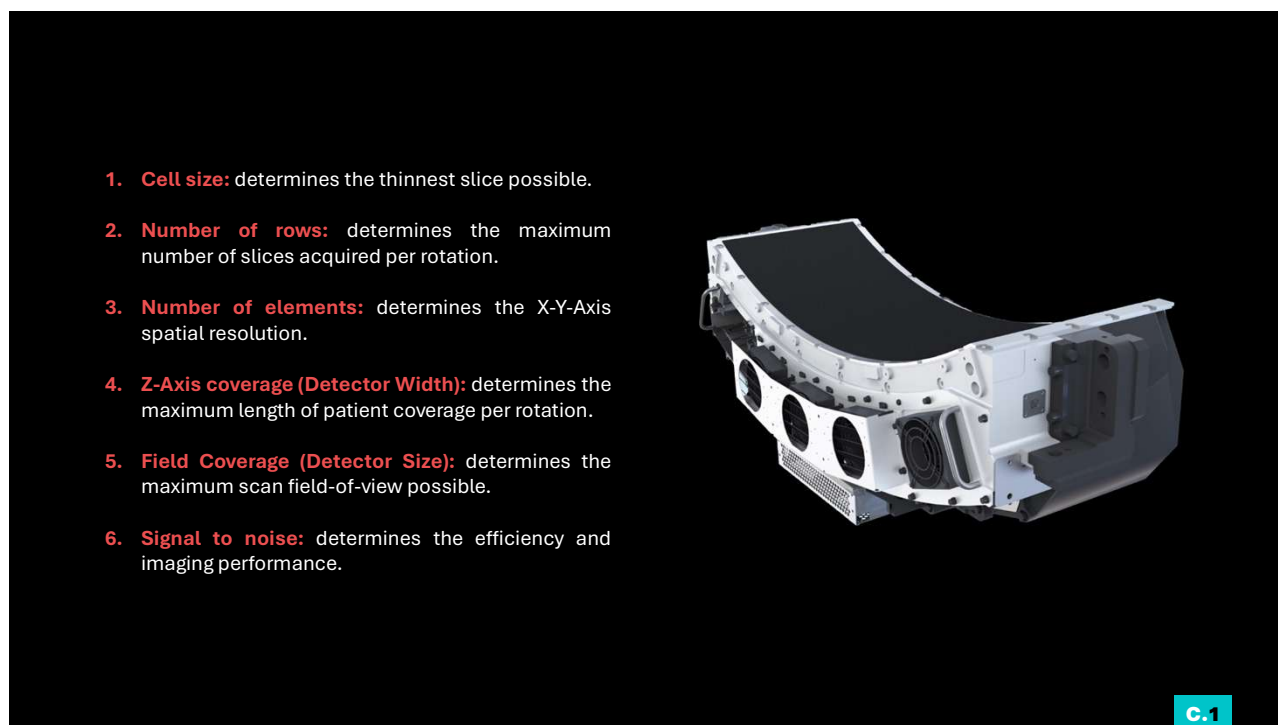
The size of the detector (length of the detector along the X and Y Axis) determines the maximum scanning field of view; circle of overlapping projections at the iso-center of the gantry)

**C.1**

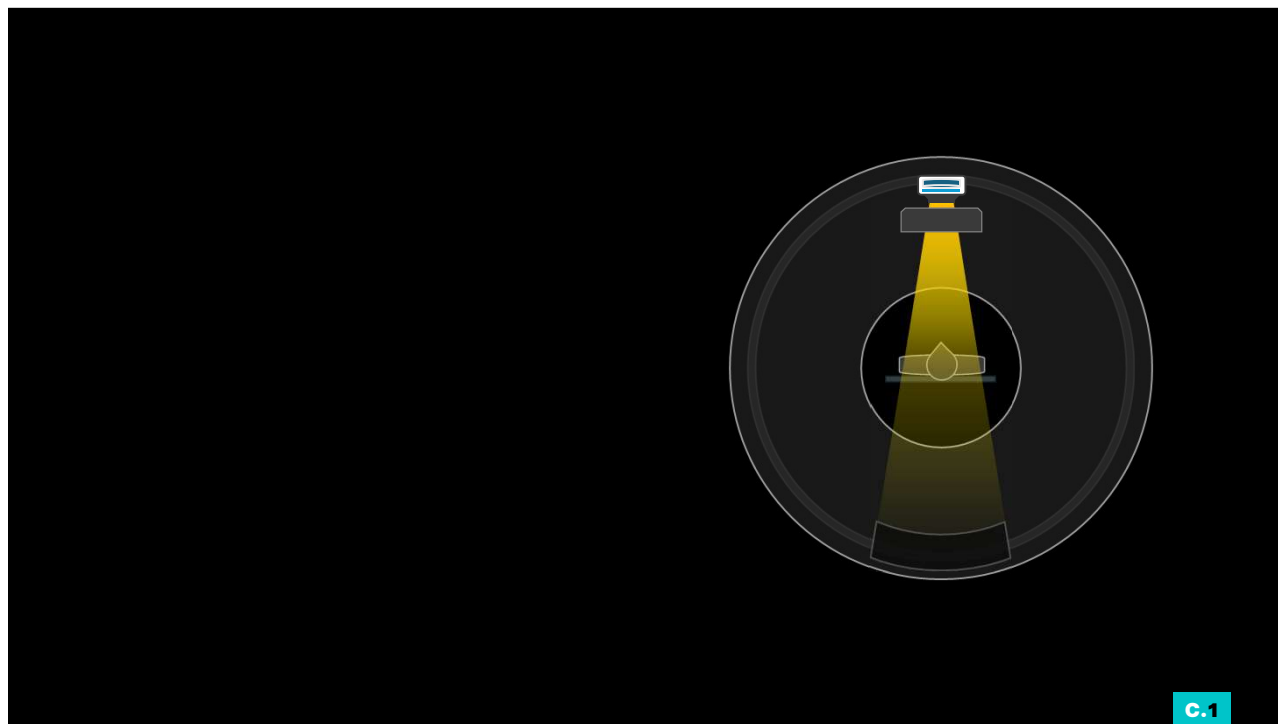
53



54



55



56

**ROTATION SYS.**

The rotation mechanism is responsible for how fast the CT scanner can complete an acquisition. It is generally referred to as “Rotation Speed”. It describes the **time it takes the X-Ray tube & Detector to complete one full rotation around the patient.**

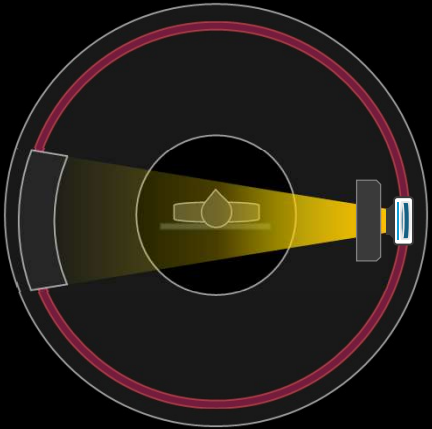
Responsible for the scanner’s  
**“TEMPORAL RESOLUTION”**

57

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Responsible for the scanner’s  
**“TEMPORAL RESOLUTION”**

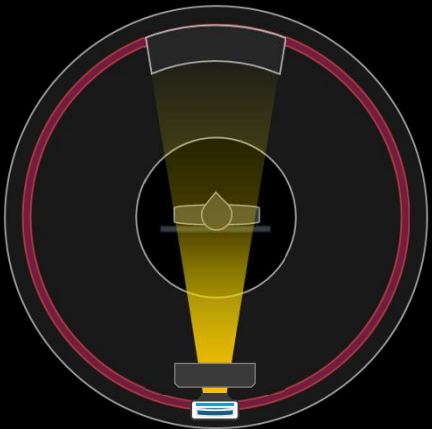


58

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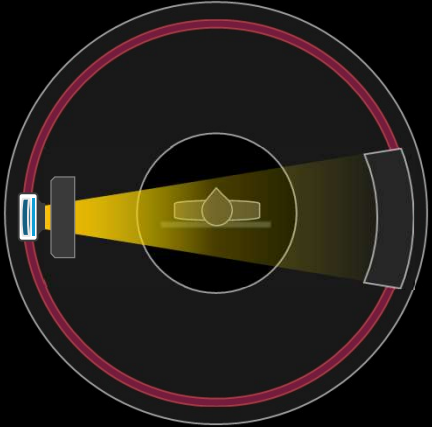
Responsible for the scanner’s  
**“TEMPORAL RESOLUTION”**



59

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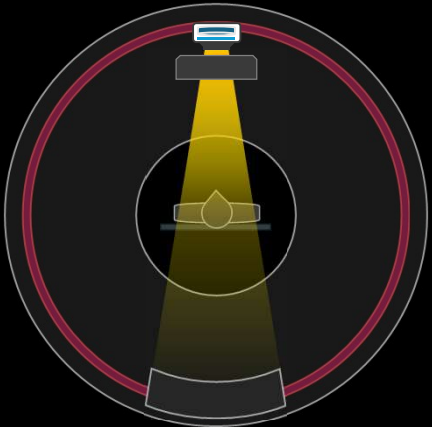


Responsible for the scanner's  
**"TEMPORAL RESOLUTION"**

60

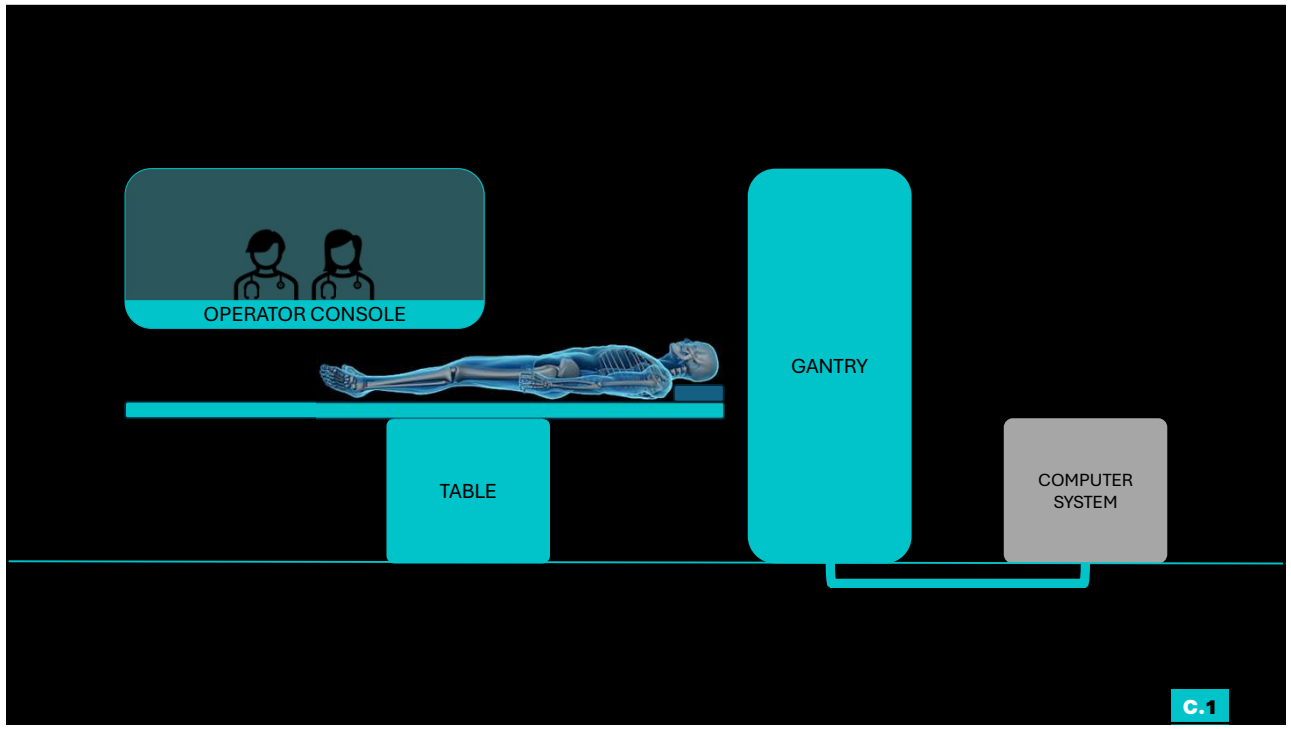
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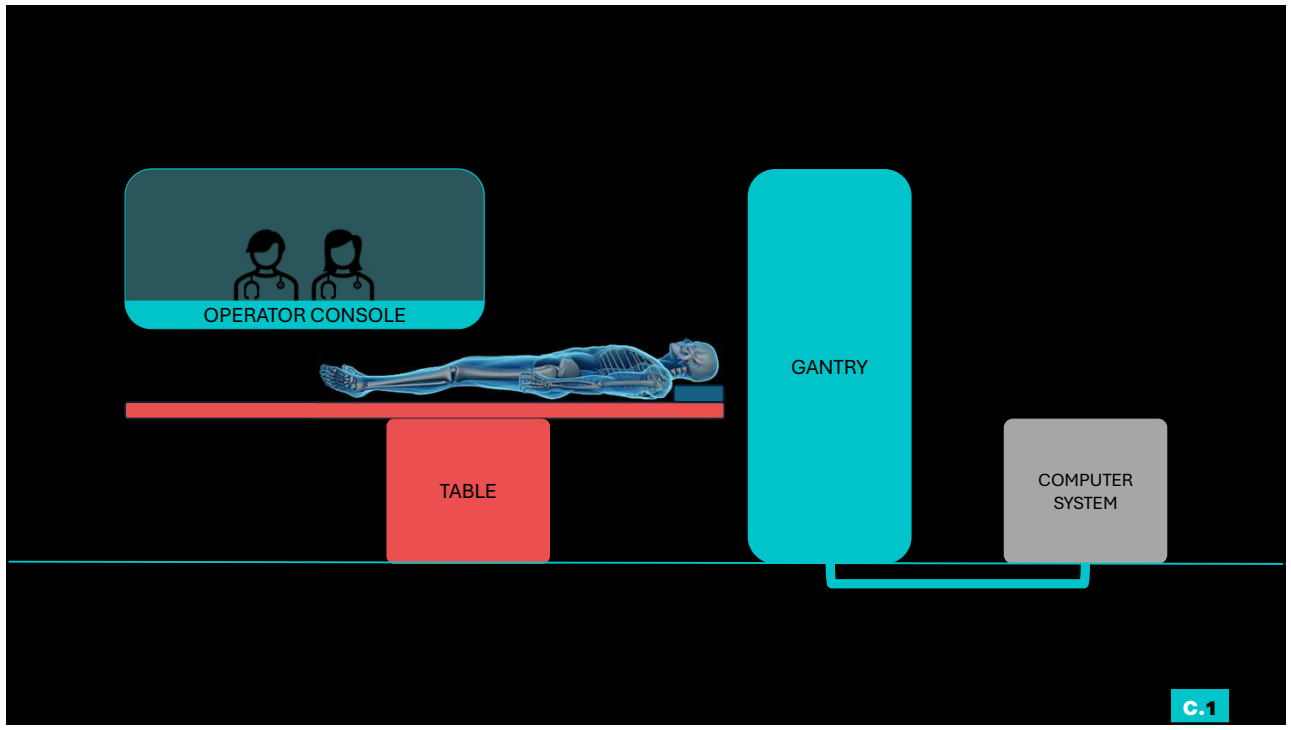


Responsible for the scanner's  
**"TEMPORAL RESOLUTION"**

61



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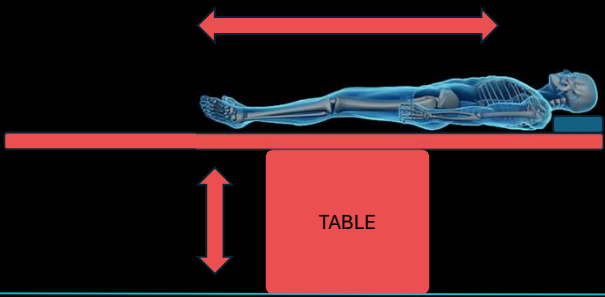


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### PATIENT TABLE

The table is responsible for feeding the patient into the gantry during the scan.

- Maximum patient weight allowed.
- Maximum scanning range.
- Maximum travel distance.
- Minimum table height possible.
- Lateral table movement (Some tables!)

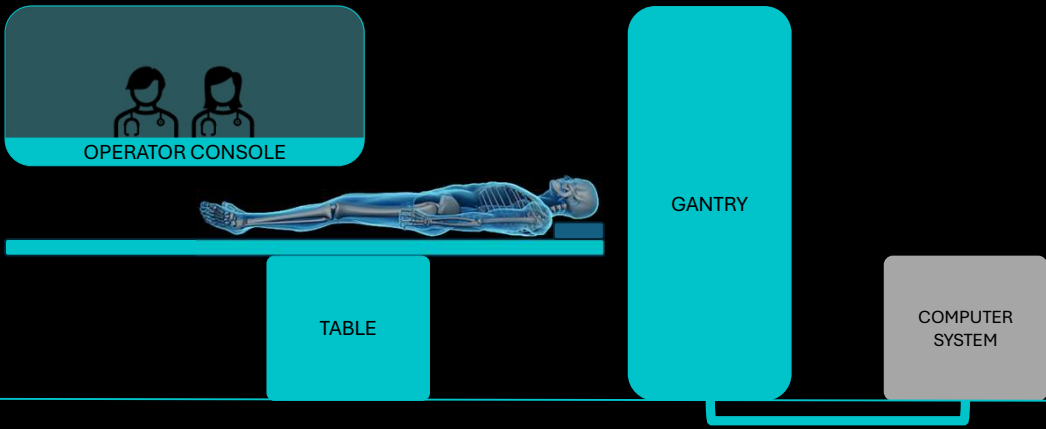


The diagram shows a human skeleton lying on a red table. A horizontal double-headed arrow above the table indicates the scanning range. A vertical double-headed arrow to the left of the table indicates its height. The table is supported by a red rectangular base labeled 'TABLE'.

- Scanning Range:** is the maximum patient length that can be scanned. (i.e. head to toe)
- Travel Distance:** is the range of movement that the table can achieve in the horizontal plane (Z-Axis)

C.1

64

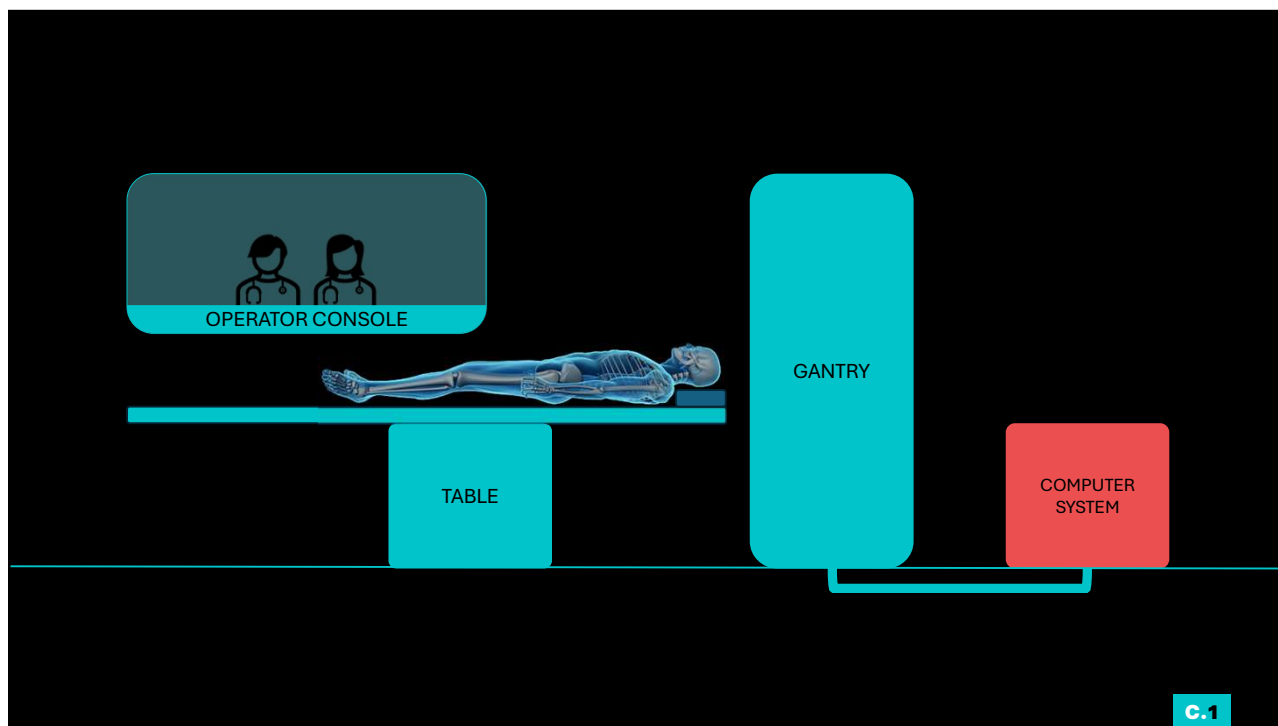


The diagram illustrates the layout of a CT scanner. On the left, an 'OPERATOR CONSOLE' is shown with icons of two people. In the center, a patient lies on a 'TABLE'. To the right of the table is the 'GANTRY'. Further to the right is the 'COMPUTER SYSTEM'. The table and gantry are supported by a common base.

C.1

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### COMPTUER SYSTEM

High-performance computers are essential for the computationally intensive tasks of image reconstruction and processing.

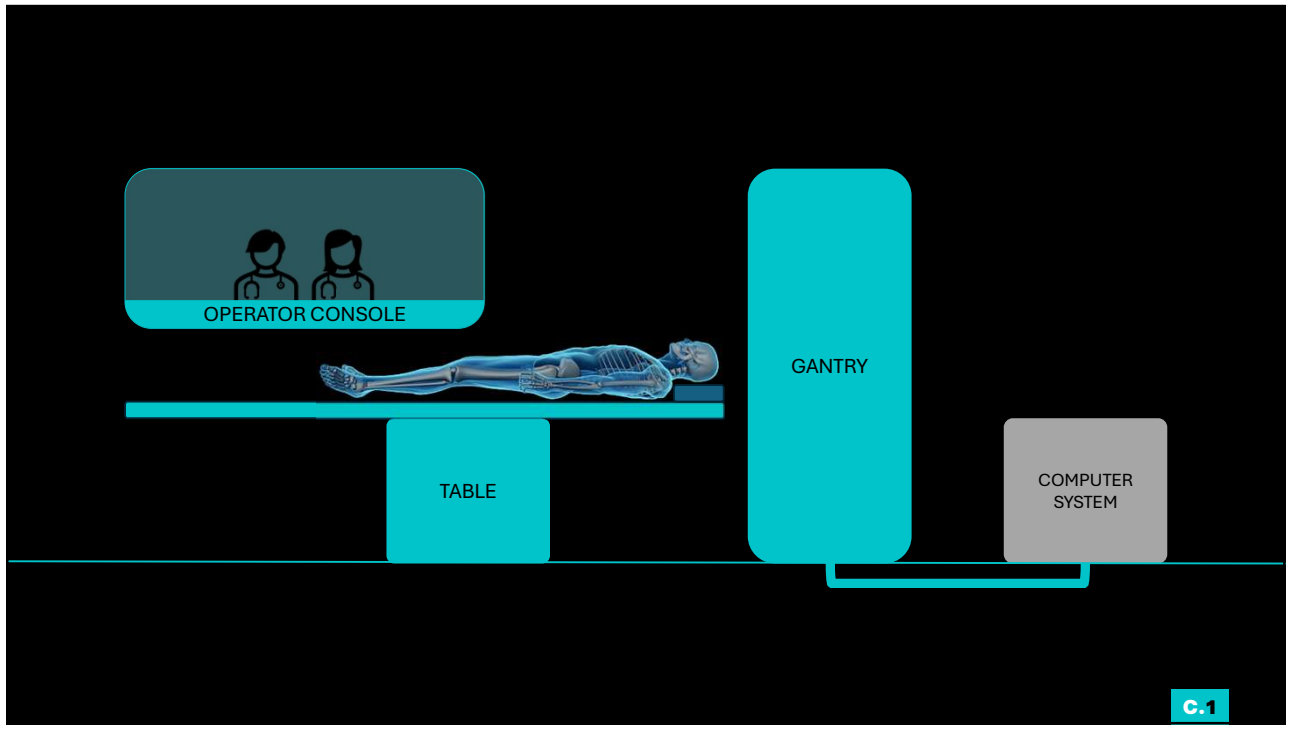
**Image Reconstruction:** The computer uses sophisticated algorithms (like filtered back projection or iterative reconstruction) to convert the raw data from the detector into cross-sectional images.

**Image Storage:** Large storage capacity is needed to archive patient data and images.

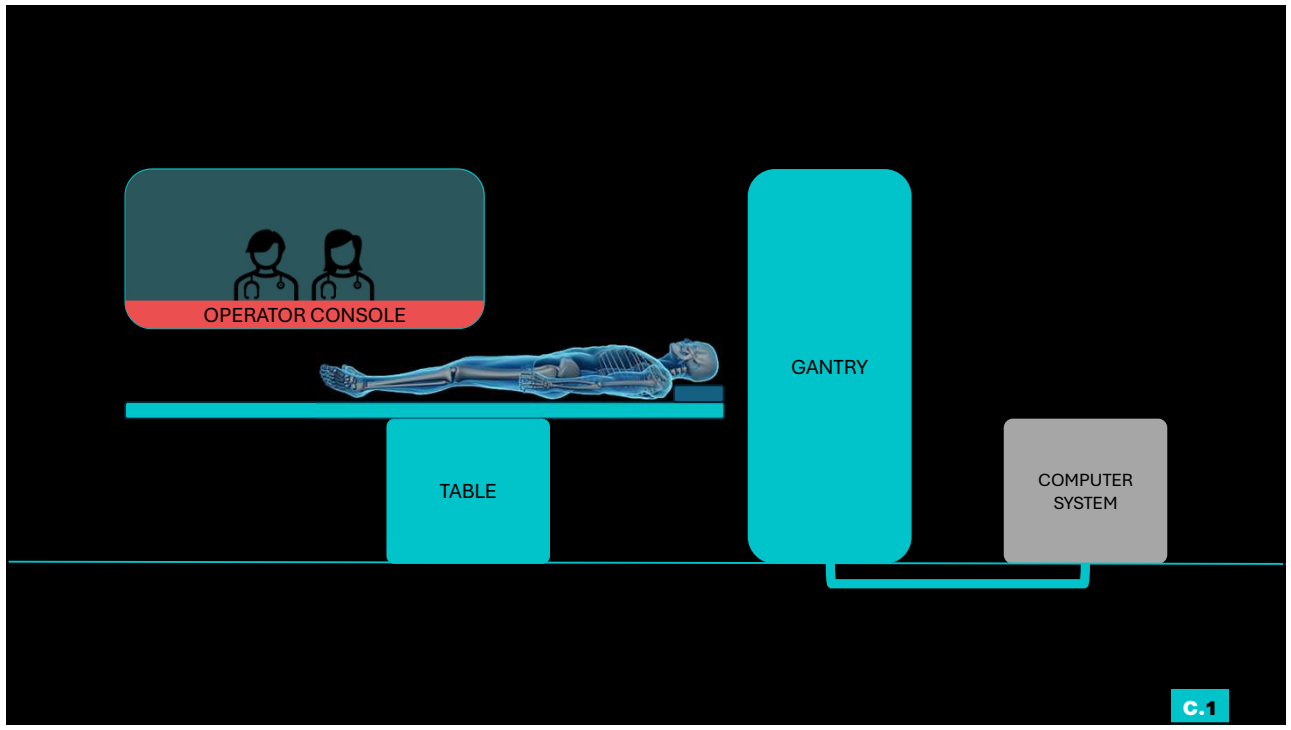
COMPUTER SYSTEM

**C.1**

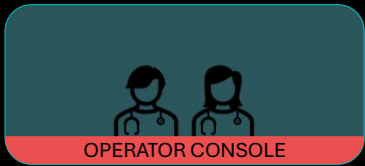
67



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**OPERATOR CONSOLE**

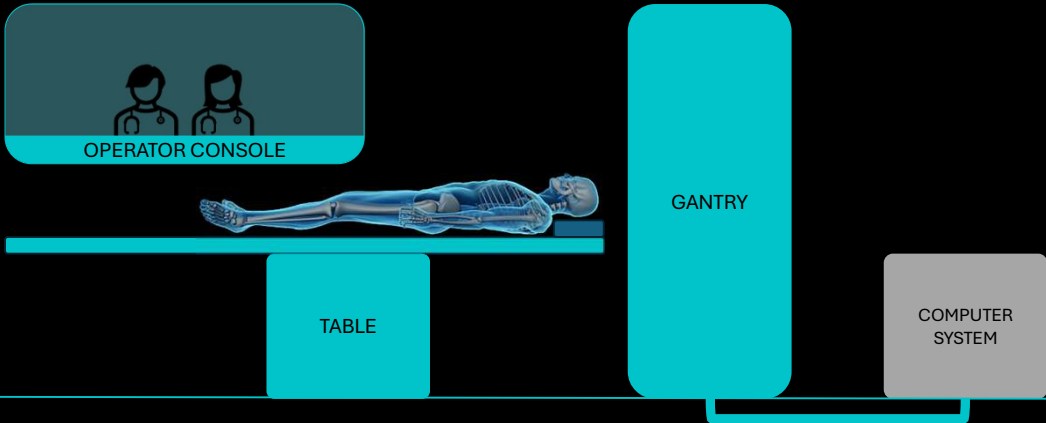
A workstation located outside the scanning room where the technologist controls the CT system.

**User Interface:** Includes a monitor, keyboard and mouse for setting scan parameters, viewing images, and managing patient data.

**Software:** Powerful software controls the scanner, processes the image data, and provides tools for image analysis and manipulation (Post Processing).

**C.1**

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**OPERATOR CONSOLE**

**TABLE**

**GANTRY**

**COMPUTER SYSTEM**

**C.1**

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<b>SCANOGRAM (SCOUT OR LOCALIZER)</b>	
<p><b>AXIAL (STEP &amp; SHOOT)</b></p> <p>The scan is performed sequentially one acquisition (exposure) at a time. The beam is turned on and off with table movement between exposures.</p>	<p><b>HELICAL (SPIRAL)</b></p> <p>The scan is performed as one continuous exposure. The tube/detector constantly rotates and expose the patient while the table is constantly moves into the gantry</p>
<p><b>VOLUME</b></p> <p>One shot exposure of an area of the patient (no table movement). The maximum possible size of the area is limited to the width of the detector in the Z-axis</p>	<p><b>DYNAMIC (CINE)</b></p> <p>A continuous exposure or multiple exposures of an area of the patient (no table movement). Used for evaluation physiological evaluations.</p>

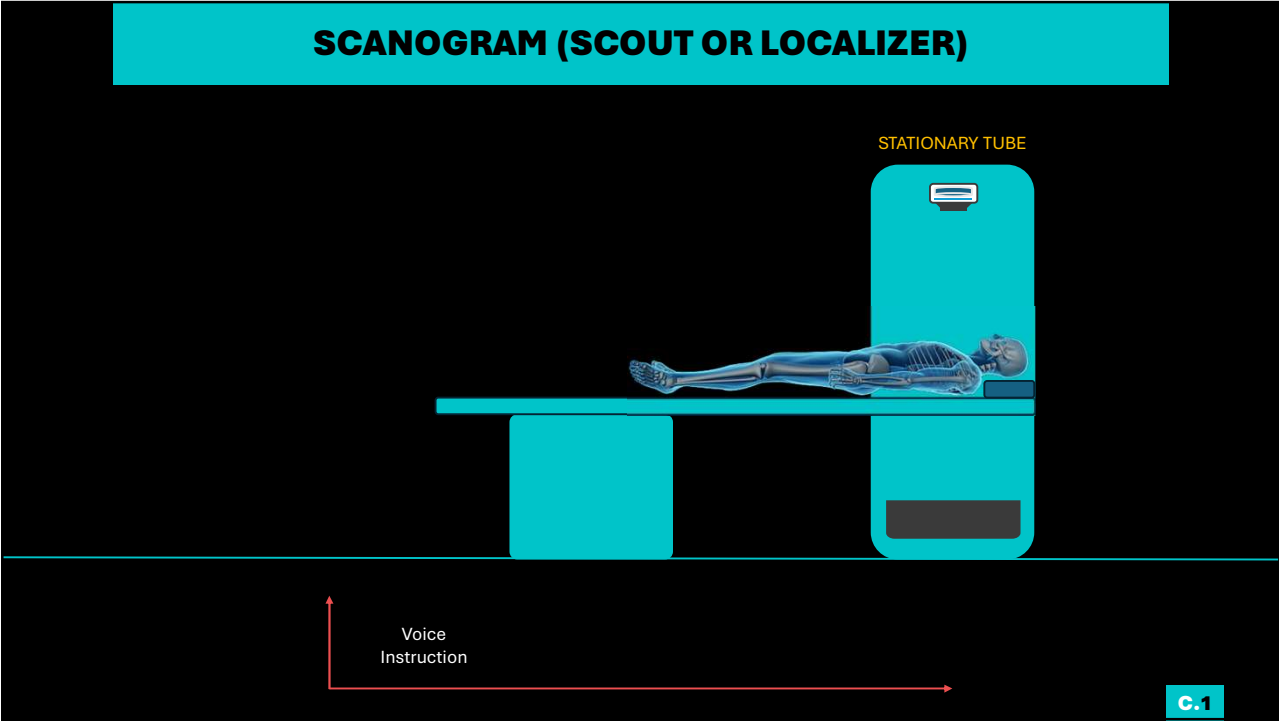
**C.1**

74

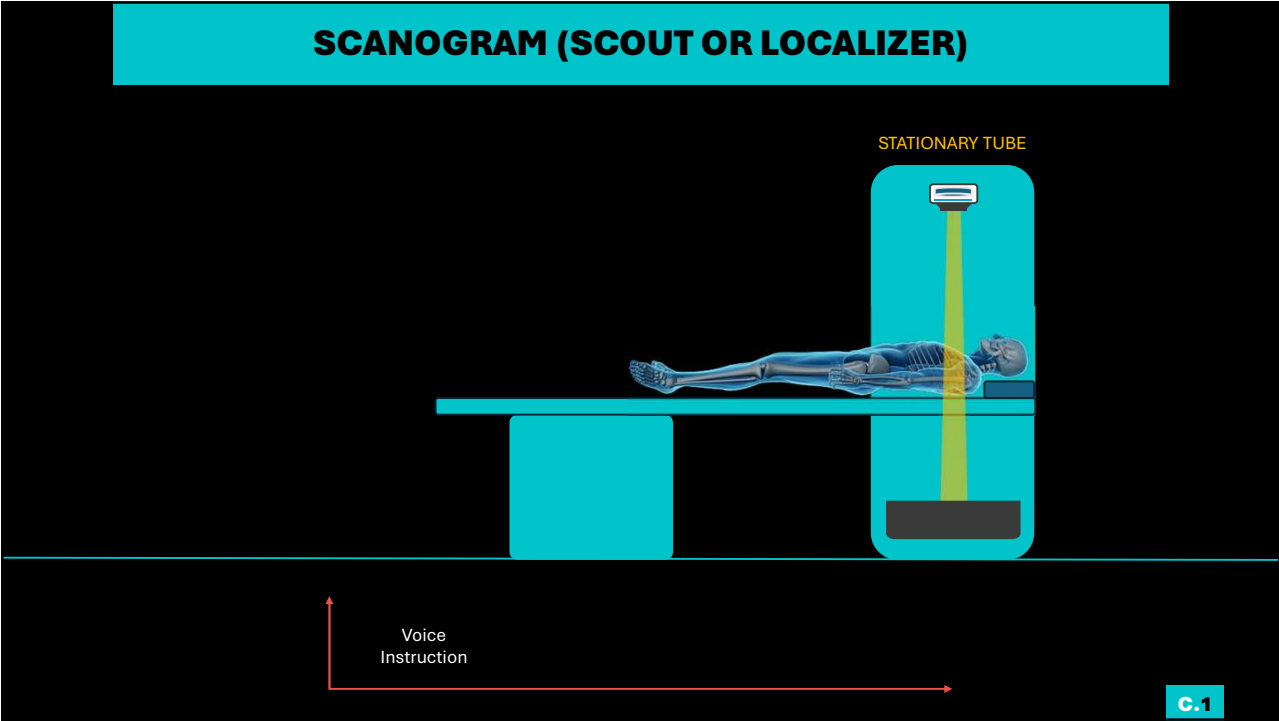
**SCANOGRAM (SCOUT OR LOCALIZER)**

**C.1**

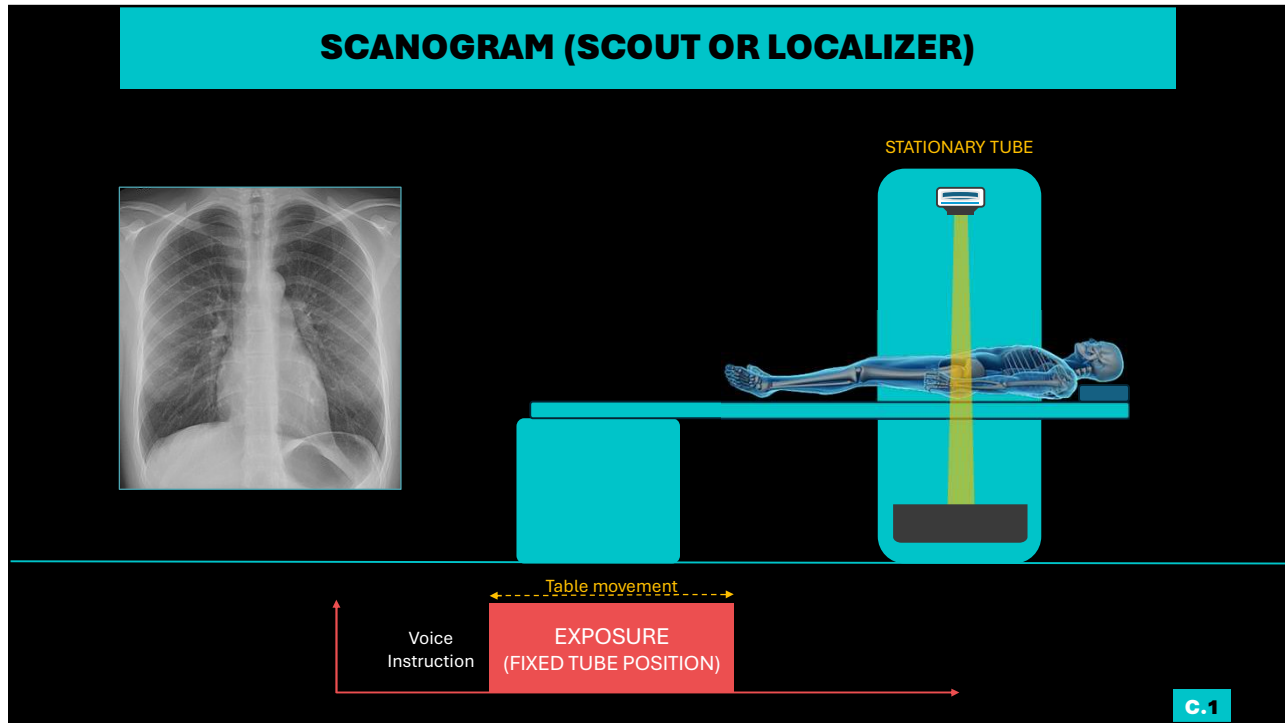
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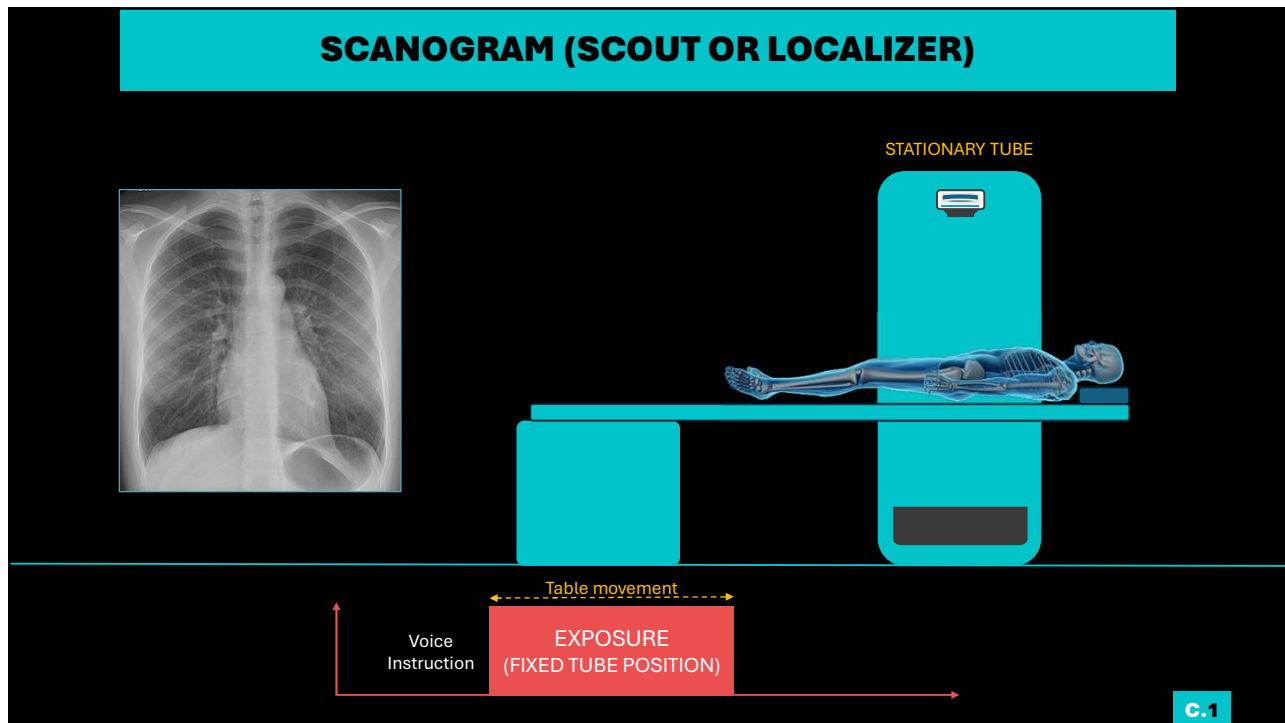
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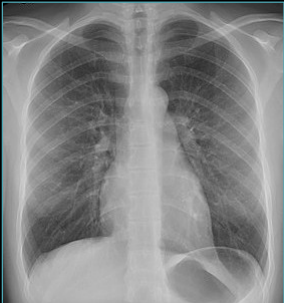
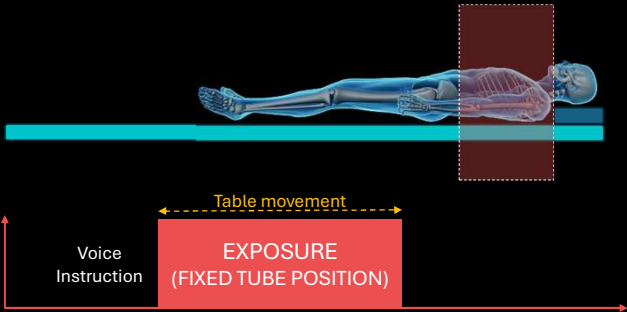


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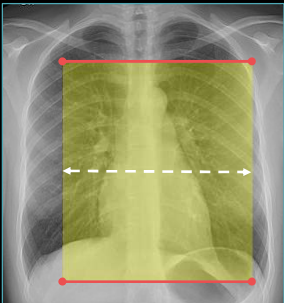
### SCANOGRAM (SCOUT OR LOCALIZER)

C.1

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### SCANOGRAM (SCOUT OR LOCALIZER)



START LOCATION

FIELD OF VIEW

END LOCATION

**Scanogram:** The scout (localizer) is a 2D radiograph acquired at the beginning of most CT procedures. It is done using a fixed X-Ray tube. The beam is turned on, continuously exposing the patient while moving the table into the gantry. The scout is used as a guide to plan the CT procedure. (Start location, End location, FOV)

C.1

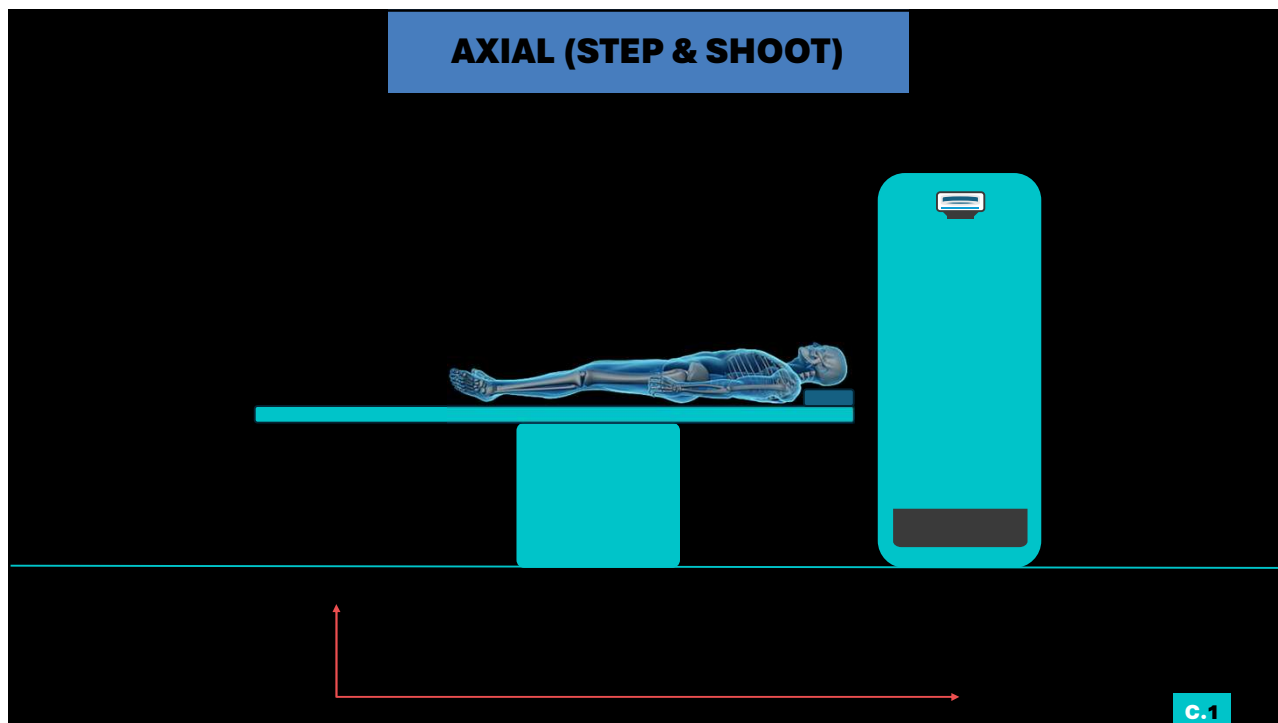
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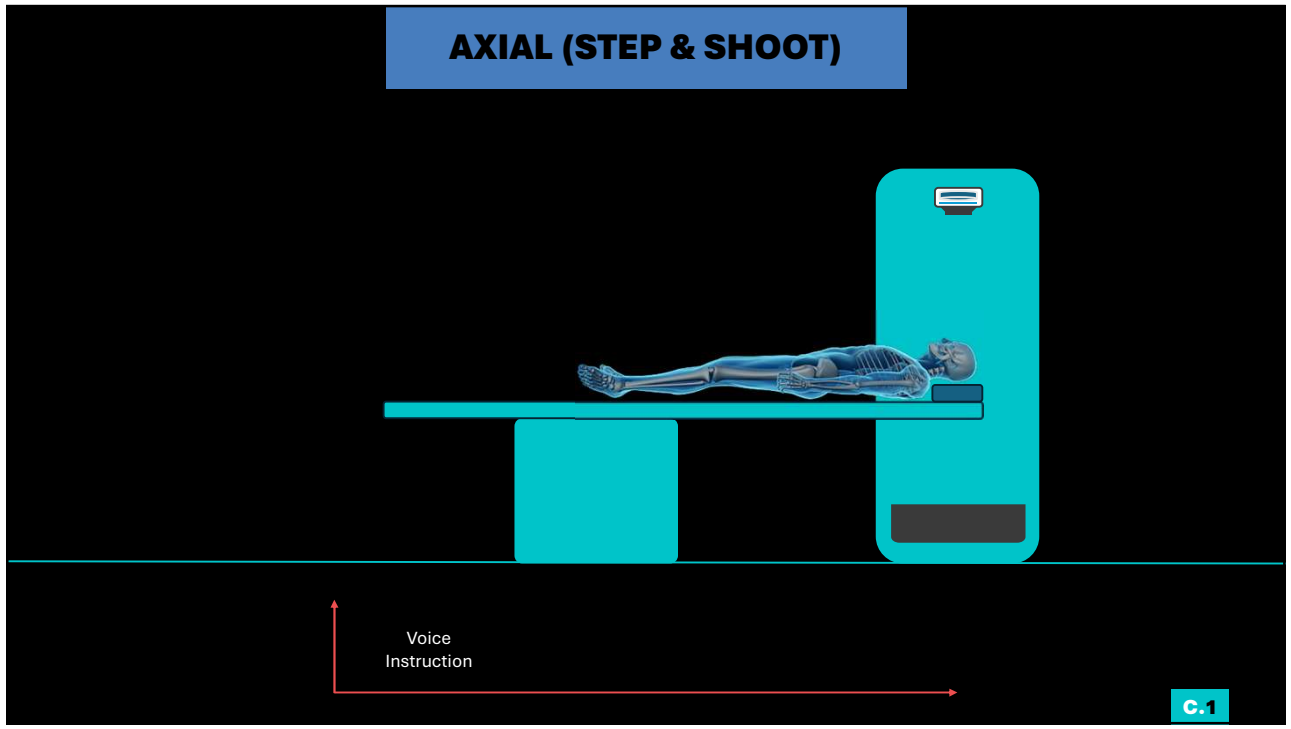
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**C.1**

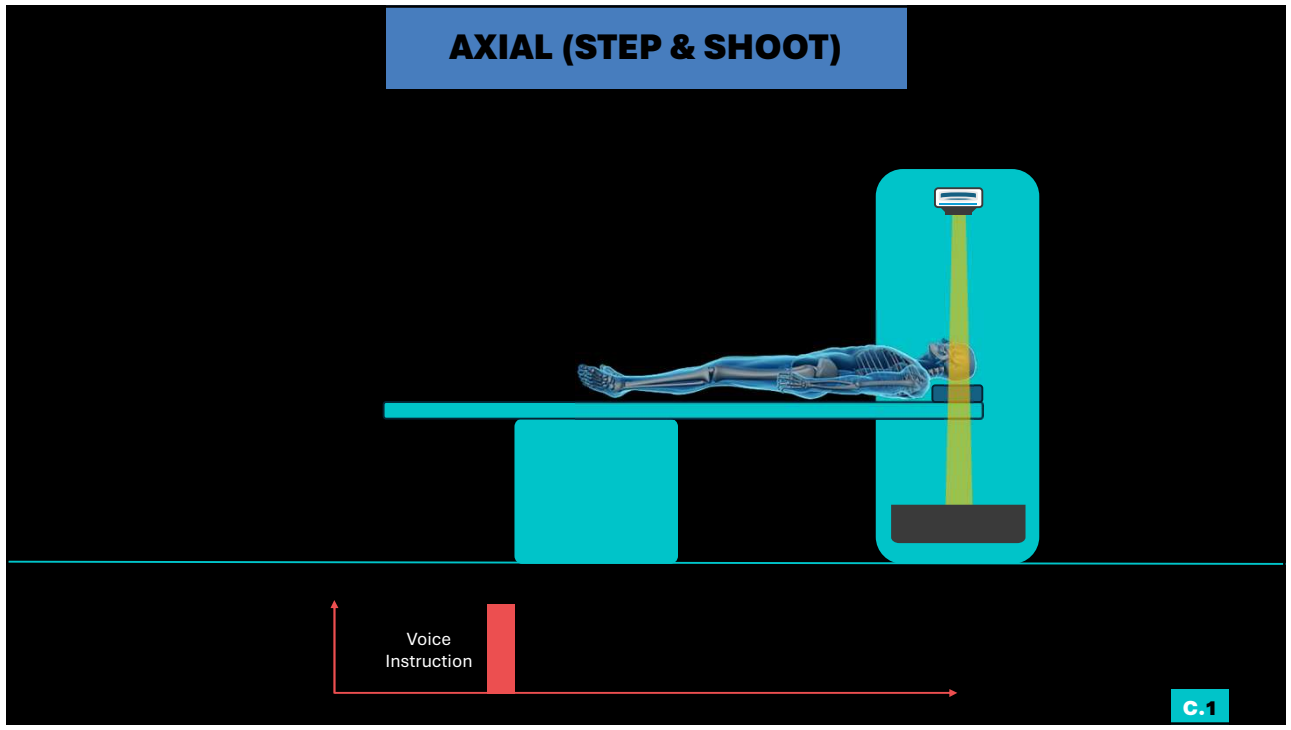
82



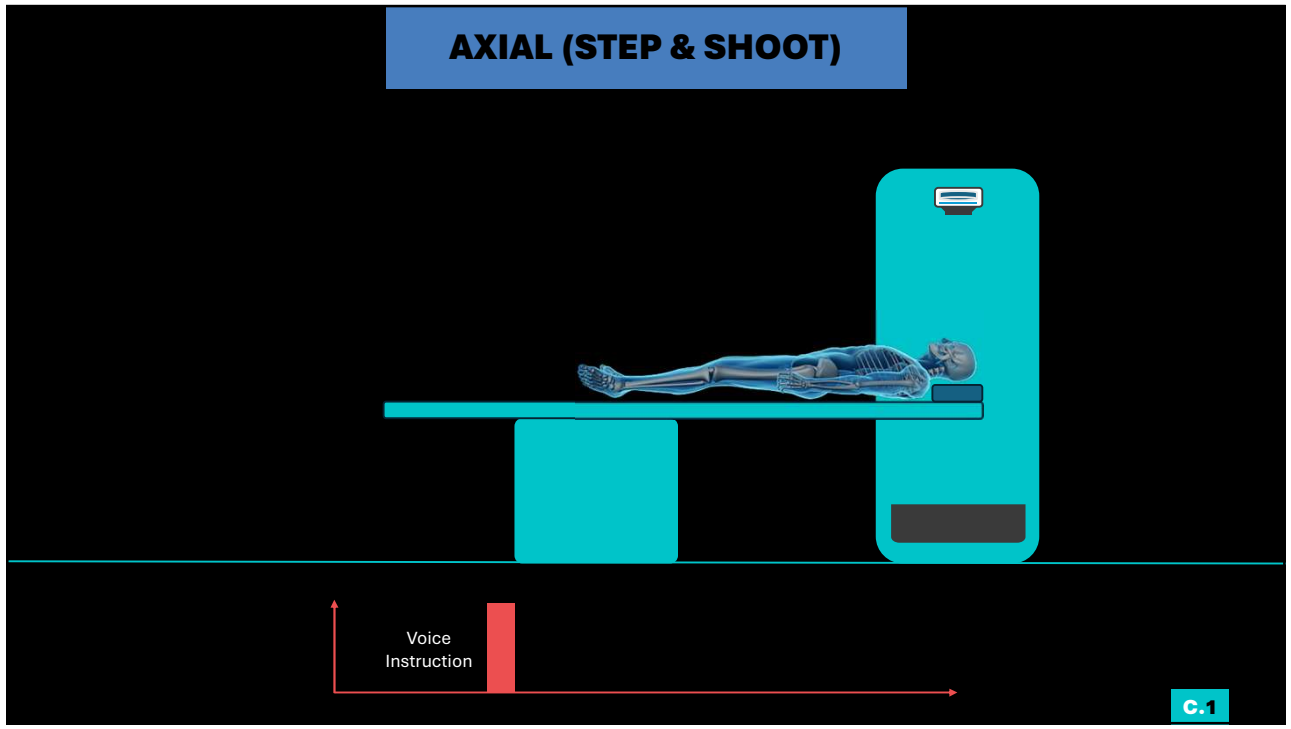
83



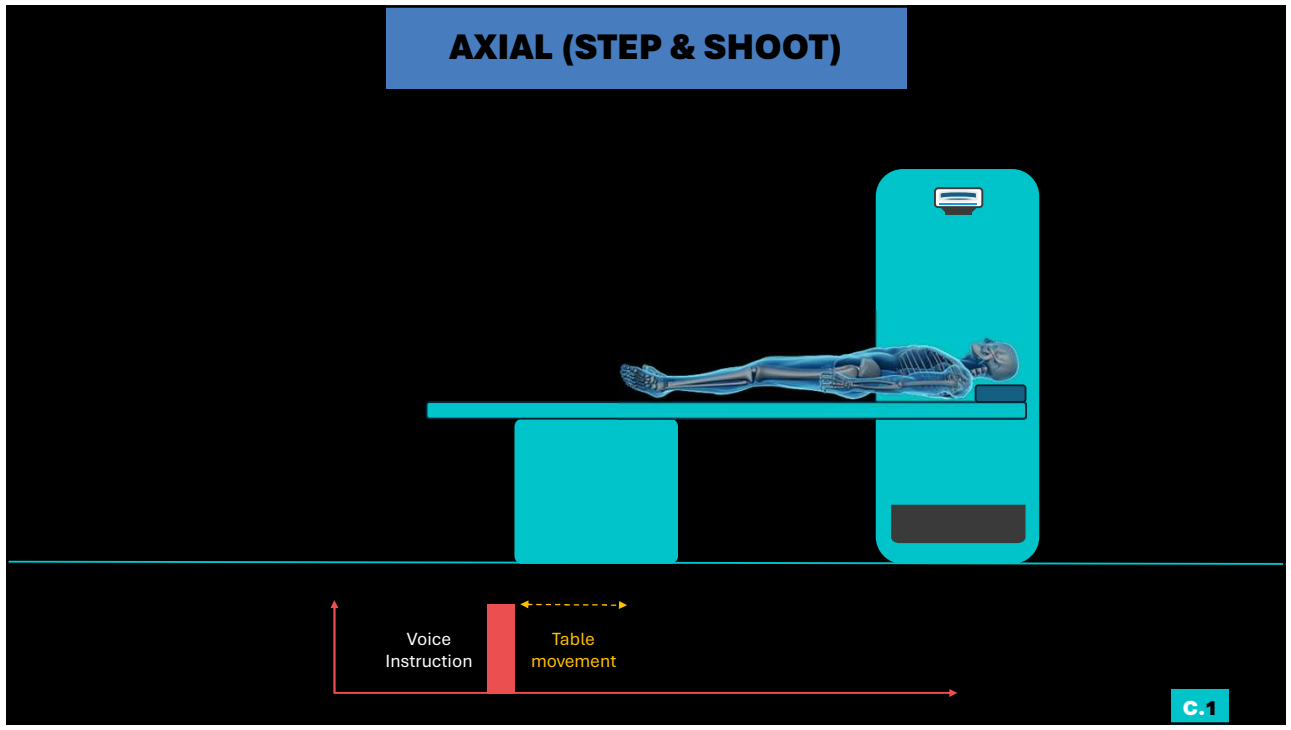
84



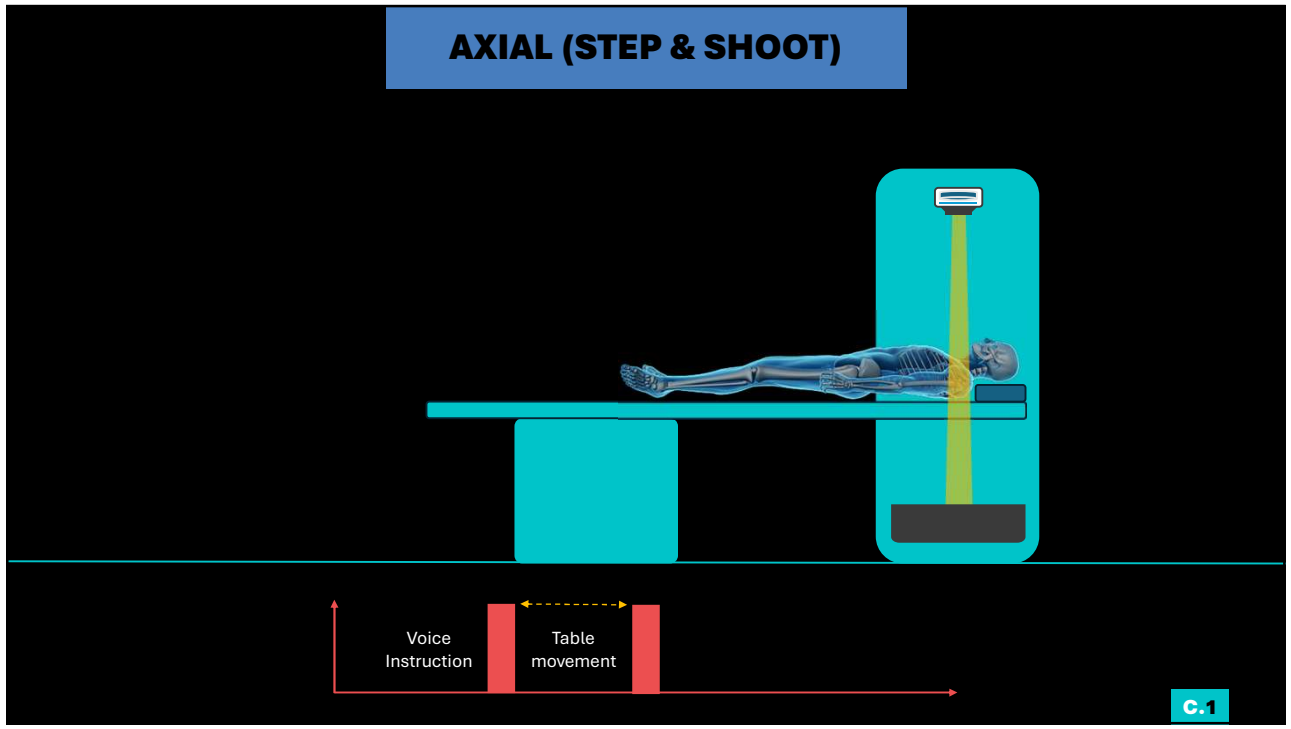
85



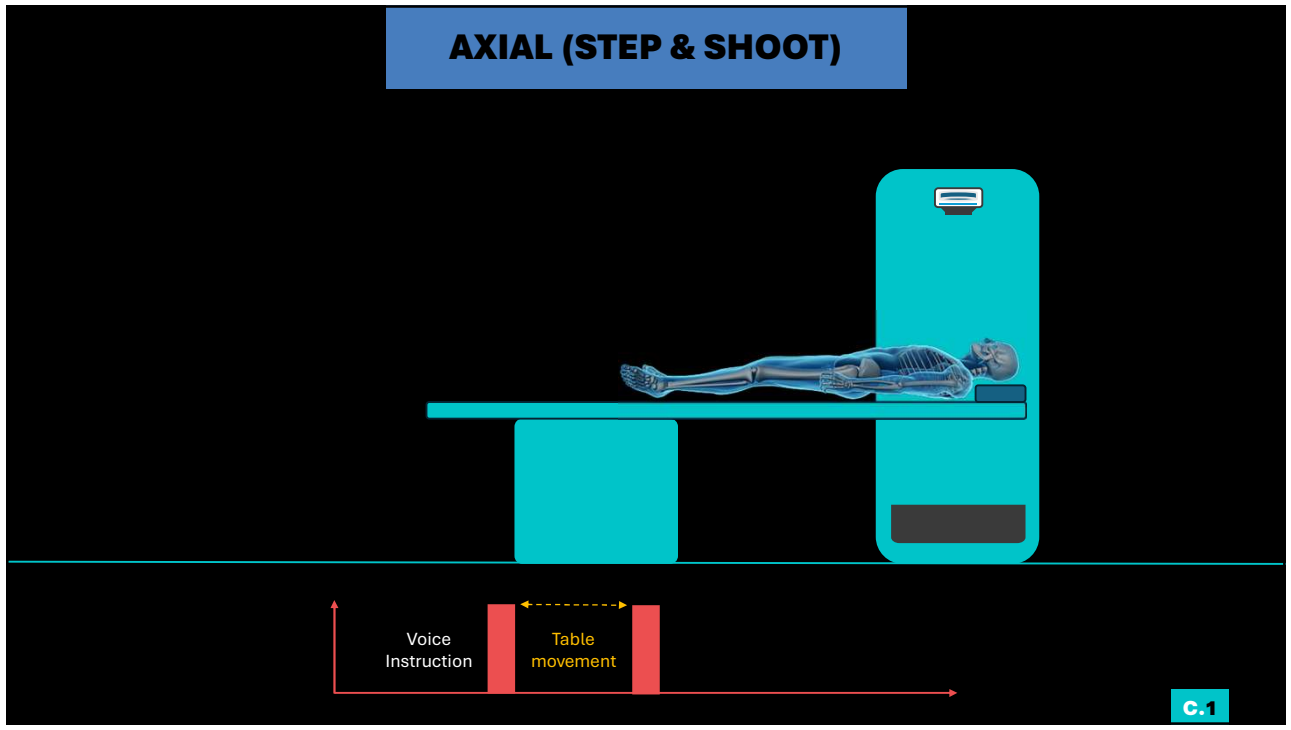
86



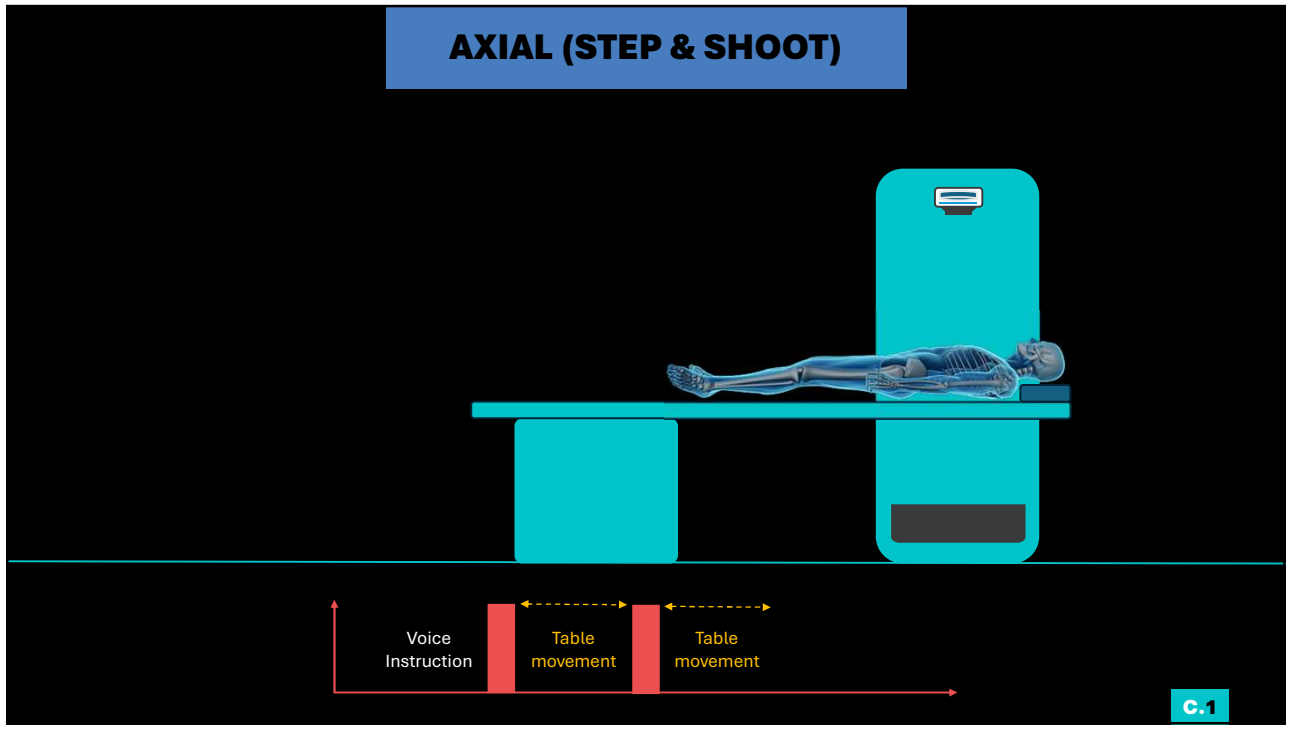
87



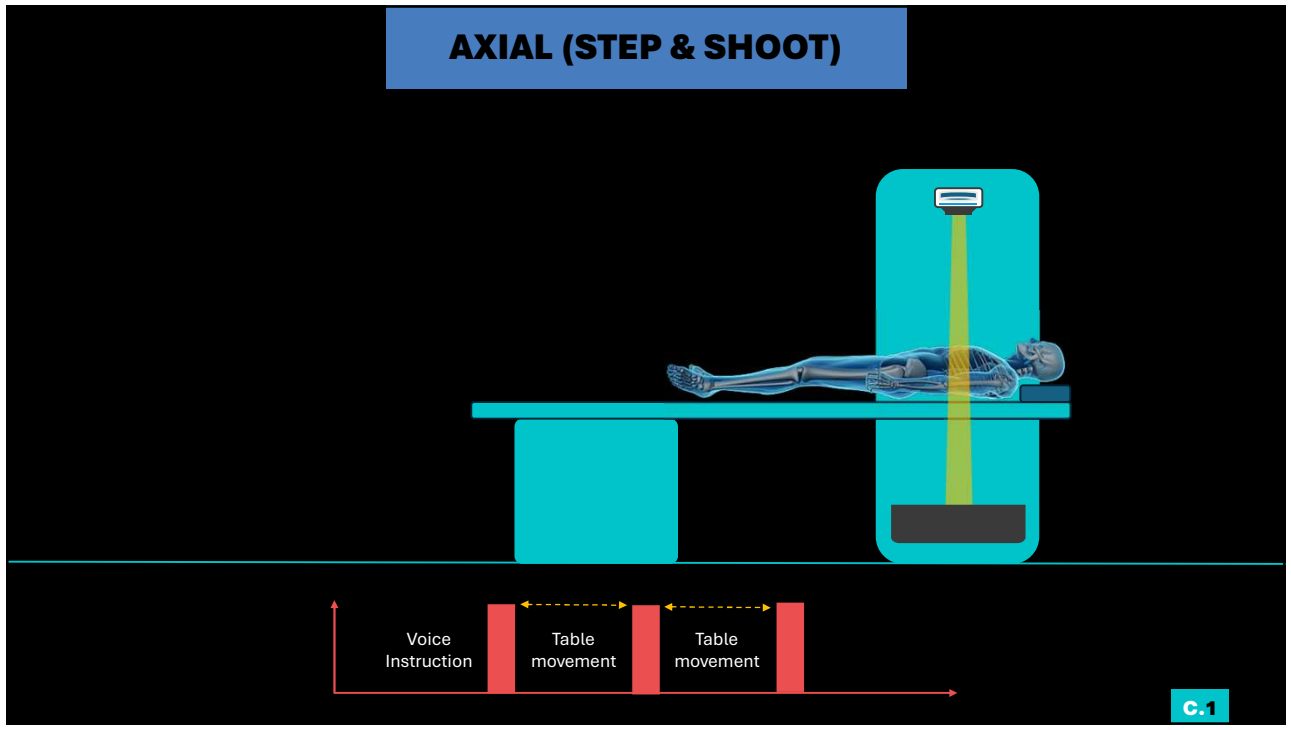
88



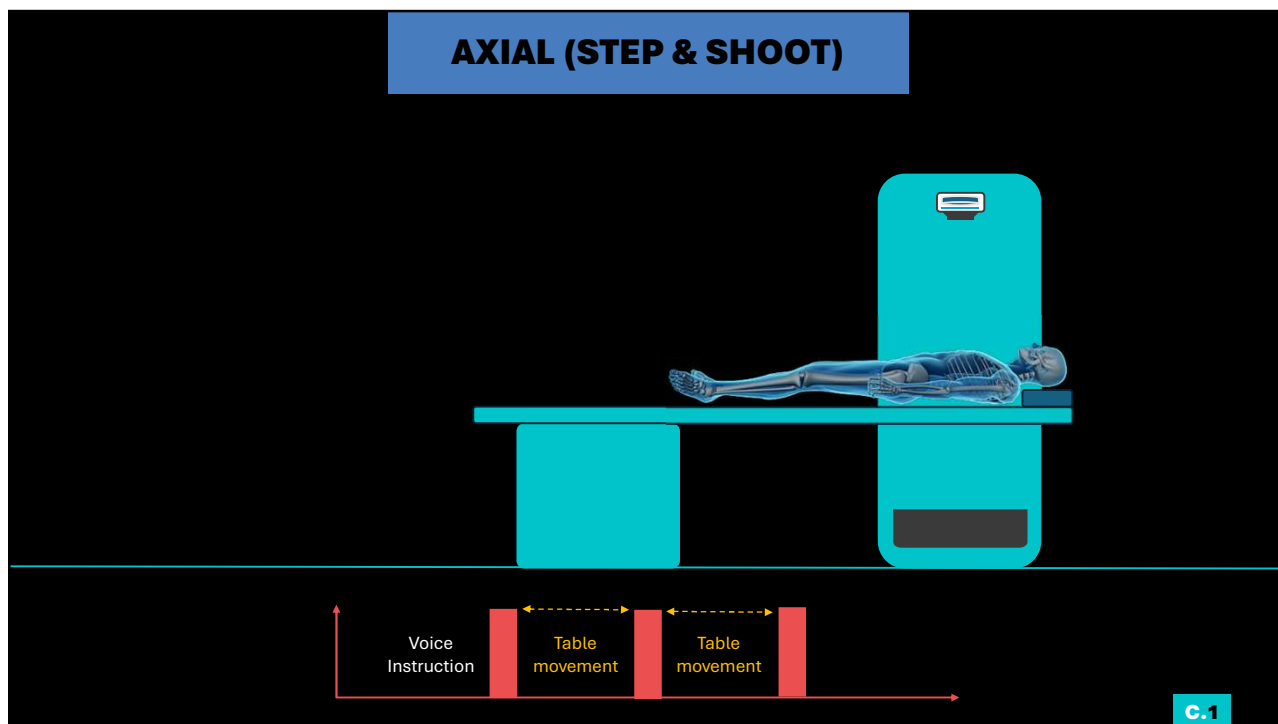
89



90



91



92

### AXIAL (STEP & SHOOT)

**How it Works:** The x-ray tube and detectors rotate around the patient while the patient table remains stationary. After one complete rotation, the table moves (increments) to the next position, and the process repeats. The result is a series of axial acquisitions.

**Pros:** Gold standard of spatial resolution.

**Cons:** very slow, limited reformatting capability

Voice Instruction    Table movement    Table movement

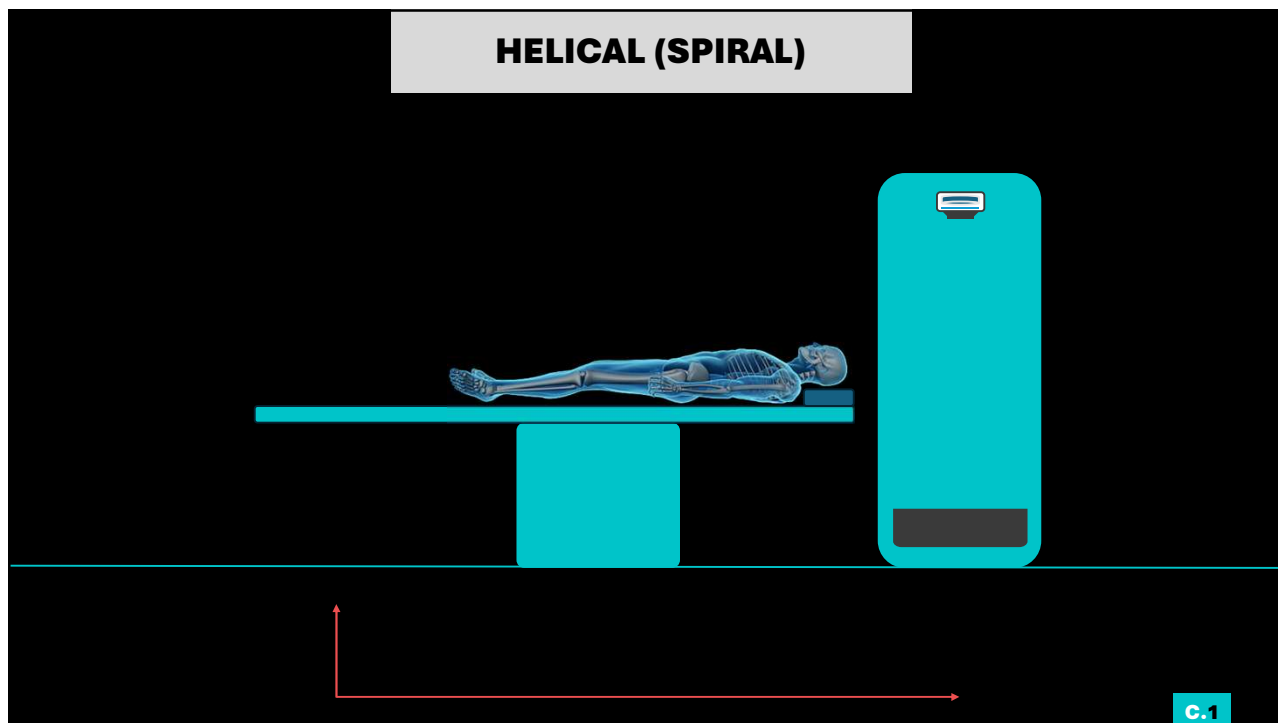
C.1

93

<b>SCANOGRAM (SCOUT OR LOCALIZER)</b>	
<p><b>AXIAL (STEP &amp; SHOOT)</b></p> <p>The scan is performed sequentially one acquisition (exposure) at a time. The beam is turned on and off with table movement between exposures.</p>	<p><b>HELICAL (SPIRAL)</b></p> <p>The scan is performed as one continuous exposure. The tube/detector constantly rotates and expose the patient while the table is constantly moves into the gantry</p>
<p><b>VOLUME</b></p> <p>One shot exposure of an area of the patient (no table movement). The maximum possible size of the area is limited to the width of the detector in the Z-axis</p>	<p><b>DYNAMIC (CINE)</b></p> <p>A continuous exposure or multiple exposures of an area of the patient (no table movement). Used for evaluation physiological evaluations.</p>

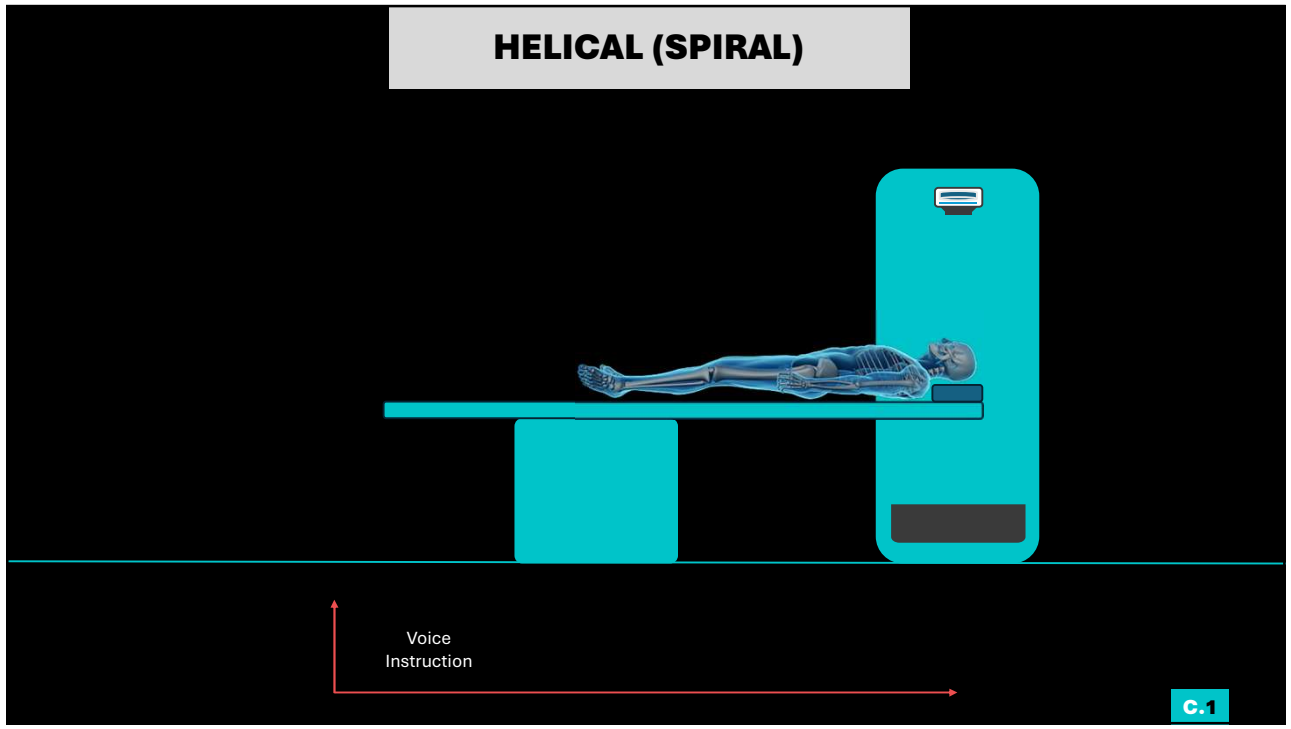
C.1

94

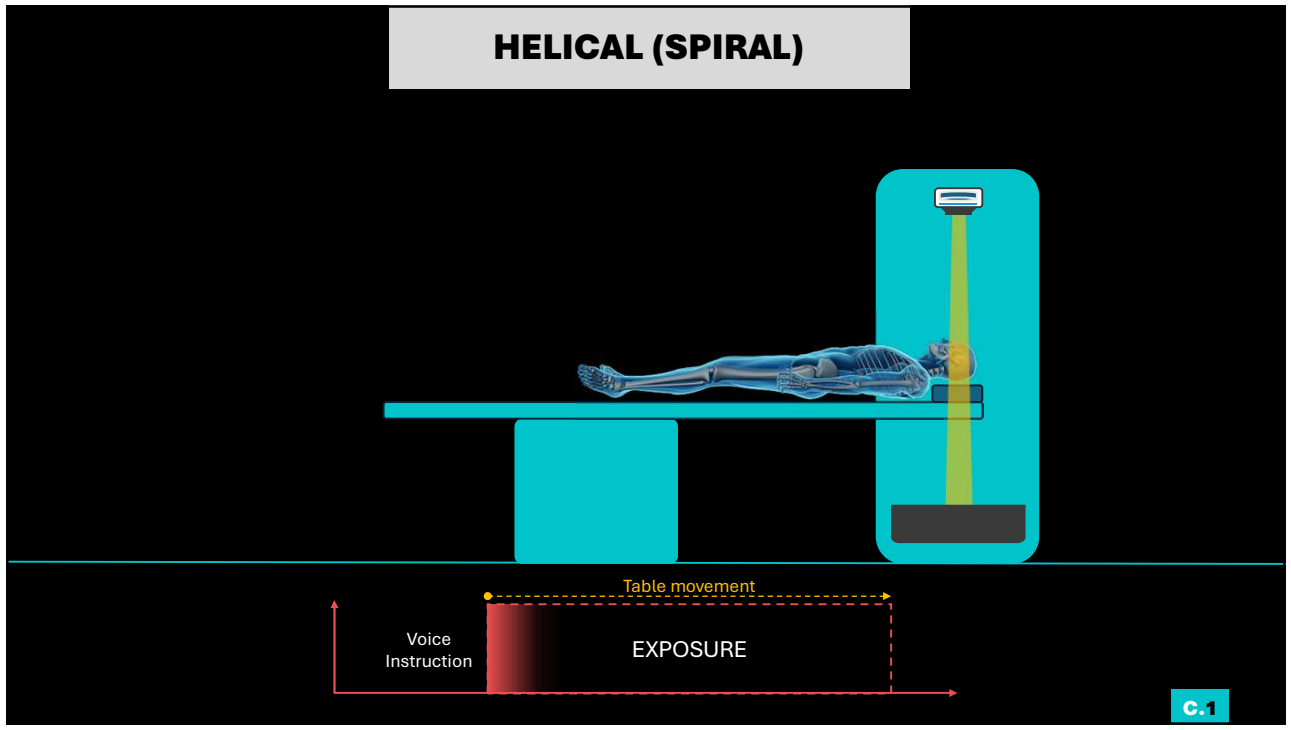


C.1

95

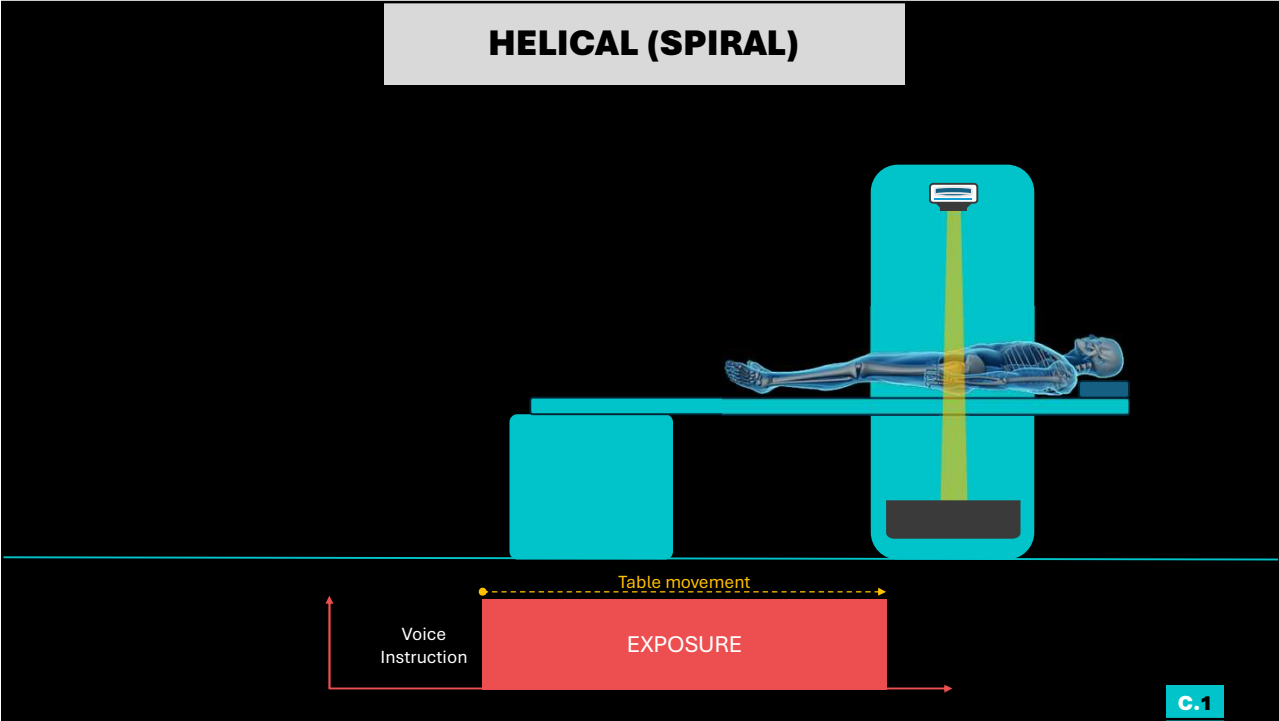


96

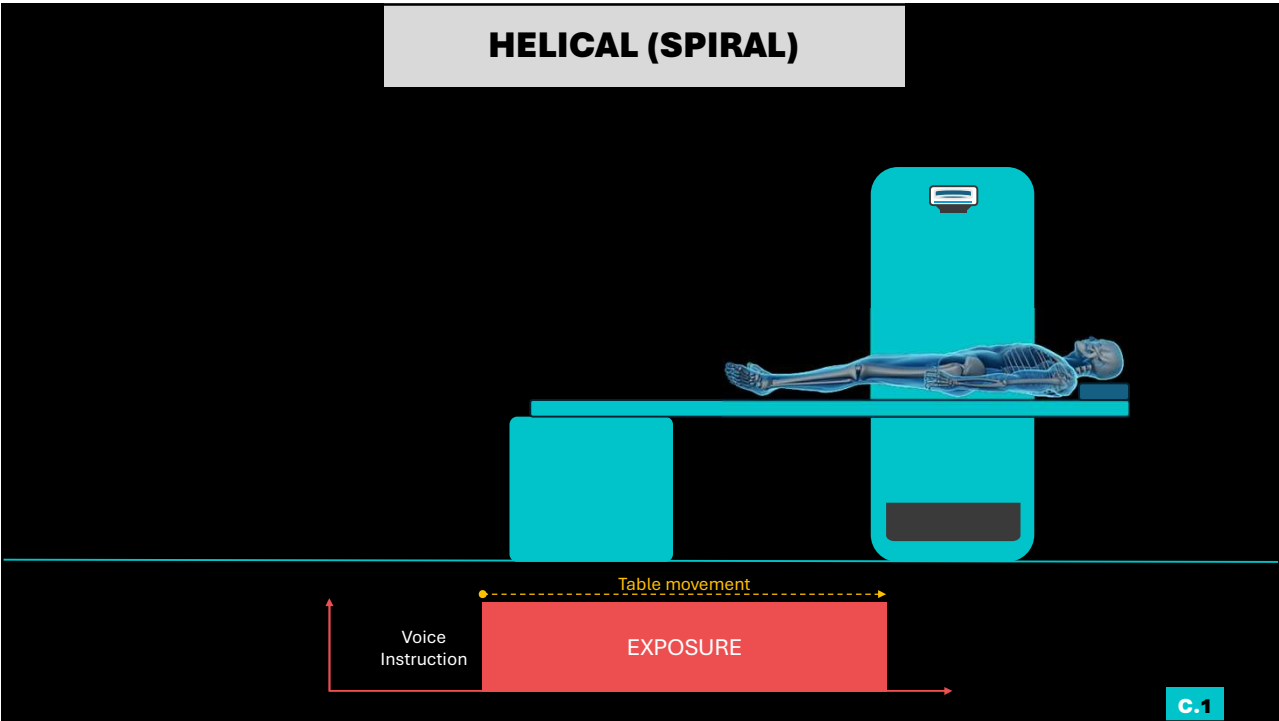


97





98



99

## HELICAL (SPIRAL)

**How it Works:** The x-ray tube and detectors rotate continuously while the patient table moves through the gantry at a constant speed. This creates a spiral or helical path of data acquisition.

**Pros:** Gold standard of spatial resolution.

**Cons:** very slow, limited reformatting capability

**C.1**

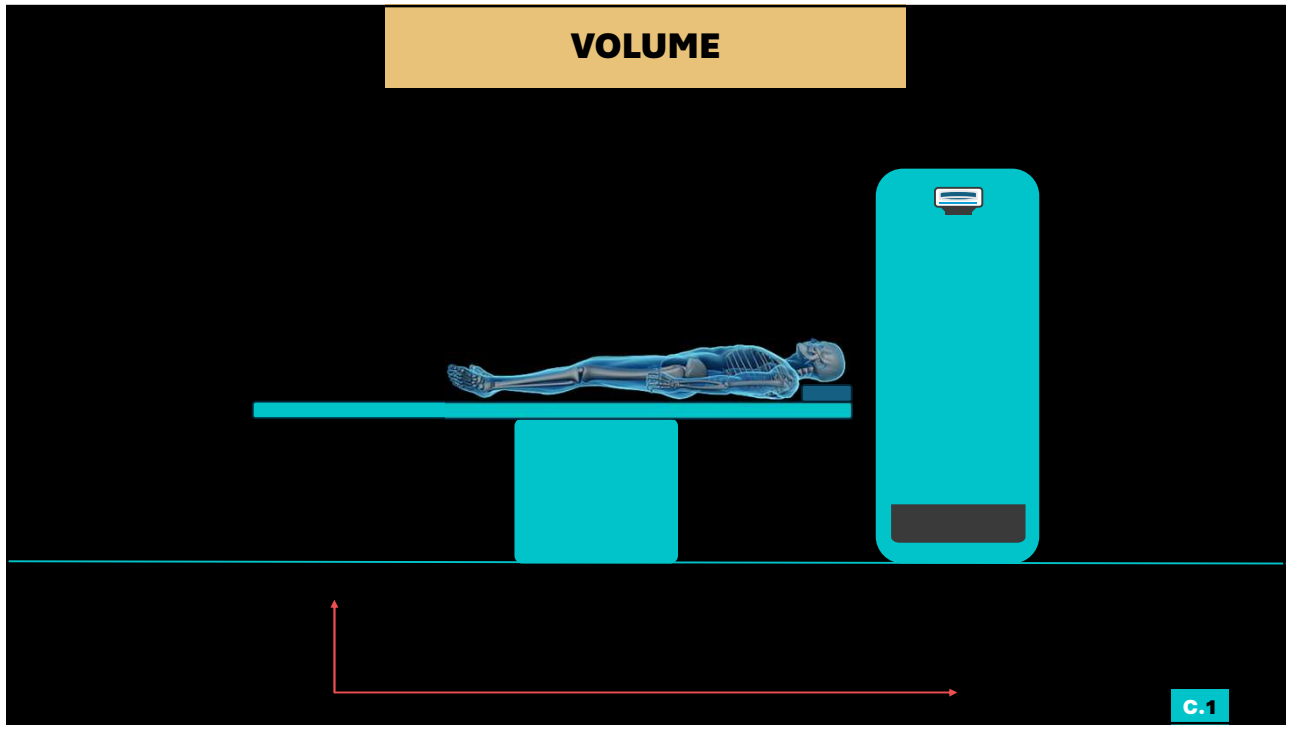
100

## SCANOGRAM (SCOUT OR LOCALIZER)

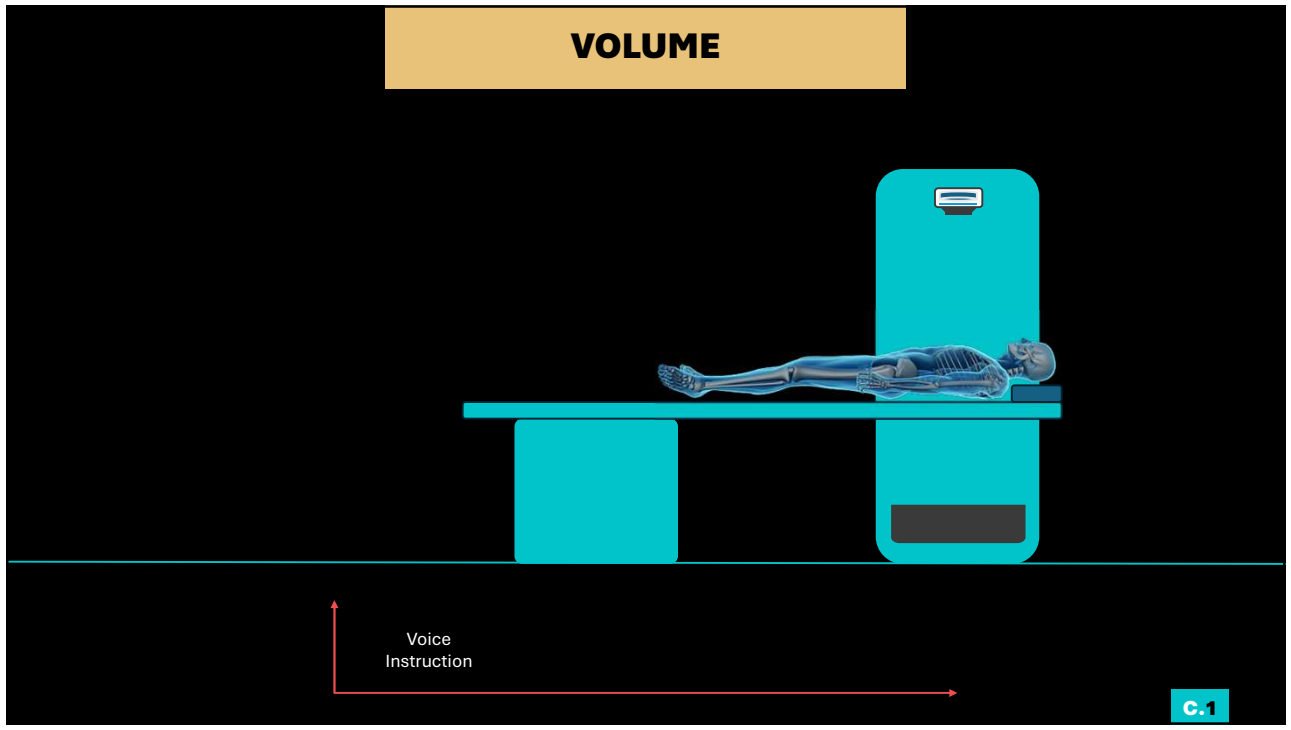
<h3 style="text-align: center;">AXIAL (STEP &amp; SHOOT)</h3> <p>The scan is performed sequentially one acquisition (exposure) at a time. The beam is turned on and off with table movement between exposures.</p>	<h3 style="text-align: center;">HELICAL (SPIRAL)</h3> <p>The scan is performed as one continuous exposure. The tube/detector constantly rotates and expose the patient while the table is constantly moves into the gantry</p>
<h3 style="text-align: center;">VOLUME</h3> <p>One shot exposure of an area of the patient (no table movement). The maximum possible size of the area is limited to the width of the detector in the Z-axis</p>	<h3 style="text-align: center;">DYNAMIC (CINE)</h3> <p>A continuous exposure or multiple exposures of an area of the patient (no table movement). Used for evaluation physiological evaluations.</p>

**C.1**

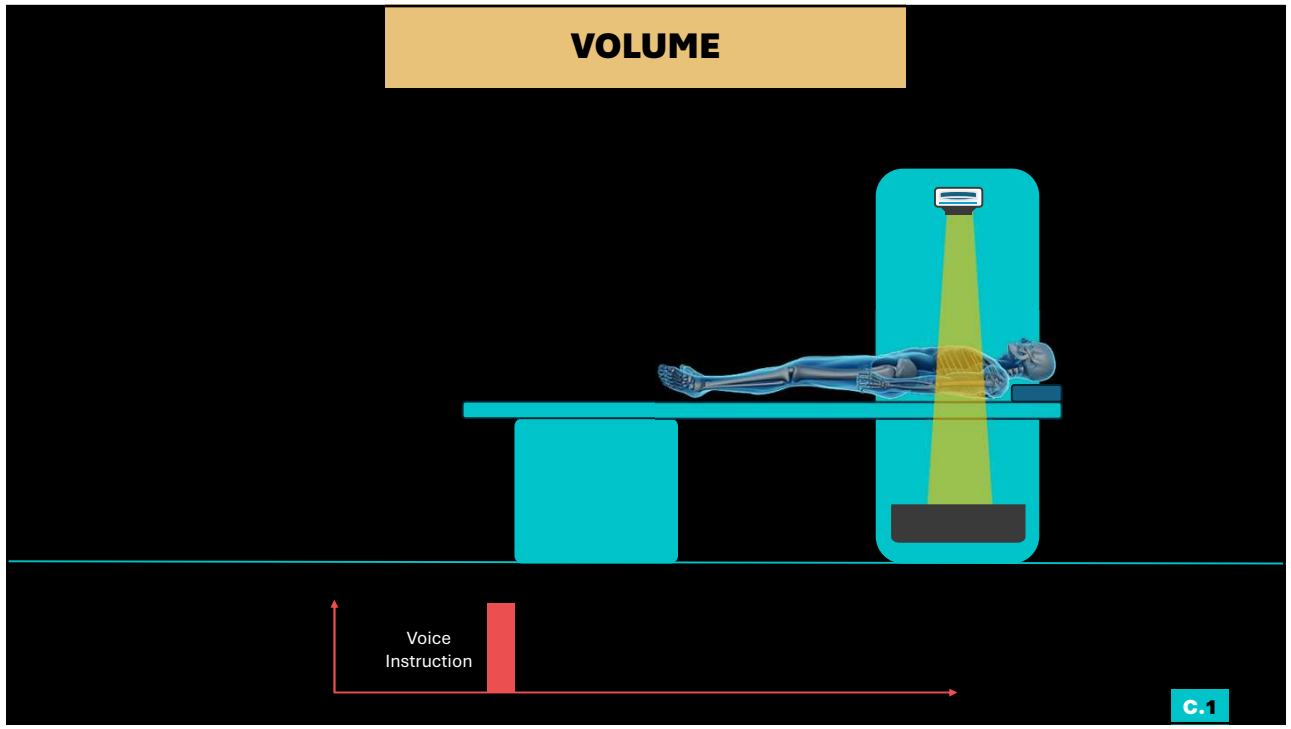
101



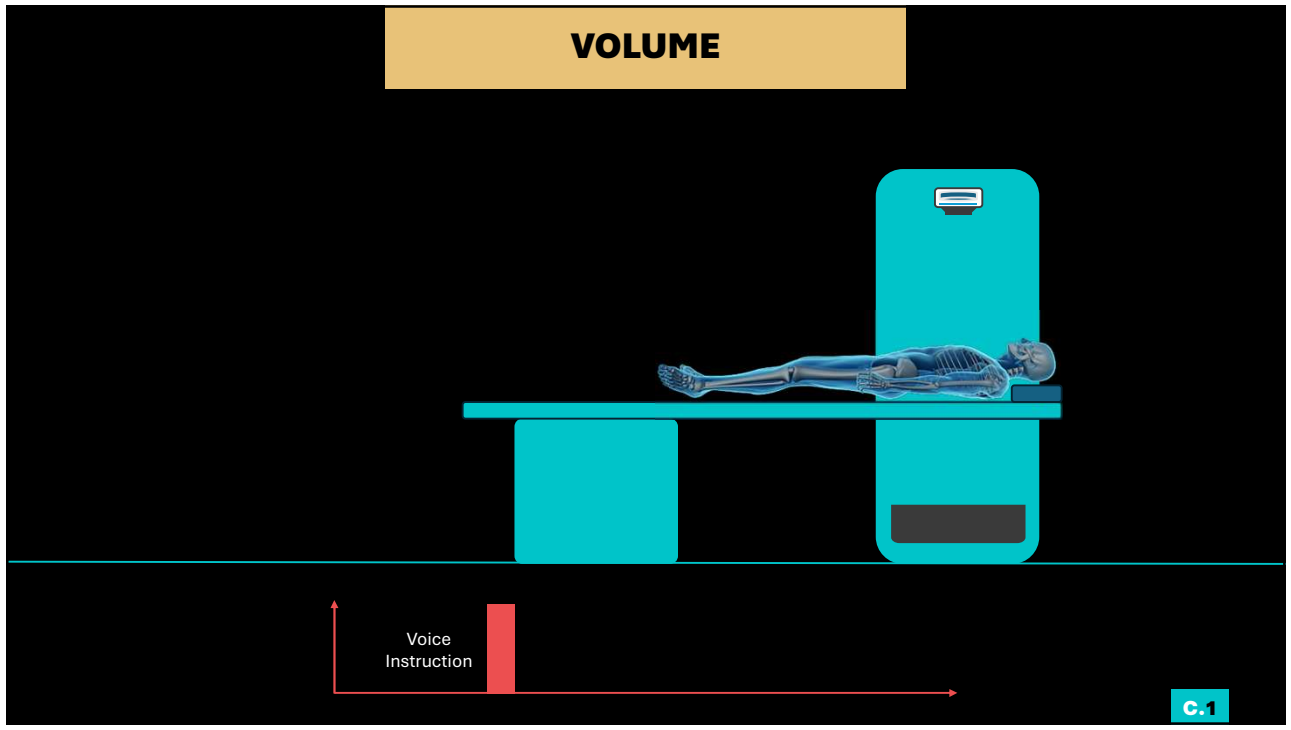
102



103



104



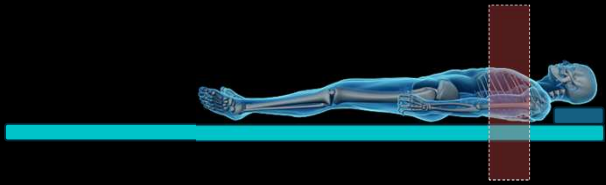
105

## VOLUME

**How it Works:** Utilizing a large area detector and wide beam-collimation, a single large axial acquisition is completed in one rotation around the patient without table movement.

**Pros:** Acquires a large volume of data quickly, low radiation dose

**Cons:** limited coverage, may have lower spatial resolution compared to axial and helical scans, large area detector require deep gantry designs.



Voice Instruction

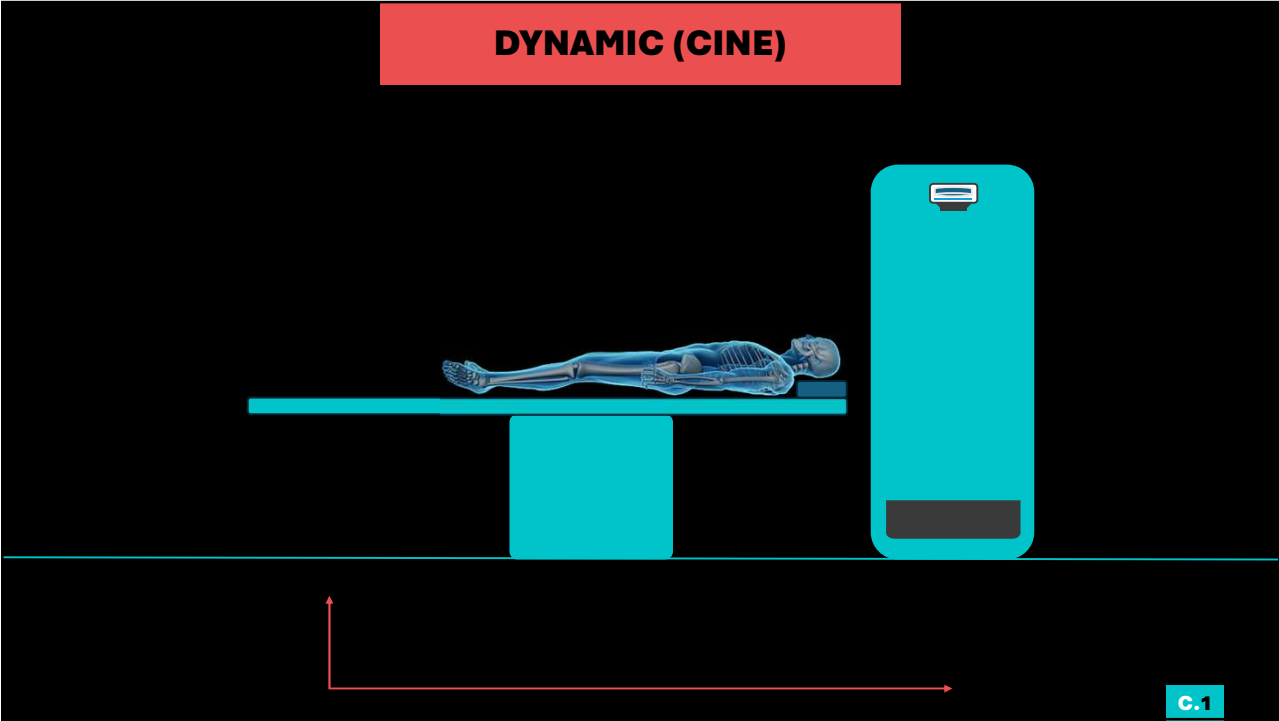
C.1

106

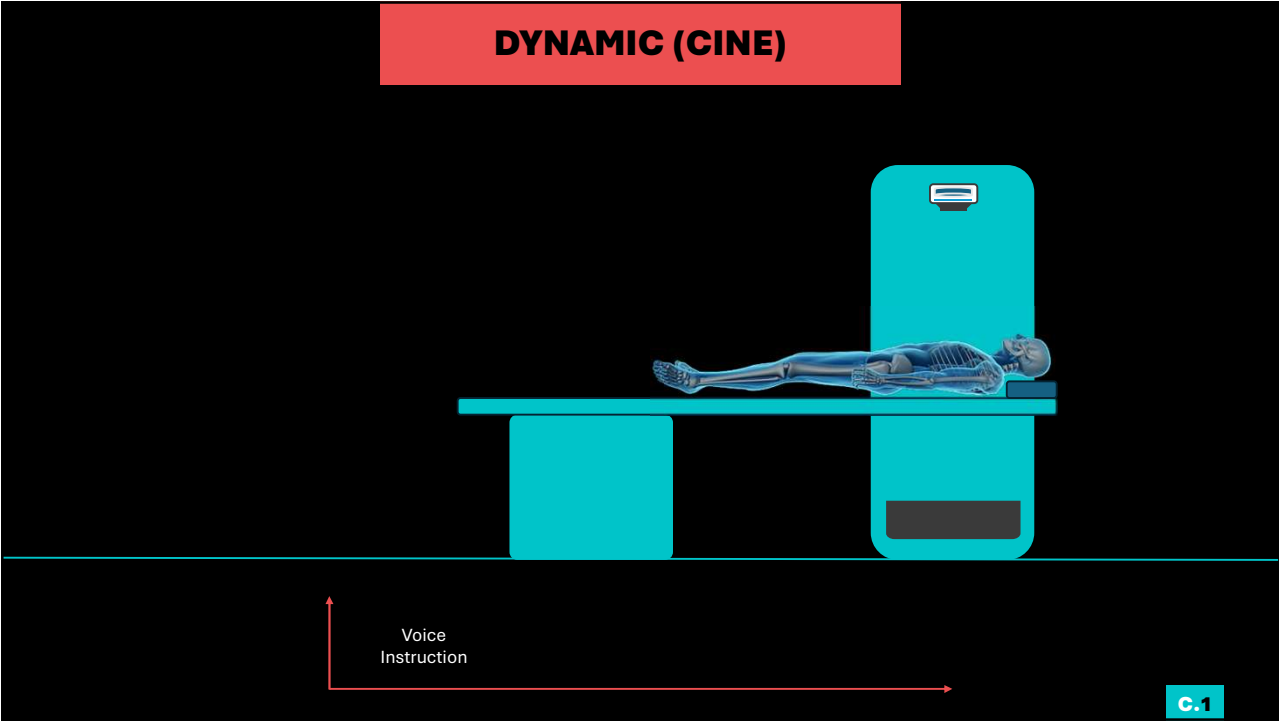
<b>SCANOGRAM (SCOUT OR LOCALIZER)</b>	
<p style="text-align: center; font-weight: bold; margin-bottom: 5px;">AXIAL (STEP &amp; SHOOT)</p> <p>The scan is performed sequentially one acquisition (exposure) at a time. The beam is turned on and off with table movement between exposures.</p>	<p style="text-align: center; font-weight: bold; margin-bottom: 5px;">HELICAL (SPIRAL)</p> <p>The scan is performed as one continuous exposure. The tube/detector constantly rotates and expose the patient while the table is constantly moves into the gantry</p>
<p style="text-align: center; font-weight: bold; margin-bottom: 5px;">VOLUME</p> <p>One shot exposure of an area of the patient (no table movement). The maximum possible size of the area is limited to the width of the detector in the Z-axis</p>	<p style="text-align: center; font-weight: bold; margin-bottom: 5px;">DYNAMIC (CINE)</p> <p>A continuous exposure or multiple exposures of an area of the patient (no table movement). Used for evaluation physiological evaluations.</p>

C.1

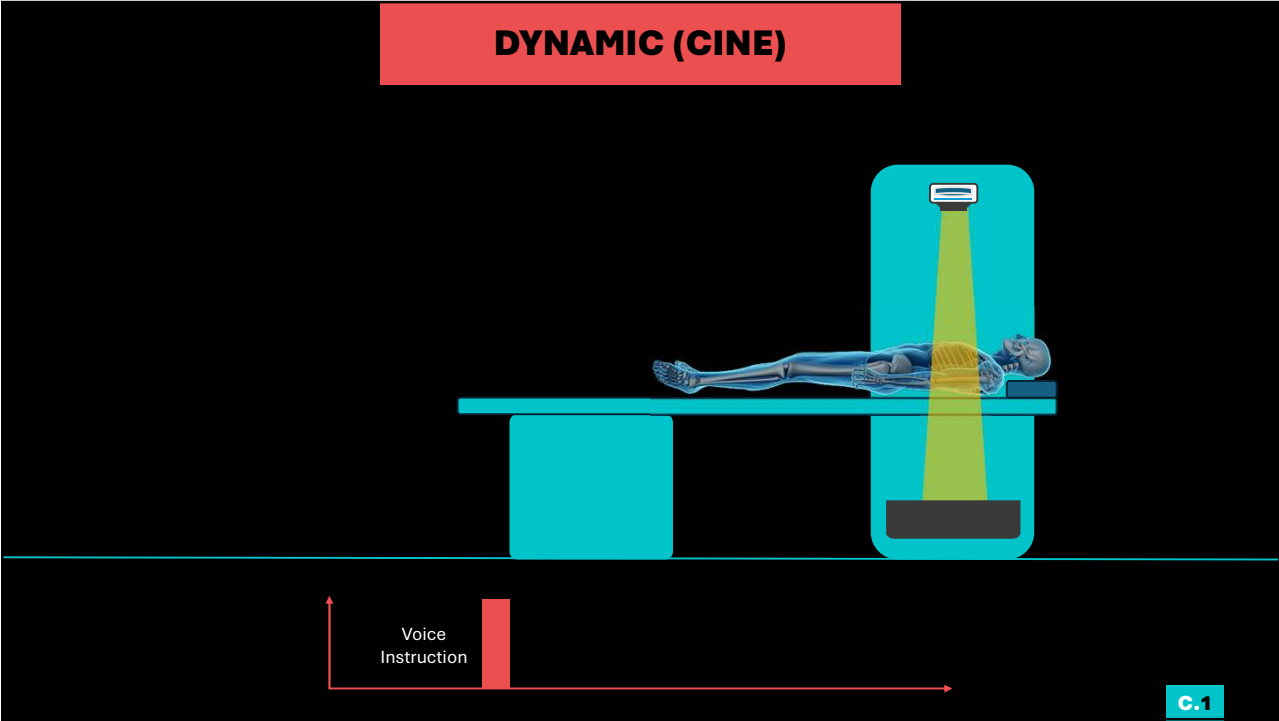
107



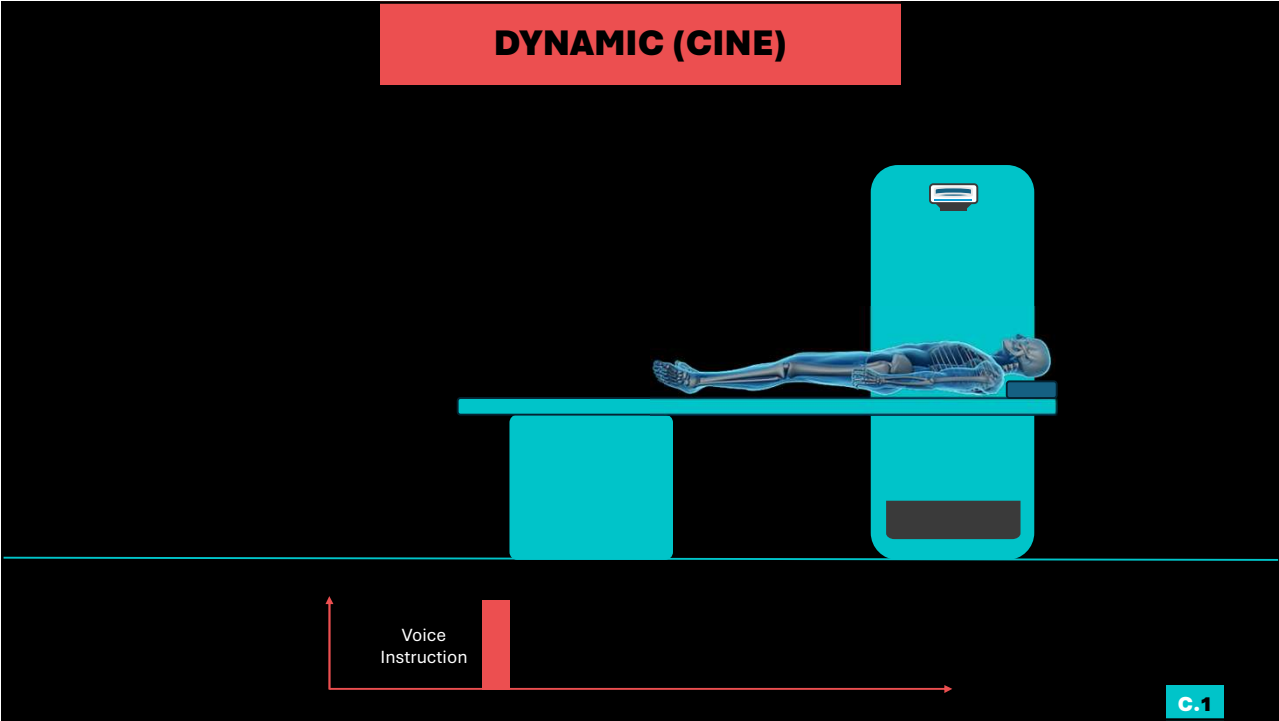
108



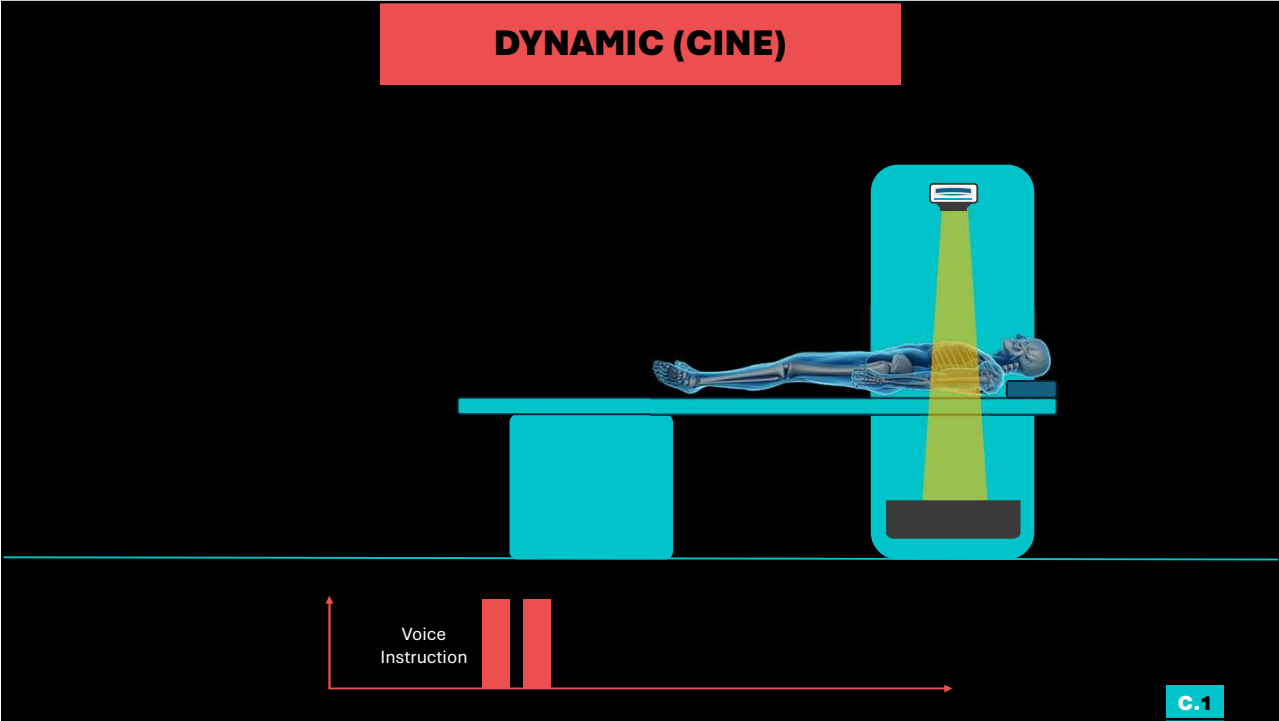
109



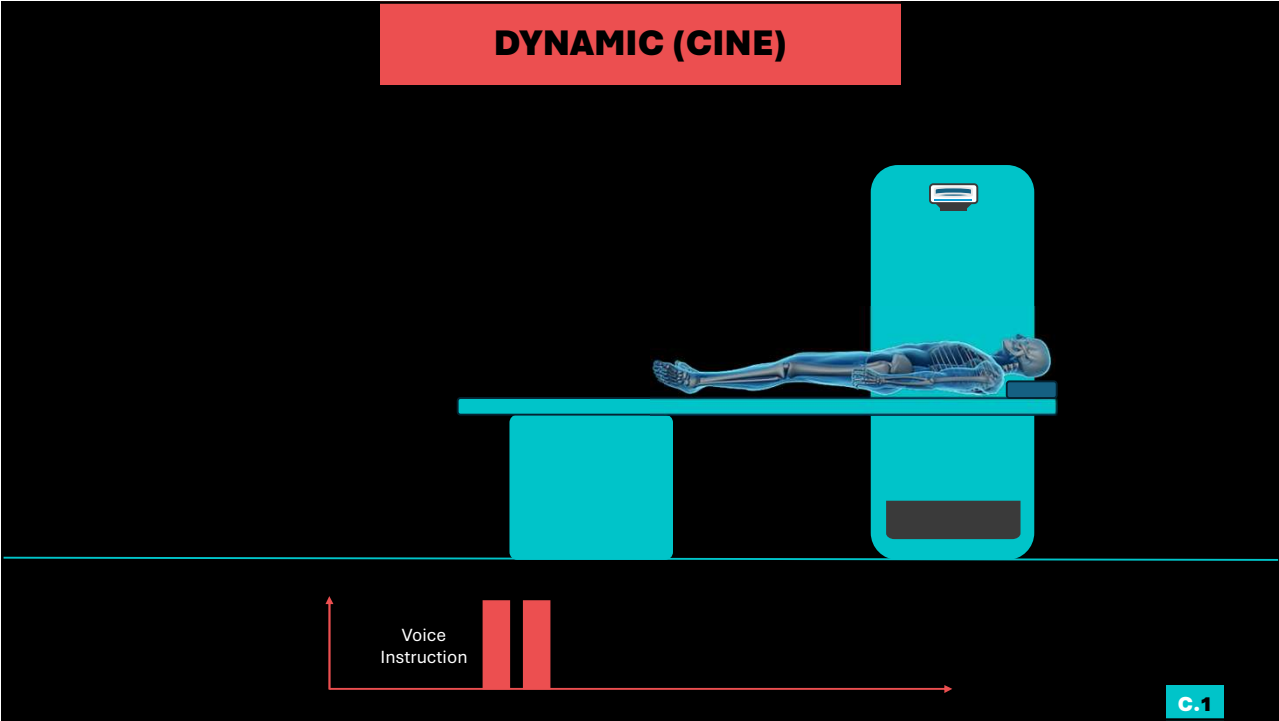
110



111

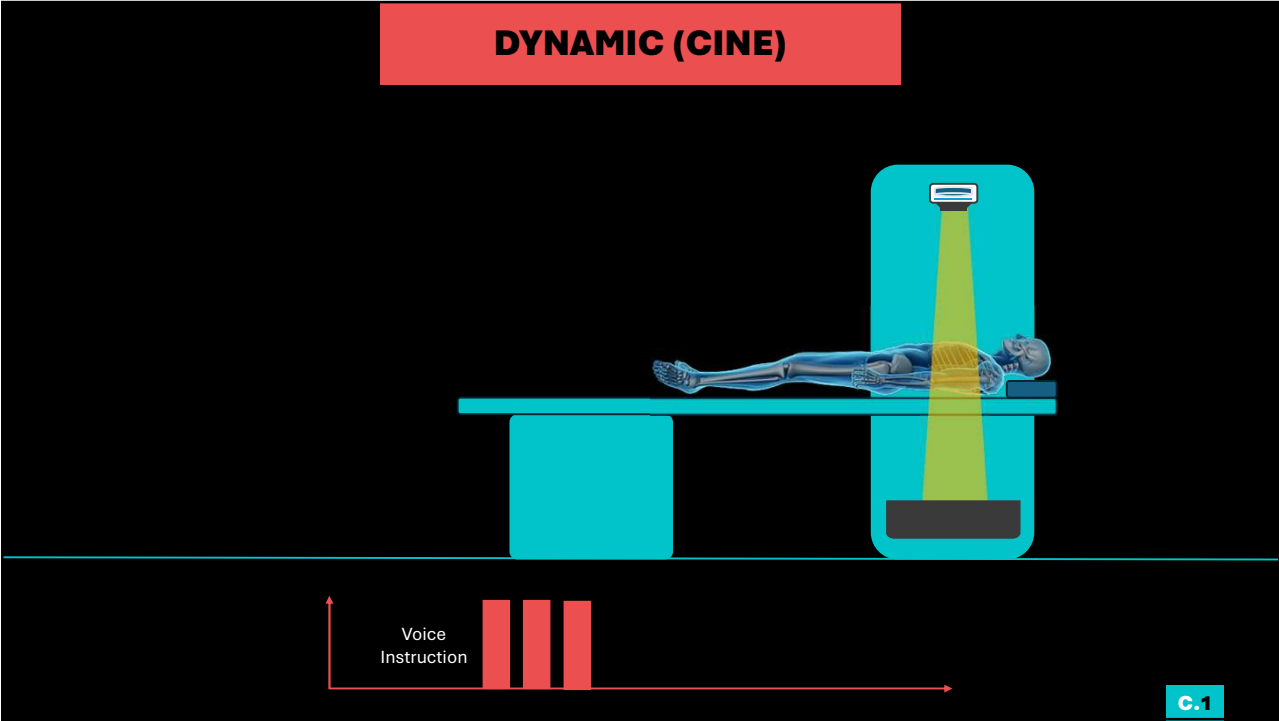


112

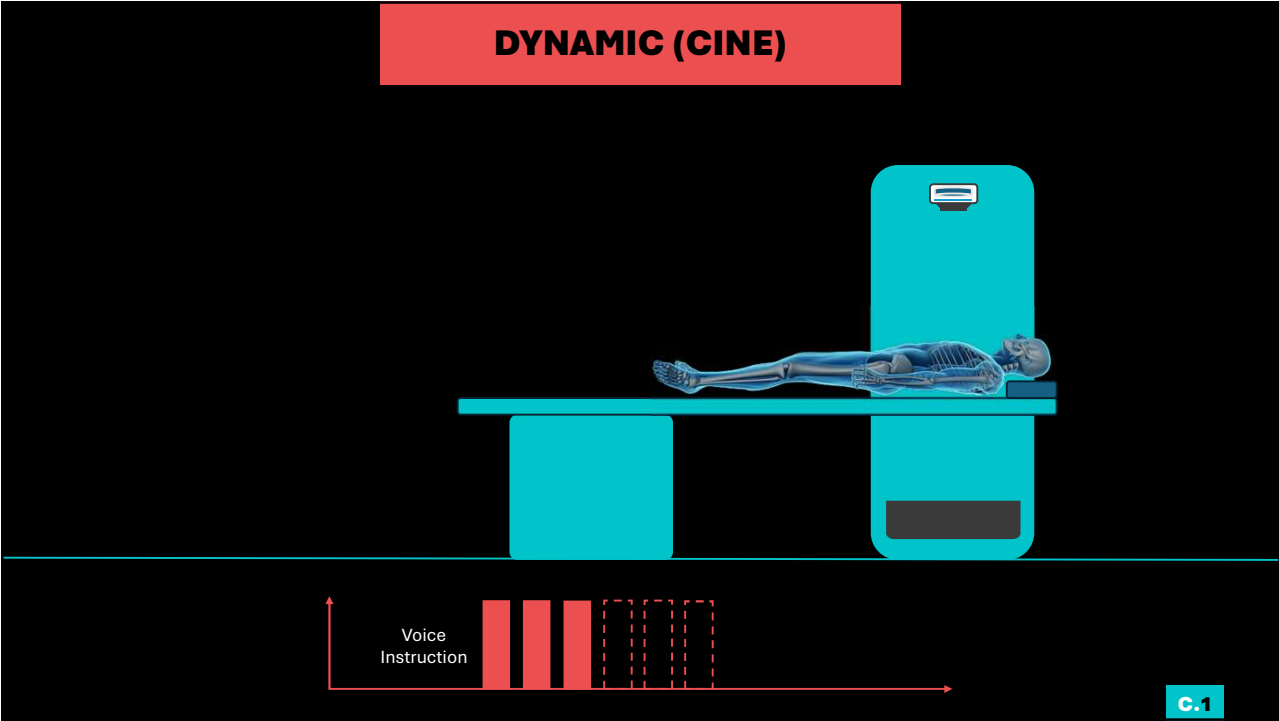


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## DYNAMIC (CINE)

**How it Works:** Acquires a series of images rapidly over time to visualize moving structures, such as the heart or blood vessels.

**Pros:** functional information, real-time visualization of dynamic processes.

**Cons:** very high dose, very large data storage requirements.

C.1

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<b>SCANOGRAM (SCOUT OR LOCALIZER)</b>	
<p style="text-align: center; font-weight: bold; margin-bottom: 10px;">AXIAL (STEP &amp; SHOOT)</p> <p>The scan is performed sequentially one acquisition (exposure) at a time. The beam is turned on and off with table movement between exposures.</p>	<p style="text-align: center; font-weight: bold; margin-bottom: 10px;">HELICAL (SPIRAL)</p> <p>The scan is performed as one continuous exposure. The tube/detector constantly rotates and expose the patient while the table is constantly moves into the gantry</p>
<p style="text-align: center; font-weight: bold; margin-bottom: 10px;">VOLUME</p> <p>One shot exposure of an area of the patient (no table movement). The maximum possible size of the area is limited to the width of the detector in the Z-axis</p>	<p style="text-align: center; font-weight: bold; margin-bottom: 10px;">DYNAMIC (CINE)</p> <p>A continuous exposure or multiple exposures of an area of the patient (no table movement). Used for evaluation physiological evaluations.</p>

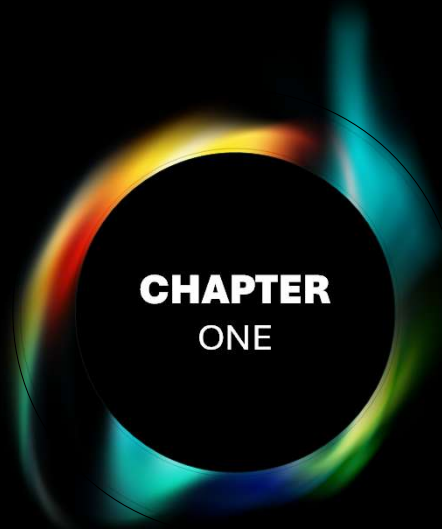
C.1

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<b>SCANOGRAM (SCOUT OR LOCALIZER)</b>	
<p><b>AXIAL (STEP &amp; SHOOT)</b></p> <p>The scan is performed sequentially one acquisition (exposure) at a time. The beam is turned on and off with table movement between exposures.</p>	<p><b>HELICAL (SPIRAL)</b></p> <p>The scan is performed as one continuous exposure. The tube/detector constantly rotates and expose the patient while the table is constantly moves into the gantry</p>
<p><b>VOLUME</b></p> <p>One shot exposure of an area of the patient (no table movement). The maximum possible size of the area is limited to the width of the detector in the Z-axis</p>	<p><b>DYNAMIC (CINE)</b></p> <p>A continuous exposure or multiple exposures of an area of the patient (no table movement). Used for evaluation physiological evaluations.</p>

**C.1**

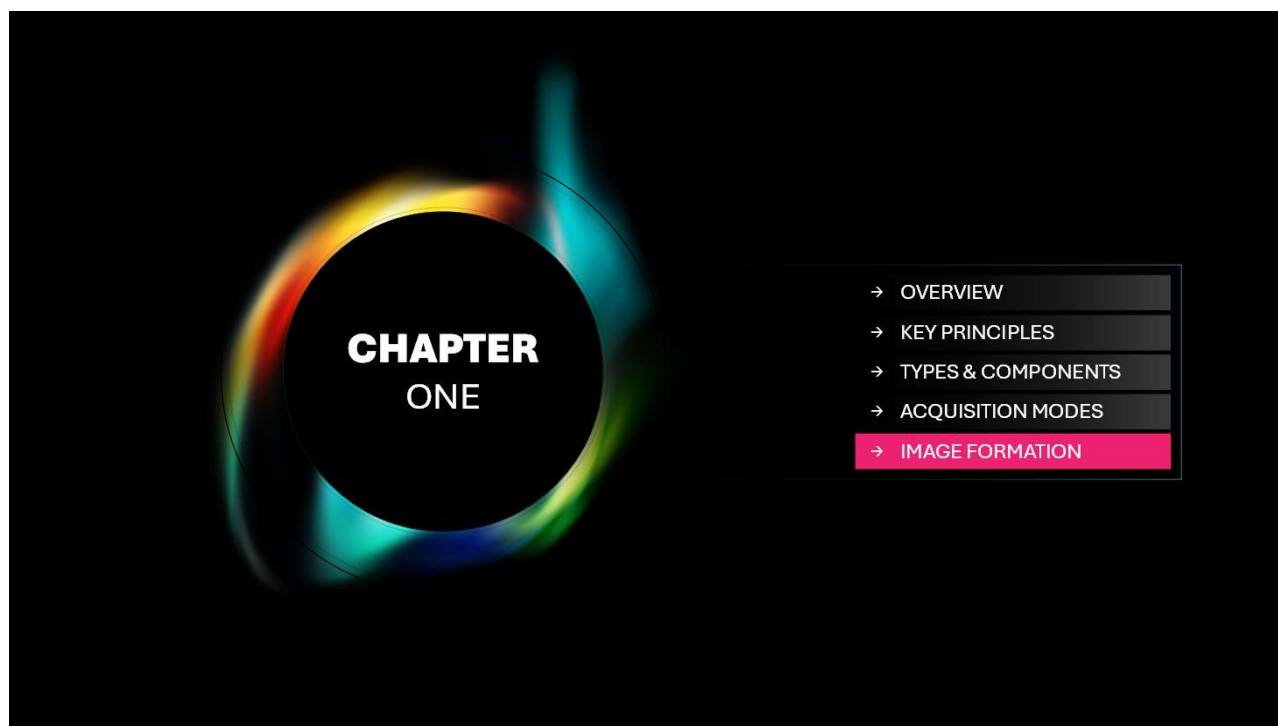
118



**CHAPTER  
ONE**

- OVERVIEW
- KEY PRINCIPLES
- TYPES & COMPONENTS
- ACQUISITION MODES
- IMAGE FORMATION

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### IMAGE PRODUCTION

The basic steps of image production in CT is very similar to digital radiography.

1. X-Ray tube produces the X-Ray beam.
2. Partial attenuation by the patient.
3. The unattenuated photons strike the IR.
4. The IR create an electrical signal.
5. Electrical signal converted to digital signal at the Analog-to-Digital-Converter (ADC).
6. The digital signal (RAW) is processed into image data.
7. Image data sent for viewing and storage.

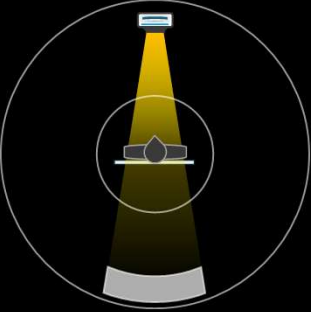
**C.1**

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## IMAGE PRODUCTION

The basic steps of image production in CT is very **similar to digital radiography**.

1. X-Ray tube produces the X-Ray beam.
2. Partial attenuation by the patient.
3. The unattenuated photons strike the IR.
4. The IR create an electrical signal.
5. Electrical signal converted to digital signal at the Analog-to-Digital-Converter (ADC).
6. **The digital signal (RAW) is processed into image data.**
7. Image data sent for viewing and storage.



**This step is different in CT compared to Digital radiography.**

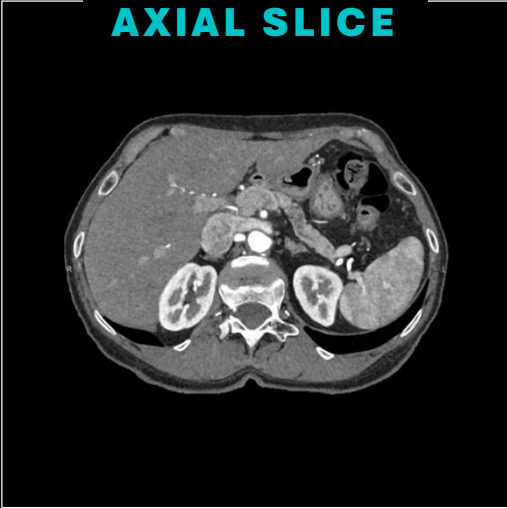
In CT hundreds of projections must be combined into a volume of data and then organized into slices

C.1

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DIGITALLY RECONSTRUCTED

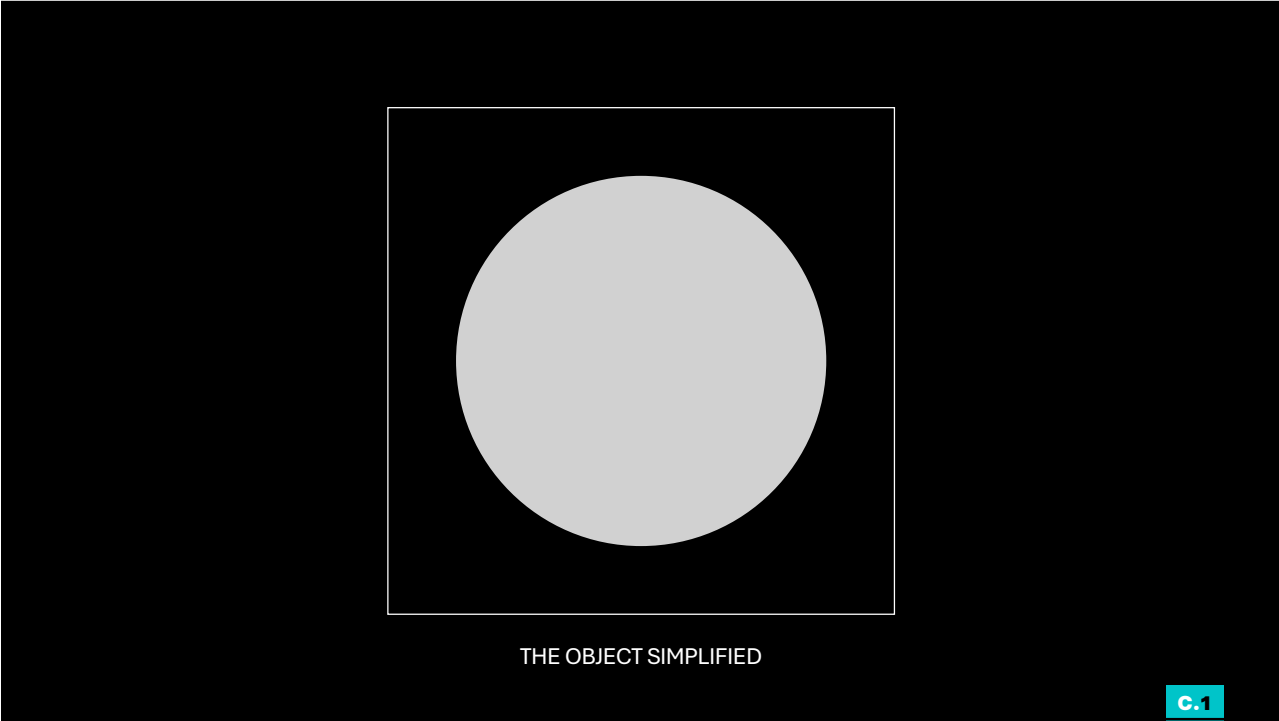
## AXIAL SLICE



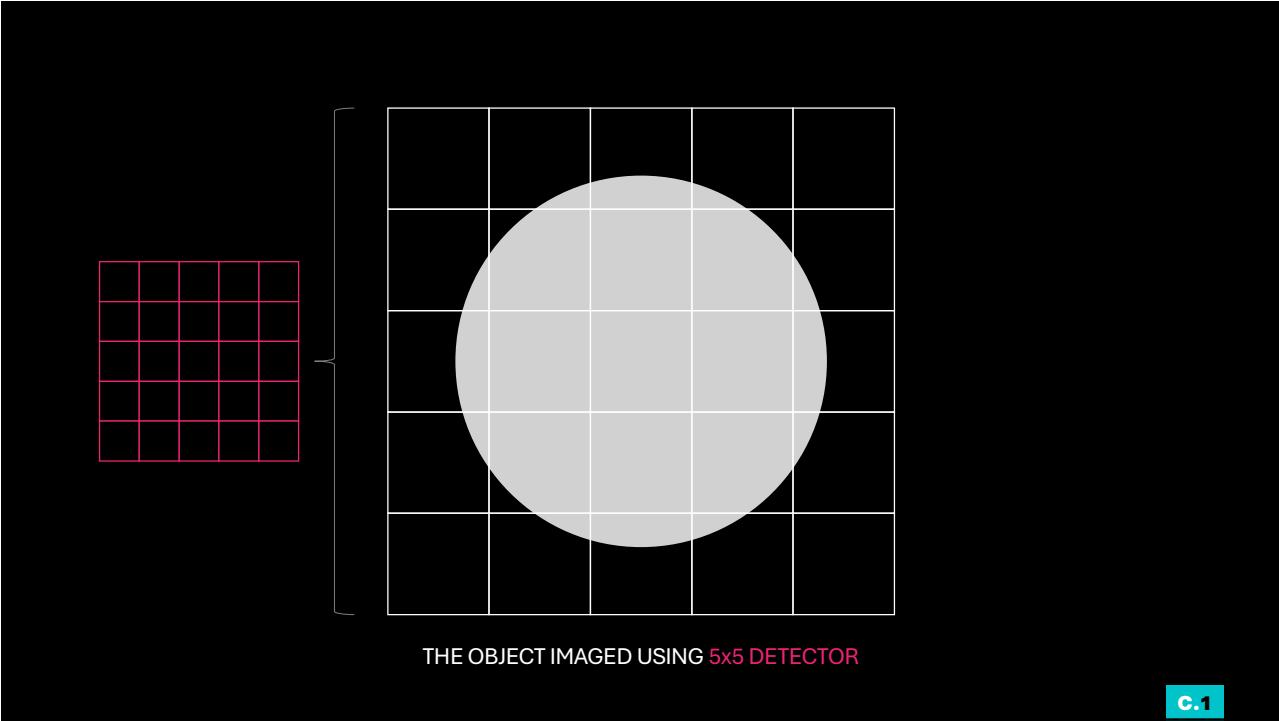
AN IMAGE OF THE OBJECT

C.1

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IN THE REAL WORLD

PROJECTION (A)

PROJECTION (B)

IN THE DIGITAL WORLD

PROJECTION (A)

0	1	2	1	0
1	2	4	2	1
2	4	8	4	2
1	2	4	2	1
0	1	2	1	0

PROJECTION (B)

Using the 5x5 detector and an X-Ray beam  
 Let us image this object from **two different perspectives: (A) & (B)**

C.1

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WE CANNOT SEE WHAT'S INSIDE

0	1	2	1	0
1	2	4	2	1
2	4	8	4	2
1	2	4	2	1
0	1	2	1	0

DETECTOR

4	10	20	10	4
---	----	----	----	---

DETECTOR

DISTRIBUTED

.8	.8	.8	.8	.8
2	2	2	2	2
4	4	4	4	4
2	2	2	2	2
.8	.8	.8	.8	.8

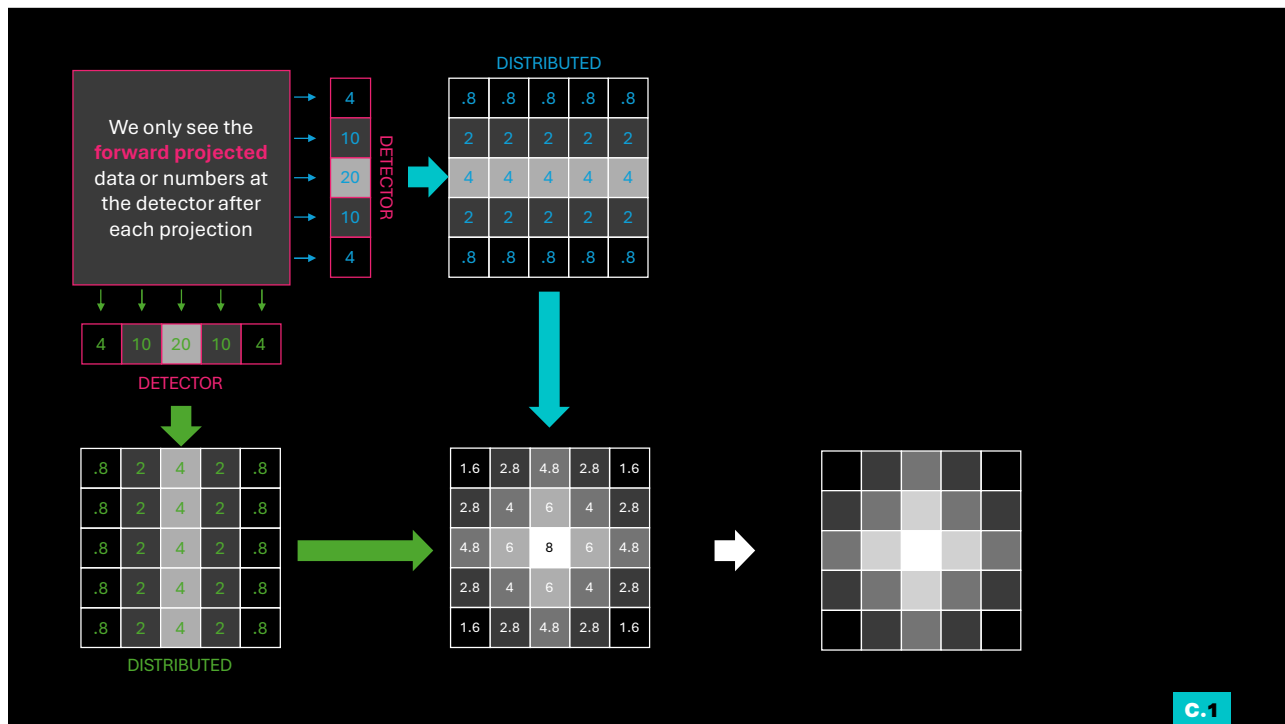
.8	2	4	2	.8
.8	2	4	2	.8
.8	2	4	2	.8
.8	2	4	2	.8
.8	2	4	2	.8

DISTRIBUTED

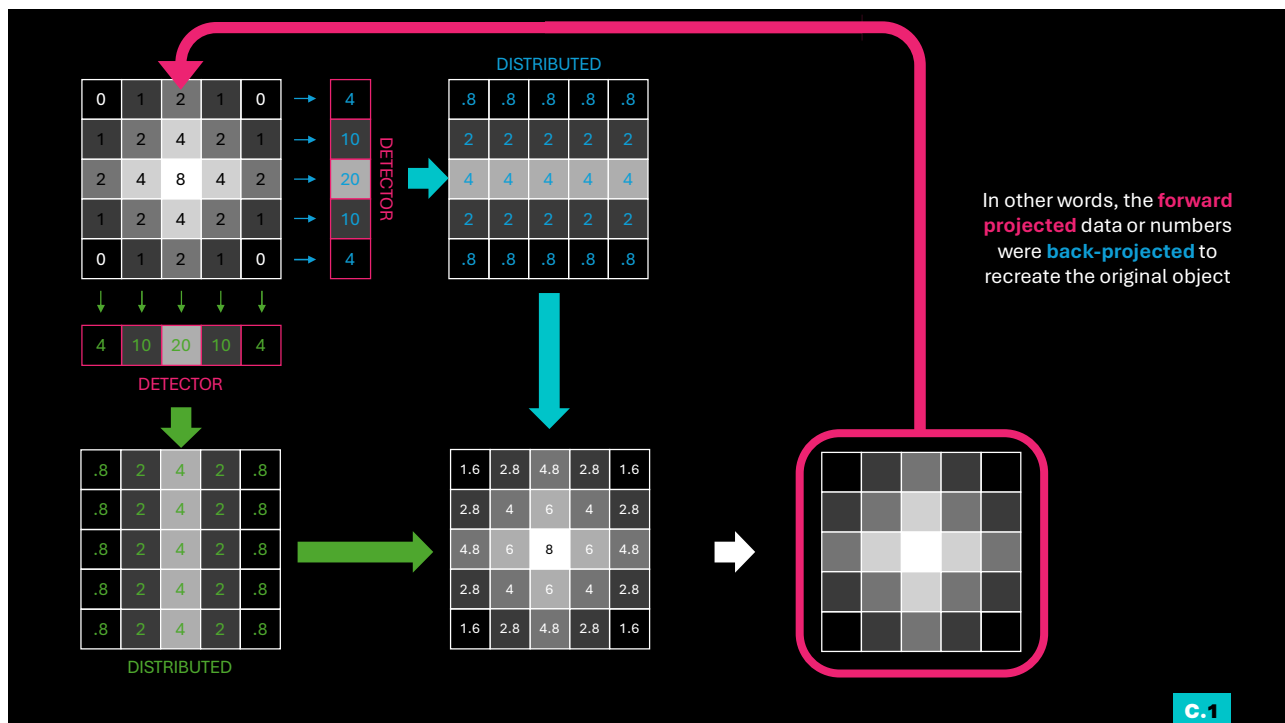
1.6	2.8	4.8	2.8	1.6
2.8	4	6	4	2.8
4.8	6	8	6	4.8
2.8	4	6	4	2.8
1.6	2.8	4.8	2.8	1.6


C.1

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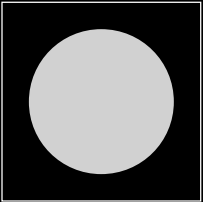
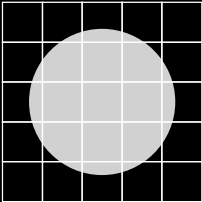
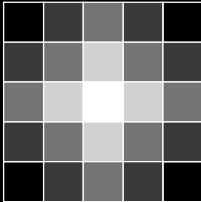


IN THE REAL WORLD

IMAGED DIGITALLY

IN THE DIGITAL WORLD


→

→


Blurry/Image

This technique is called [back-projection](#). It can recreate the original object using multiple forward projections.

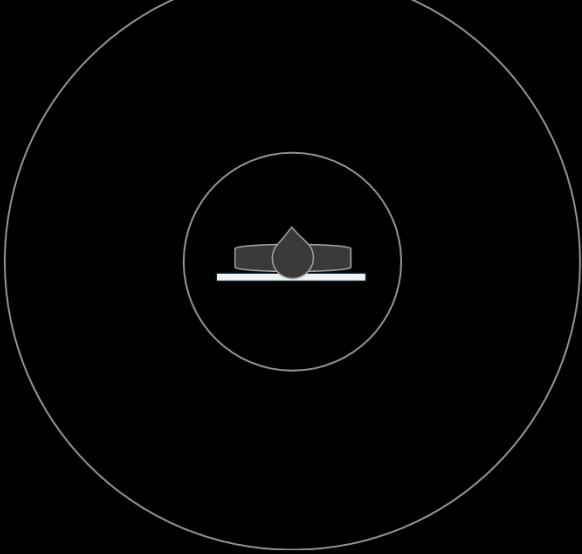
**The problem:** Many projections are needed + [blurry edges](#)

**The solution:** add edge-enhancing sharpening filter ([Filtered back-projection](#))

C.1

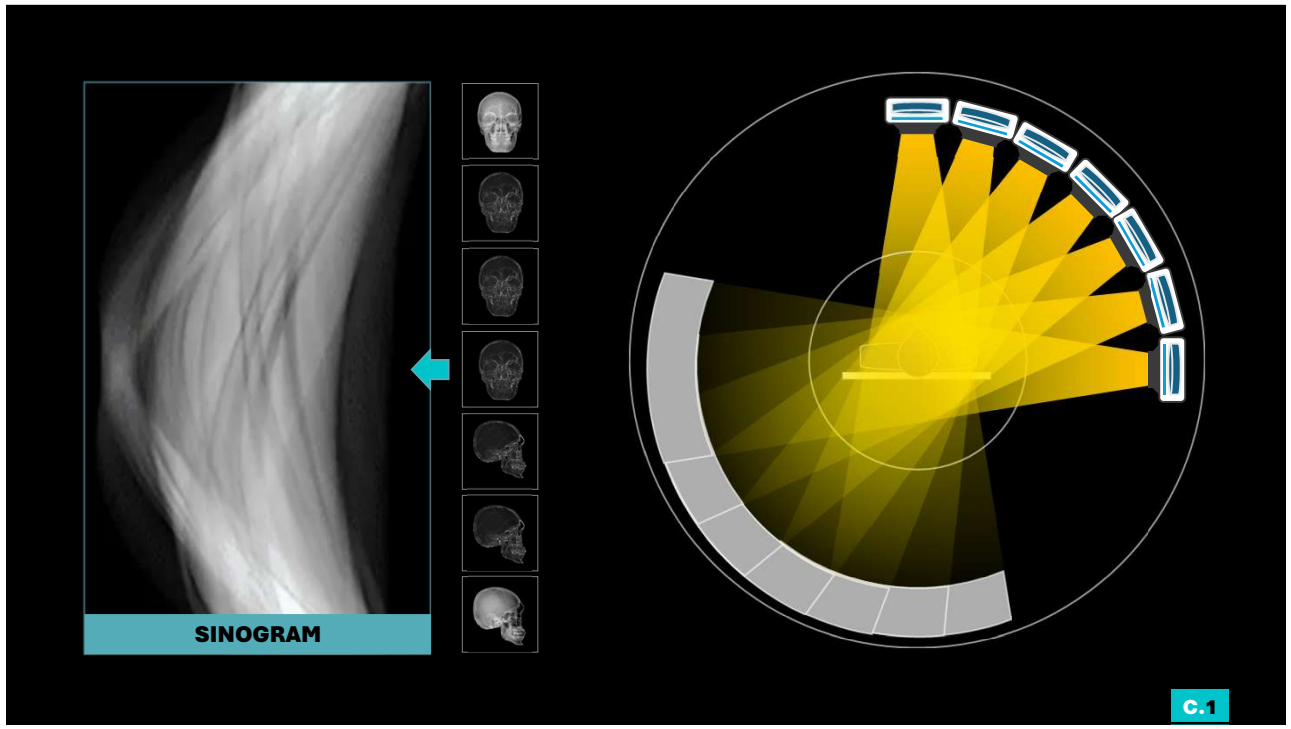
130

FILTERED BACK-PROJECTION

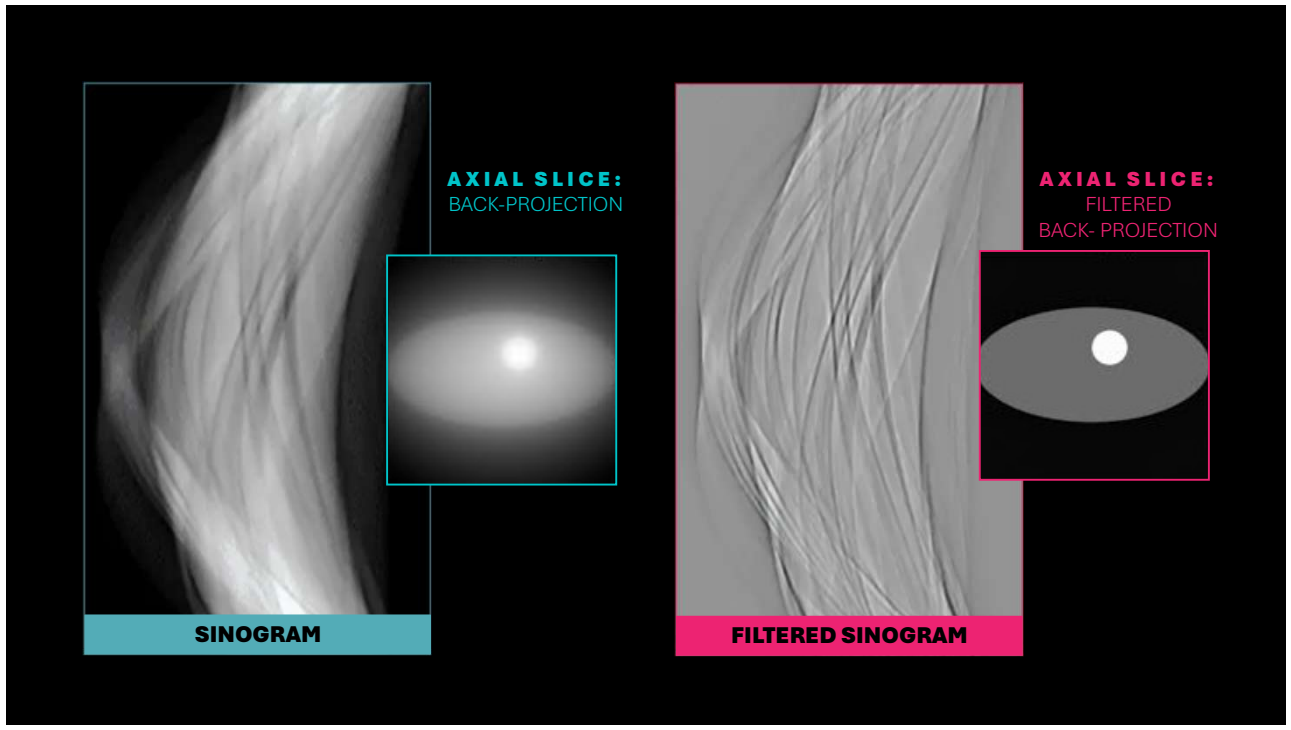


C.1

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### FILTERED BACK-PROJECTION

**How it Works:**

1. **Projection Data:** FBP starts with the projection data acquired by the detectors, which represents the attenuation of the x-ray beam as it passes through the patient from different angles.
2. **Back Projection:** The algorithm "smears" or "back projects" this projection data back onto the image grid. Imagine each projection as a blurred shadow of the object.
3. **Filtering:** To correct for the blurring introduced by back projection, a filter is applied in the frequency domain. This filter is designed to remove the "star-like" artifacts that would otherwise appear in the image.

PROS	CONS
<ul style="list-style-type: none"> <li>Fast and computationally efficient</li> <li>well-established (industry standard)</li> </ul>	<ul style="list-style-type: none"> <li>Susceptible to noise and artifacts</li> <li>FBP does not explicitly account for the physics of x-ray interactions, which can lead to inaccuracies in the reconstructed image.</li> </ul>

C.1

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### ITERATIVE RECONSTRUCTION

Iterative reconstruction (IR) is a CT image processing technique that refines images through multiple cycles of comparison and improvement. Starting with an initial guess, IR simulates the scan and compares it to the actual data. Differences are used to improve the image with each cycle, leading to higher quality images with less noise and potentially lower radiation dose.

```

    graph TD
        START[START] --> E[Estimated image]
        E -- "Forward projected" --> ERD[Estimated Raw Data]
        ERD -- "Compare" --> ARD[Actual Raw Data]
        ARD -- "Back projected" --> CI[Corrected Image(s)]
        CI -- "Iteration" --> ERD
        CI -- "When the conditions are met" --> END[END]
        END --> FI[Final Image]
    
```

C.1

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**ITERATIVE RECONSTRUCTION**

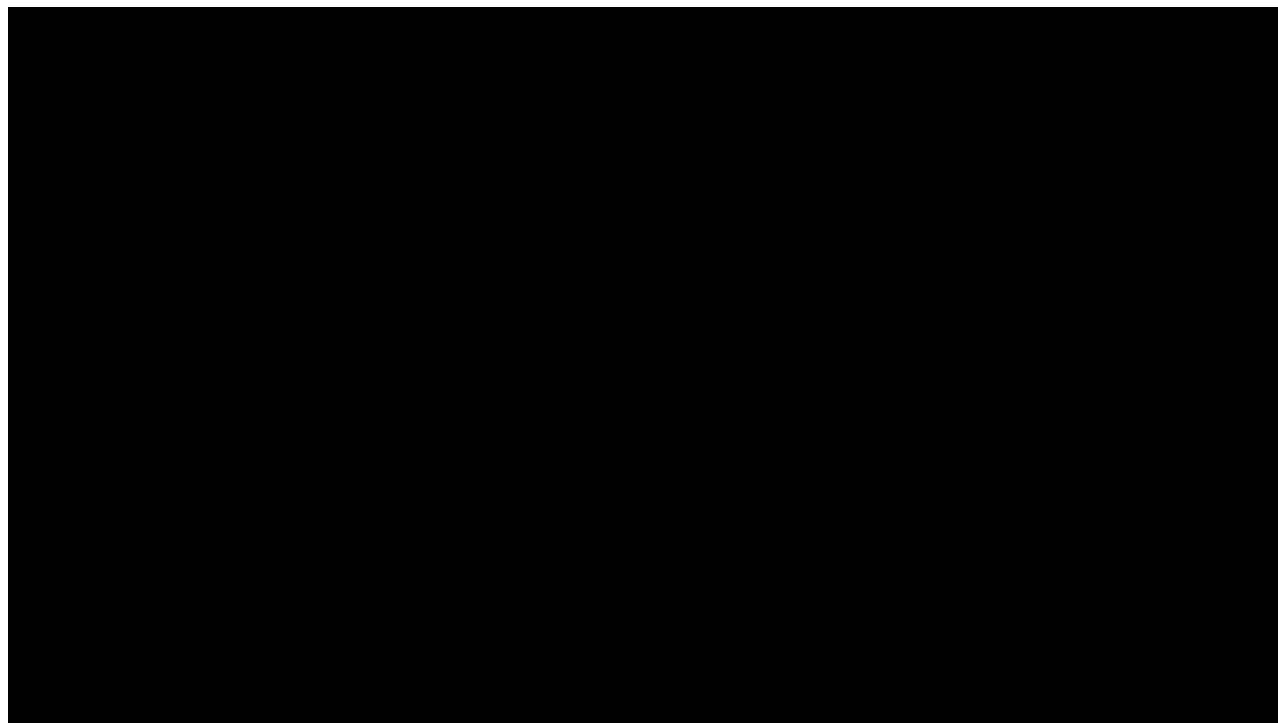
**How it Works:**

1. **Initial Image Estimate:** IR starts with an initial estimate of the image (FBP).
2. **Forward Projection:** The algorithm then "projects" this estimated image forward to simulate what the detector readings would be.
3. **Comparison:** These simulated projections are compared to the actual measured projections.
4. **Image Update:** Based on the difference between the simulated and measured projections, the algorithm updates the image estimate.
5. **Iteration:** This process is repeated iteratively, with each iteration refining the image estimate until it converges to a solution that is consistent with the measured data and the physics of the imaging process.

<b>PROS</b>	<b>CONS</b>
<ul style="list-style-type: none"><li>• Excellent noise reduction and Image quality</li><li>• Has potential to reduce the radiation dose</li><li>• Less susceptible to artifacts and can be used to reduce artifacts.</li></ul>	<ul style="list-style-type: none"><li>• Slow and computationally demanding</li><li>• Images may look "Plastic-y"</li></ul>

**C.1**

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